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## **Isotope tracing enhancement of chemiluminescence assays for nitric oxide research**

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## Abstract

Chemiluminescence assays are used widely for the detection of nitric oxide (NO)-derived species in biological fluids and tissues. Here we demonstrate that these assays can be interfaced with mass-sensitive detectors for parallel determination of isotopic abundance. Results obtained with tri-iodide and ascorbic acid-based reductive assays indicate that mass spectrometric detection enables NO isotope-tracing experiments to be carried out to a limit of detectability of a few picomol, a sensitivity similar to that of standard gas phase chemiluminescence methods. The advantage afforded by mass spectrometric detection is demonstrated using the murine macrophage cell line J774, which is shown here to reduce  $^{15}\text{NO}_3^-$  to  $^{15}\text{NO}_2^-$  under anoxic conditions. The particular combination of an analytical and cellular system described here may hold promise for future characterization of the enzymatic pathways contributing to mammalian nitrate reductase activity, without background interference from  $^{14}\text{NO}_2^-$  derived from other sources.

**Keywords:** chemiluminescence assay; isotope tracing; mass spectrometer; nitrate; nitrate reductase; nitric oxide, nitrite.

## Introduction

Nitric oxide (NO) plays an important role in cell signaling by promoting a wide range of posttranslational protein modifications, such as heme nitrosylation and S-nitrosation. Despite the attention that these signaling mechanisms have received in the last two decades, there remains much ambiguity about the precise chemical pathways that link NO sources to the resulting protein modifications. For instance, the classical NO-signaling pathway involving heme-nitrosylation, which includes the prototypical activation of soluble guanylyl cyclase, is widely viewed as arising from capture of NO generated from local enzymatic NO synthesis via oxidation of L-arginine. It is now recognized that nitrite ( $\text{NO}_2^-$ ) may also contribute to hemeprotein nitrosylation via interaction with the mitochondrial electron transport chain (Walters et al., 1967; Nohl et al., 2000, Tischner et al., 2004), deoxyhemoglobin (Cosby et al., 2003; Hunter et al., 2004), myoglobin (Rassaf et al., 2007; Shiva et al., 2007; Hendgen-Cotta et al., 2008), xanthine oxidase (Li et al., 2004; Webb et al., 2004), non-enzymatic formation of NO as a result of disproportionation of nitrous acid (Zweier et al., 1995; Hunter et al., 2004), and a co-operative mechanism between hemes and thiols (Bryan et al., 2005). In the case of protein S-nitrosation, the process can potentially occur through many intermediate pathways that involve reactions with higher order nitrogen oxides (e.g.  $\text{N}_2\text{O}_4$  or  $\text{N}_2\text{O}_3$ ) (Williams, 1988) superoxide (Schrammel et al., 2003), metal ions (Williams, 1988; Stubauer et al., 1999), thiyl radicals (Jourdeuil et al., 2003) and nitrite (Bryan et al., 2005). Further compounding this

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complexity, the chemical pathways connecting NO sources to potential protein modifications are critically dependent on intracellular conditions (e.g. oxygen tension, pH, redox state), on the presence of hydrophobic regions in proximity to NO sources (Liu et al., 1998), and on the nature of the protein microenvironment around the thiol group (Stamler et al., 1997; Ascenzi et al., 2000). The multiplicity of potential pathways is thus leading to a growing realization that much work remains to be done before the role NO plays in cellular function can be fully characterized. Attaining this level of understanding will require a combination of analytical tools that not only are capable of detecting biologically relevant levels of NO-related products, but also able to trace their chemical origin through isotopic differentiation.

A common approach for the detection of biologically generated NO species is the NO chemiluminescence assay. This approach relies on the extraction of NO from selective species, either chemically or optically, and their subsequent detection with an NO chemiluminescence detector where trace levels of NO are detected in the gas phase through its chemiluminescent reaction with ozone (Fontijn, 1970). When coupled to the gas efflux from purge vessels containing reducing/oxidizing solutions or from UV irradiated capillaries, this detector can quantify NO products, including nitrite and nitrate (Walters et al., 1978; Cox and Frank, 1982; Dunham et al., 1995; Yang et al., 1997; Trushina et al., 1997), nitroso products (Massey et al., 1984; Stamler et al., 1992; Samouilov and Zweier, 1998; Ewing and Janero, 1998; Gladwin et al., 2000; Rassaf et al., 2002; Jourdain et al., 2005; Wang et al., 2005; Zhang et al., 2005), nitrosyl-hemes (Gladwin et al., 2000; Feelisch et al., 2002) and total NO (Sonoda et al., 1997). The wide use of NO chemiluminescence detectors in life science laboratories can be attributed to several factors, including sensitivity, selectivity, quick response, ease of use, and the relatively moderate pricing and space requirements that are comparable to other commonly used laboratory instruments. Here we describe an enhancement to NO chemiluminescence assays that retains their original advantages while providing isotopic differentiation capabilities. Following earlier work by Russow (1999) on mass spectrometric detection of NO from aqueous nitrite and nitrate using a chemical vessel, this work demonstrates that a mass spectrometer detector can either replace, or operate in parallel with, NO chemiluminescence detectors without altering assay conditions and sacrificing convenience. The approach incorporates a detector that is commonly used in GC/MS systems, which is also sold as a stand-alone system with supporting data acquisition software. Our results indicate that mass spectrometric detection used in this way allows NO isotopic-tracing experiments to be carried out to a limit of detectability of a few picomoles. The advantage afforded by mass spectrometric detection is illustrated by providing evidence that the murine macrophage J774 displays nitrate reductase capabilities, as demonstrated by the emergence of  $^{15}\text{NO}_2^-$  immediately following the addition of  $^{15}\text{NO}_3^-$  to cell lysates.

## Results

### Apparatus

The apparatus described here for the isotopic detection of NO products is shown schematically in Figure 1. The setup is based on those designed previously for the use of NO-ozone chemiluminescence detection (CLD), with a few modifications to accommodate the added mass-sensitive detector (MSD) and to control the relative flow toward both instruments. The CLD in our lab is a Dasibi 2108 (Dasibi Environmental Corp., Glendale, USA), modified to process the output from the photomultiplier tube (PMT) directly into a DAT-710 A/D converter (DataQ Instruments, Akron, OH, USA) using a sampling rate of 1 Hz. The nominal intake flow rate for this instrument is 100 ml/min and the NO sensitivity under direct PMT monitoring is approx. 10 ppb. The MSD used here (5975B XL; Agilent Technologies, CA, USA) employs electron impact ionization and a high-volume turbopump (ca. 260 l/min). The flow to the MSD is restricted by a 0.25mm ID fused silica gas chromatography (GC) column measuring 7.5 m in length, resulting in an intake flow rate of 4 ml/min for an input pressure of 2 atmospheres. The column is maintained at all times at a temperature of 100°C inside an oven (1321F; VWR, West Chester, PA, USA) to prevent accumulation of adsorbed gases that may occur primarily when the apparatus is not in use. A hole two inches in diameter was bored through the side of the oven to accommodate the MSD inlet in order to prevent condensation of volatile species at that point. The MSD is operated in selected ion monitoring (SIM) mode, scanning for masses  $m/z = 29, 30,$  and  $31$ . Integration times were set to either 100 ms for scanning conditions using MSD auto-tuning parameters or 400 ms when operating under manually adjusted MSD parameters (see below).

Samples containing NO related products are injected into a 40 ml Sievers purge vessel (GE Analytical Instruments, Boulder, CO, USA), containing a suitable reactive solution that strips the NO off its binding site and releases it into the gas phase. The vessel is continuously purged with ultrahigh-purity helium (UHP He) with an inlet gauge pressure of typically 20-40 psi (135-270 kPa) that rapidly extracts dissolved NO from the solution and transports it at rates of 50-100 ml/min towards the detectors for quantification. Water vapor transported by the carrier gas is partially recondensed by the jacketed condenser that is built into the Sievers purge vessel, maintained here near 0°C. The remaining gas is filtered through a 10 ml Sievers purge vessel containing a 1 M solution of NaOH to trap corrosive gases and higher order nitrogen oxides. Finally, the water vapor of the gas en route to the detectors is reduced by the condenser built into the second purge vessel, which is also maintained near 0°C.

The gas sample emerging from the chemical vessels is split by a Swagelok T connector between the two detectors. The majority of the flow (>90%) is directed toward the CLD since the MSD flow is limited to 4 ml. To help maintain the intake pressure near 1 atm for the CLD,

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the line leading to it is opened to the atmosphere with the aid of a T connector that is uncapped at one end. This open point also acts as a constant pressure point that helps to regulate upstream where the flow splits toward the MSD. Exposure to atmospheric NO contributes minimally to our signals since our lab is located in a wooded campus within a relatively small metropolitan area. In areas where NO levels are higher and variable, the same pressure regulation could be achieved with the aid of a balloon attached to the open end, which is filled periodically with He. Finally, a needle valve between the two T's adjusts the flow through that line in order to control the balance of flow between the MS and CL detectors.

Even with non-detectable levels of atmospheric NO, air contamination in the gas stream can produce small contributions to the signals at  $m/z = 30$  as demonstrated in Figure 3. The contribution at  $m/z=30$  is likely due to the partial fragmentation of  $O_2$  and  $N_2$  in the ion source, followed by recombination into NO. The signal observed at  $m/z=31$  always tracks the levels of  $O_2$  at  $m/z=32$  and is likely due to crosstalk between the two mass channels. Control of air leaks into the gas lines is therefore critical for proper quantification of NO with minimal interference. Since molecular oxygen can diffuse with ease through plastics, care is taken to avoid using these materials in the gas lines. Our apparatus makes use of 1/8 inch (3.2 mm) stainless steel (SS) tubing, except for a portion leading to the chromatography (GC) column which used 1/16 inch (1.8 mm) tubing. All tubing is joined with SS Swagelok connectors. Coupling of the GC column to the 1/16 inch tubing is achieved with a Valco 1/16 inch stainless steel internal union with a fused silica adapter ferrule on the column side. In addition to air tight tubing and junctions, our apparatus makes use of injection septa designed for GC injectors. Another factor that affects these levels is contamination of the lines leading to the MSD, which is particularly evident when they are opened and exposed to atmospheric gases. For this reason we typically isolate those lines at the end of the day by shutting the switch-valve and the Teflon valve at the exit of the second condenser and keeping the MSD running continuously. In addition to leaks, one must contend with dissolved air that may be present in solution. For samples that can be studied under anoxic conditions, the air contamination can be eliminated simply by purging with pure argon for 30 seconds prior to injection into the reaction vessel. Whenever experiments require extended periods of purging, e.g. biological samples that must be maintained anoxic for several minutes, it is recommended that the gas be scrubbed with NaOH to trap NO<sub>x</sub> contaminants that may result in the creation of artifactual NO-related products. When normoxic or hypoxic conditions are required, we resort to an analytical procedure that uses information obtained from  $m/z = 29$  to subtract the contributions due to contamination at  $m/z = 30$  and 31. This procedure is discussed below in the section.

As illustrated in Figures 1-5, signals obtained with MS detection are very similar in lineshape to those obtained with chemiluminescence (Feelisch et al., 2002). They are best described by exponentially modified gaussian functions, resulting from the convolution of gaussian

processes such as diffusion of gases, and exponentially decaying processes such as reaction kinetics in the purge vessel, extraction of the analytes from the reducing solution, and detector response. Our analysis software (Peakfit, Systat Software, CA, USA) allows for incorporation of this profile information to determine the best peak fit, underlying background, and area under the peak. Figure 2 shows a representative curve fit obtained with a 100 pmol injection of nitrite into a tri-iodide assay.

**Performance under autotuned MSD operation and with minimal signal processing** In this section we describe the performance of MSD based NO detection under two experimental conditions that facilitate MSD operation and minimize signal processing: autotuning MSD operation and use of He under high pressure/flow settings. Autotuning offers a hands-free approach to maintaining instrument sensitivity and selectivity. It allows a mass spectrometer to determine its own voltage and current settings that ionize and guide molecules towards their detectors. The performance is optimized for selectivity and sensitivity over a wide range of molecular masses, but not necessarily for smaller mass ranges such as the one targeted in this study. The second aforementioned experimental condition is the adoption of pressure settings that in our experience minimizes baseline fluctuations and thus facilitates subsequent signal analysis. Those were found to occur at a supply and split flow gauge pressures of 40 and 32 psi, respectively. In the next section we describe other conditions that require additional optimization and signal processing but provide greater sensitivity. Both approaches are presented separately here in the interest of those who may wish to duplicate our system for the following reasons. The first approach is easier to implement and may be sufficiently sensitive to quantify NO products in e.g. translational studies using biological fluids such as plasma and urine. Furthermore, it offers a valuable benchmark to meet before attempting to implement the more advanced changes that provide greater sensitivity.

Typical MSD tracings extracted for the signals at  $m/z = 29, 20,$  and  $31$  are shown in Figure 3. The curves illustrate the performance of the system obtained with 1 nmol injections of  $^{14}\text{NO}_2^-$ ,  $^{15}\text{NO}_2^-$ , and of an equimolar mixture of  $^{14}\text{NO}_2^-$  and  $^{15}\text{NO}_2^-$ , all in Ar-purged PBS. The fourth injection illustrates the signals generated by dissolved air in fully aerated buffered solutions. Large amplitude signals are seen with every injection, with ionic masses in accordance to the substances injected and to their proportions. The large peak arises from  $^{14}\text{N}^{15}\text{N}$  (natural abundance of 0.73%). Smaller artifactual signals are also seen in adjacent mass channels. The smaller signal registered at  $m/z=31$  during the first injection of  $^{14}\text{NO}_2^-$  arises in part from the isotopic contribution from  $^{15}\text{N}^{16}\text{O}$  and  $^{14}\text{N}^{17}\text{O}$  (total natural abundance of 0.4%) with the remaining contribution (approx. 0.6%) arising from cross-talk with the  $m/z=30$  signal. The next injection of  $^{15}\text{NO}_2^-$  also displays a small signal at  $m/z=30$  corresponding to a 2% fraction of the 1 nmol injection of  $^{15}\text{NO}_2^-$ . This fraction is consistent with the 2%  $^{14}\text{NO}_2^-$  impurity level quoted by the  $^{15}\text{NO}_2^-$  supplier. Lastly, the small signals at  $m/z = 30$  and  $31$  seen with injections of a

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fully aerated PBS sample arise from  $^{14}\text{N}^{16}\text{O}$  formed by partial fragmentation of  $\text{O}_2$  and  $\text{N}_2$  in the ion source, and from crosstalk between the larger signal at  $m/z=32$  ( $^{16}\text{O}^{16}\text{O}$ ) and  $m/z=31$ .

To test the linearity of our MSD approach and its correlation with chemiluminescence detection, 100  $\mu\text{l}$  solutions of  $^{15}\text{NO}_2^-$  with concentrations of 100 nM, 300 nM, 1  $\mu\text{M}$ , 3  $\mu\text{M}$  and 10  $\mu\text{M}$ , were injected in triplicate into an  $\text{I}^-/\text{I}_3^-/\text{HCl}$  reductive assay (see Figure 4). The top panel of Figure 4 shows a realtime scan extraction for  $m/z = 31$  corresponding to the expected mass for  $^{15}\text{NO}$ . The peak areas for those injections are shown in the middle panel of Figure 4 as a function of  $^{15}\text{NO}_2^-$  injected. The linearity of the response is evaluated through a power law fit  $y = ax^b$  and resulted in a near-unity power dependence with  $b=0.9733$ . The lower panel compares the same integrated signals with those obtained simultaneously with a chemiluminescence detector. The near-linear relationship between the two confirms that the MSD signals observed are due to the detection of NO. Similar MSD linearity and correlation with chemiluminescence detection were obtained with injections of  $^{14}\text{NO}_2^-$  and monitoring of  $m/z$  30 (data not shown).

Similar experiments were conducted with the nitrite specific reactive mixture containing ascorbic acid and HCl. Compared to the tri-iodide assay, the ascorbic acid based assay produces broader temporal signals with consequently lower limits of detection (approx. 30 pmol, see Figure 5, top panel).

### **Extended performance using reduced purge flow, manual tuning, and background subtraction**

Additional hardware adjustments and signal processing have enabled us to achieve extended performance in terms of sensitivity and in the ability of handling aerated samples. To attain higher signals we lowered the flow rate to the chemiluminescence relative to that into the MS detector. Best results were achieved at a He supply and split-flow gauge pressures of 20 psi and 17 psi, respectively. Under these operating conditions we observe that the duration of the NO signals is increased from 0.2 to more than 0.8 minutes. Further gain in signal to noise ratio were attained with adjustments to parameters that control the performance of the MSD analyzer. One simple adjustment takes advantage of the fourfold increase in duration of the NO signals registered under lower flow conditions. This enabled us to decrease the sampling rate fourfold by increasing the integration time from 100 to 400 ms per ion. A four-fold increase in integration time resulted in a twofold increase in signal to noise ratio. Additional sensitivity was obtained with manual adjustments to default and autotuned parameters that control the MSD analyzer. Using an electron ionization current of 60.6  $\mu\text{A}$ , and voltages for ion focusing, the repeller, entrance lens, and entrance lens offset of 90.2V, 30.12V, 40.0V, and 15.31V, respectively, we were able to increase the integrated signal another fourfold without significant changes in background noise.



A drawback from lower pressure operation is the emergence of ripples in the baseline with a period also on the order of a minute, as illustrated in middle panel of Figure 5. The nature of the ripple is unclear at this time since it manifests itself at only at selected  $m/z$  ions including all the ones monitored here. However, since the ripples at  $m/z = 30$  and  $31$  are consistently in phase with the one at  $m/z=29$ , we followed a simple procedure that uses the data from the latter to correct for the ripple in the former ions. To null the ripple at  $m/z=30$ , for instance, the data from  $m/z=29$  was first scaled down by a constant factor and then subtracted from the data at  $m/z=30$ . The factor selected corresponded to one that minimized the standard deviation for a portion of the subtracted curve that should normally be flat, i.e. a portion before or after the signal. The minimization of the standard deviation can be accomplished manually by trial and error or using an automatic routine such as the Solver option available in Microsoft Excel. The effectiveness of this background subtraction procedure is illustrated in the lower panel of Figure 5.

The background subtraction procedure outlined above proved effective for samples purged of air. For un-purged samples, where dissolved air produces artifacts as illustrated in Figure 3, we developed an additional procedure that subtracts the air artifacts from the signals. The relative contributions of air to the signals at  $m/z=29$ ,  $30$  and  $31$  were first determined using fully aerated buffer injections and Peakfit analysis. Once these contributions were standardized, the  $m/z=29$  trace in the samples was inspected for air signals which were analyzed with Peakfit for amplitude and shape. This information together with the scaling factors obtained with aerated standards allowed us to estimate the anticipated amplitude and shape of air contributions at  $m/z=30$  and  $31$ . Once those contributions were subtracted from the data in all three traces the ripple subtraction and signal analysis proceeded as outlined above.

Together, the adjustments made to the flow through the purge vessels and to the MSD analyzer increased our overall signal to noise ratio by nearly one order of magnitude. Figure 7 demonstrates the increased sensitivity achieved when all enhancements described above were implemented. The results show that signals as low as 3 picomoles could be quantified using the ascorbic acid assay. Similar performance (data not shown) was achieved using the tri-iodide based assay. Although the adjusted values quoted here are largely specific for the mass spectrometer model we use, it suggests that similar adjustments when implemented with other models could likely result in significantly enhanced performance.

### **Isotopic detection in J774 cells**

There is currently much interest surrounding the biological activity and therapeutic uses of nitrite, an oxidative product of NO synthesis that until recently was regarded as biologically inert (Gladwin et al., 2005). The interest in this anion has been intensified further with recent evidence that mammalian tissues can reduce nitrate to nitrite through the action of xanthine oxidase (Jansson et al., 2008), an enzyme that plays a significant role in the immune system.

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Since macrophages are part of that system and constitutively express this enzyme, we sought to explore whether these cells are able to reduce  $^{15}\text{NO}_3^-$  (nitrate) to  $^{15}\text{NO}_2^-$  (nitrite) using our mass selective technique.

A representative set of data from our mass selective experiments is shown in the top panel of Figure 7. The hatched gray zone around the horizontal axis represents our limit of detectability, i.e. the area where measurements essentially correspond to baseline fluctuations. Following J774.2 cell homogenization, samples were kept aerated at 37°C as 100 µl volumes were drawn periodically and injected into an ascorbic acid based nitrite assay. Each column in the Figure represents the average of three injections performed over a period of 20 minutes following 10 minutes of Ar purging, for a total of 30 minutes. The gray and white columns in the top panel of Figure 7 show the levels of  $^{14}\text{NO}_2^-$  and  $^{15}\text{NO}_2^-$ , respectively, before and after addition of 100 µM  $^{15}\text{NO}_3^-$  to the lysate at the 90 minute mark. The data shows the emergence of  $^{15}\text{NO}_2^-$  only after addition of  $^{15}\text{NO}_3^-$ , consistent with the notion that J774.2 cells should exhibit nitrate reductase activity. Similar experiments performed with control culture flasks incubated without J774.2 cells, confirm that the  $^{15}\text{NO}_3^-$  reduction is obtained only in the presence of cells. The lower panel of Figure 7 compares results obtained for  $^{15}\text{NO}_2^-$  before and after addition of 100 µM  $^{15}\text{NO}_3^-$  to lysates, for Ar-purged and un-purged samples. These results demonstrate that the nitrate reductase activity of J774 cells is potently inhibited by oxygen.

In addition to the signals obtained for  $^{15}\text{NO}_2^-$ , the upper panel of Figure 7 illustrates the artifactual progressive increase in the  $^{14}\text{NO}_2^-$  signal usually seen when a biological sample or culture media is purged with an industrial grade gas that has not been scrubbed with NaOH. The increase was not observed in our standards or PBS alone. This phenomenon is attributed to hydrolysis of NO<sub>x</sub> species present in the purge gas, which interestingly seems to be potentiated by the presence of biological material in the sample. The ability of our system to discern isotopically nitrate-to-nitrite reduction from other reactions that produce nitrite only demonstrates the advantage of using isotopic tracing methods to characterize sources of NO signaling.

## Discussion

The current work demonstrates that mass spectrometric detection can be successfully incorporated into NO chemiluminescence assays with relative ease to provide isotopic tracing capabilities. The system described here places an MS detector in parallel with an NO chemiluminescence detector mainly to validate our findings, but the MS detector could have easily been used as the sole detector in the system if desired. The limit of detection for both  $^{14}\text{NO}$  and  $^{15}\text{NO}$  is on the order of a few pmol using the MSD option, rendering it nearly as sensitive as chemiluminescence detection. Tests with cell homogenates indicate that these detection limits are also attainable in with biological samples.

The present technique offers advantages and imposes limitations that should be considered carefully before adopting it. The main advantage of our MS based technique is its direct compatibility with chemiluminescence based NO assays, which not only allows it to use extensively validated chemical assays but also facilitates cross-referencing of results obtained by either technique. The benchtop space requirements and the detector costs are also essentially similar for either technique. Another advantage associated with MS detectors is that their technology has matured to the point of providing turn-key operation and easy servicing steps. Consumable items such as electron impact filaments, detector horns, capillary columns, are widely available through a variety of vendors at competitive pricing. Compared to costlier and more labor-intense GC/ Negative Ion Chemical Ionization MS techniques that rely on derivatization of NO-related products (Tsikas, 2000), the current technique offers the advantage that biological samples can be assessed for nitrite, nitroso, and nitrosyl-heme species within a few minutes and with minimal sample preparation. Finally, unlike laser IR techniques reported to date which enable sensitive detection of  $^{14}\text{NO}$  or  $^{15}\text{NO}$ , but not both simultaneously (Gabler and Lehmann, 2005; Yi et al., 2006; Fritsch et al., 2008), our MS approach is able to cycle between those two detection channels in only a few milliseconds therefore allowing simultaneous detection of  $^{14}\text{NO}$  and  $^{15}\text{NO}$  with equal sensitivity. Laser-based techniques are also significantly costlier than the technique described here.

In terms of disadvantages and limitations, the lowest concentration of NO-related products that can be quantified currently with our technique is on the order of tens of nM assuming that sampling is performed in 100  $\mu\text{l}$  volumes. This level of sensitivity most likely precludes its use for studies of basal nitrosation and heme nitrosylation in small animals (Bryan et al., 2004). Such products may be best studied using GC/MS (Tsikas, 2000) or one of the IR laser spectroscopic methods (Fritsch et al., 2008) alluded to above. Nevertheless the sensitivity of our technique should still be sufficient to trace isotopically other products such as nitrite and nitrate in fluids and tissues of small animals. Another disadvantage is the inconvenience imposed by the additional data processing steps required to subtract the contributions of

dissolved air from the NO signals. In the future, this inconvenience may be minimized through programmed steps using software developed in-house.

Finally, we demonstrated the applicability of the present technique with experiments focused on the detection of nitrate-to-nitrite reduction in anoxic J774.2 cell lysates. When lysates were spiked with  $^{15}\text{N}$ -labeled nitrate, we observed very clearly its reduction to  $^{15}\text{N}$ -nitrite, even as the levels of  $^{14}\text{NO}_2^-$  changed due to other processes. Our analytical system also enabled us to determine that the reduction of nitrate to nitrite was distinctly suppressed in aerated samples. These results suggest that this cellular model combined with our analytical system may hold promise for future characterization of the enzymatic pathways contributing to mammalian nitrate reductase activity.

### Materials and methods

Standard solutions of  $^{14}\text{NO}_2^-$  and  $^{15}\text{NO}_2^-$  were prepared from  $\text{Na}^{14}\text{NO}_2$  and  $\text{Na}^{15}\text{NO}_2$  (Sigma-Aldrich, St. Louis, MO, USA) in 40 mM HEPES or phosphate-buffered saline (PBS) solutions. All samples were bubbled with argon (Ar) for 30 seconds prior to injection to remove dissolved air, which produces some interference at  $m/z = 30$  and  $31$ . They were then injected in  $100\mu\text{L}$  volumes into a 40 mL Sievers reaction vessel containing either tri-iodide (Feelisch et al., 2002) or ascorbic acid based solutions (Nagababu and Rifkind, 2007), in which 1 M HCl was substituted for acetic acid to avoid background interference from the molecular fragments  $\text{CH}_2\text{OH}$  at  $m/z = 31$  (NIST). The tri-iodide solution consisted of 1M HCl at room temperature, to which 10 mg of  $\text{I}_2$  and 300 mg of KI were added. The ascorbic acid solution was prepared from a mixture of 32 ml of 1 M HCl and 4 ml of 0.5 M ascorbic acid maintained at  $37^\circ\text{C}$ . The nitrite specificity of the ascorbic acid/HCl mixture was validated with side by side injections of nitrite, nitrate, and S-nitrosoglutathione (Sigma-Aldrich). The NO formed from the reduction of nitrite was purged out of the reaction vessel with ultrahigh-purity helium (UHP He) and scrubbed through a 1 M NaOH solution, and quantified with our combined CLD/MS detection system described in the following section.

J774.2 cells (Sigma-Aldrich) were grown to near confluence (5-7 days) in T75 flasks with DMEM in the presence of 10% fetal bovine serum (Sigma-Aldrich), penicillin (200 U/ml), and streptomycin (200  $\mu\text{g}/\text{ml}$ ). On the day of the experiment, the cell culture supernatant was aspirated and the adherent cells were washed 2-3 times with sterile PBS. Cells were then collected by scraping using a rubber policeman into 1-2 ml of PBS and lysed using an Ar-pressurized Parr Bomb. The resulting cell lysate was used immediately in experiments. Control flasks were incubated under identical conditions for the same period of time without cells and processed identically to those containing cells. In addition, the media from each of the control flasks were centrifuged in 15 ml tubes, at 1000 g for 60 minutes. The remaining pellet was re-

suspended in 1 ml of PBS and tested immediately.

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## Figure legends

**Figure 1** Diagram highlighting key features of the setup for simultaneous detection of NO products using chemiluminescence and mass spectrometers detectors.

**Figure 2** Analysis of a 100 pmol signal generated with MS detection.

The dots correspond to data points collected directly from the MSD, while the solid curve represents a data fit to an exponentially modified Gaussian over a linearly graded background. Curvefitting is performed with Peakfit which automatically determines optimal parameters for the peak and the background, and automatically calculates the area under the peak.

**Figure 3** Typical MSD tracings extracted for the signals at  $m/z = 29, 30,$  and  $31$ .

The curves illustrate the performance of the system obtained with 1 nmol injections of  $^{14}\text{NO}_2^-$ ,  $^{15}\text{NO}_2^-$ , and of an equimolar mixture of  $^{14}\text{NO}_2^-$  and  $^{15}\text{NO}_2^-$ , all in Ar-purged phosphate-buffered saline solution. The fourth injection illustrates the signals generated by dissolved air in fully aerated buffered solutions. The large peak arises from  $^{14}\text{N}^{15}\text{N}$  (natural abundance 0.73%; see text for details).

**Figure 4**  $^{15}\text{NO}_2^-$  quantification using a tri-iodide assay and standard MS detection conditions (see text).

Top panel: realtime scan of multiple  $^{15}\text{NO}_2^-$  injections of increasing concentration. Middle panel: areas under the curve for the injections shown in the top panel. Lower panel: comparison between the areas under the curve measured simultaneously with MS and CL detection.

**Figure 5** Performance comparison between autotune/high-pressure, manual-tune/low-pressure, and manual-tune/low-pressure/signal-subtraction modes of operation.

All panels show signals obtained at  $m/z=30$  with two injections of 30 pmol of  $^{14}\text{NO}_2^-$  into an ascorbic acid/HCl assay. The upper panel shows barely discernable signals obtained with injections at 5 and 7.5 minutes under autotune/high-pressure conditions. The middle panel exemplifies the enhancement in performance that is achieved with lower pressure and MSD manual tuning. A drawback from this mode of operation is the emergence of ripple in the baseline with a period comparable to that of the signal. The lower panel demonstrates that much of the ripple can be eliminated by subtracting a fraction of the signal at  $m/z=29$  to further enhance the sensitivity of the system.

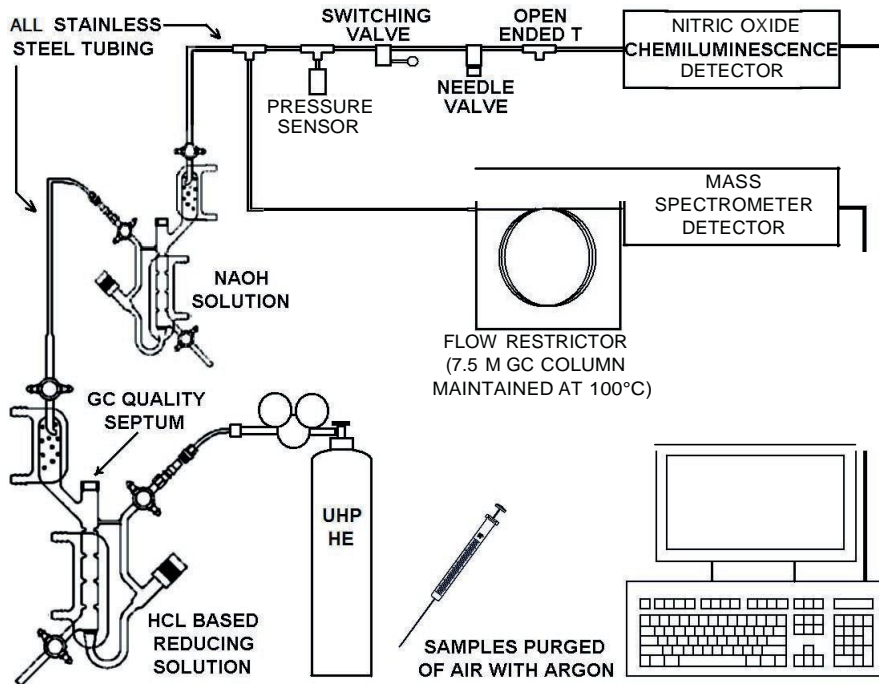
**Figure 6** Quantification of  $^{14}\text{NO}_2^-$  (upper panel) and  $^{15}\text{NO}_2^-$  (lower panel) using an ascorbic acid/HCl assay and enhanced MS detection conditions (see text).

**Figure 7** Mass-selective detection of nitrite from the murine J774.2 macrophage cell line.

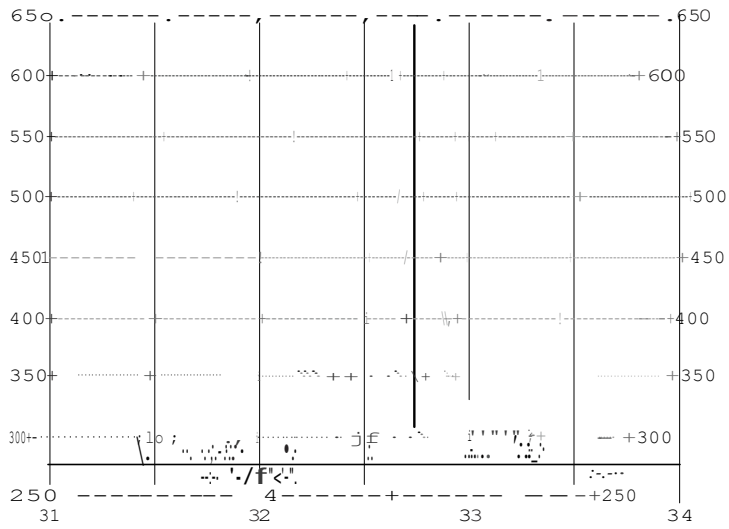
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The gray and white columns in the top panel show the levels of  $^{14}\text{N}\text{O}_2$  and  $^{15}\text{N}\text{O}_2$ , respectively, before and after addition of 100 fM of  $^{15}\text{N}\text{O}_3$  to the lysate at the 90 minute mark. The gray hatched zone around the horizontal axis represents our limit of detectability, i.e., the area where measurements are essentially indistinguishable from baseline fluctuations. The lower panel compares results obtained for  $^{15}\text{NO}_2$  prior to and after addition of 100 fM of  $^{15}\text{N}\text{O}_3$  to lysates, for air-purged samples (white columns) or un-purged (hatched columns),

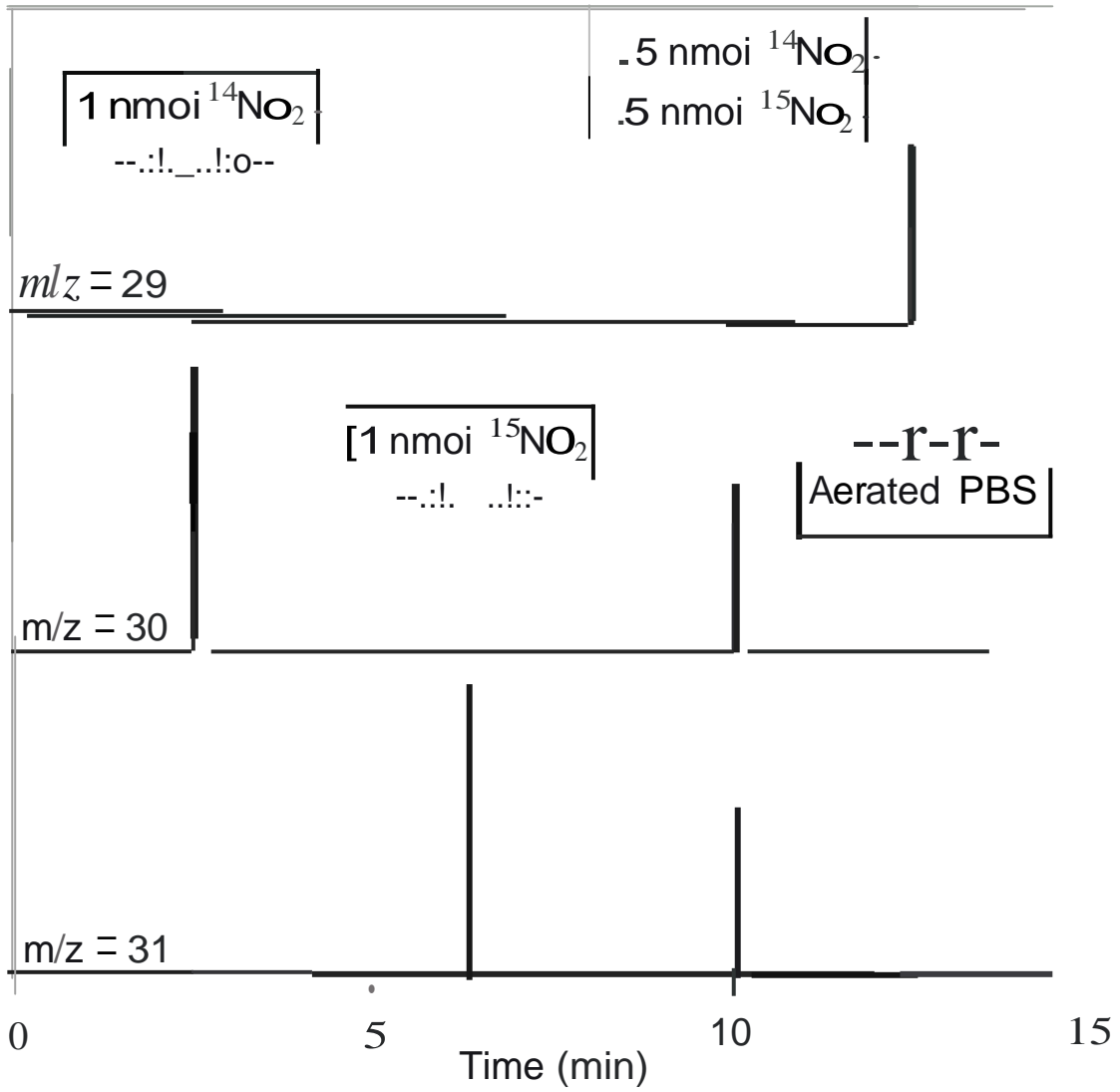
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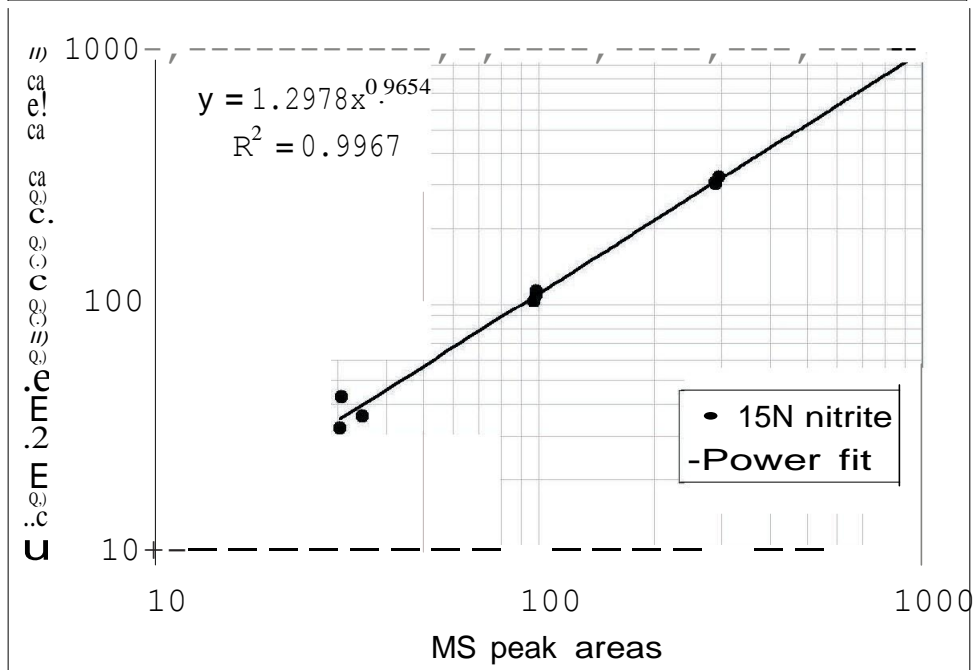
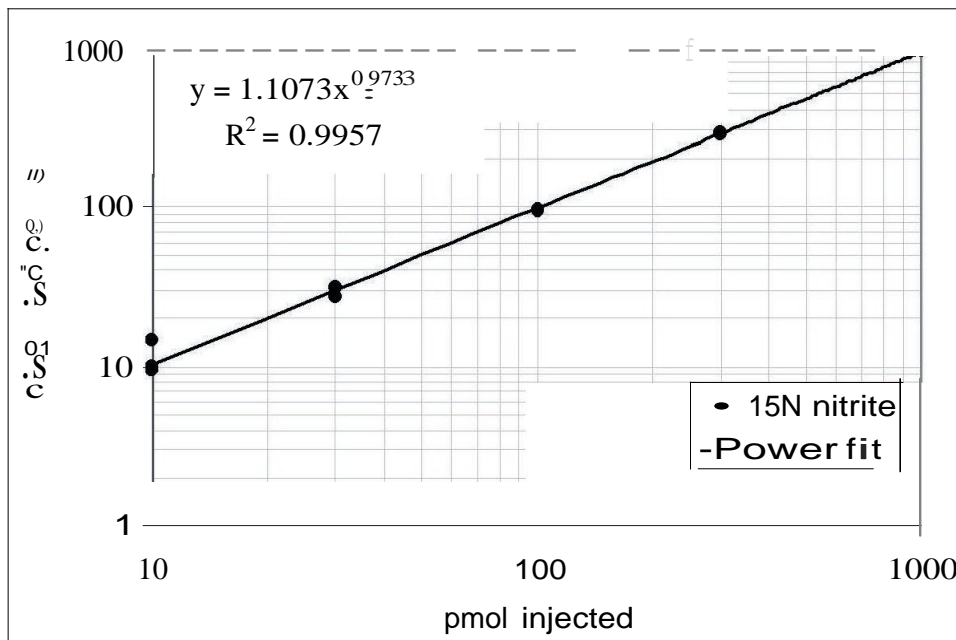
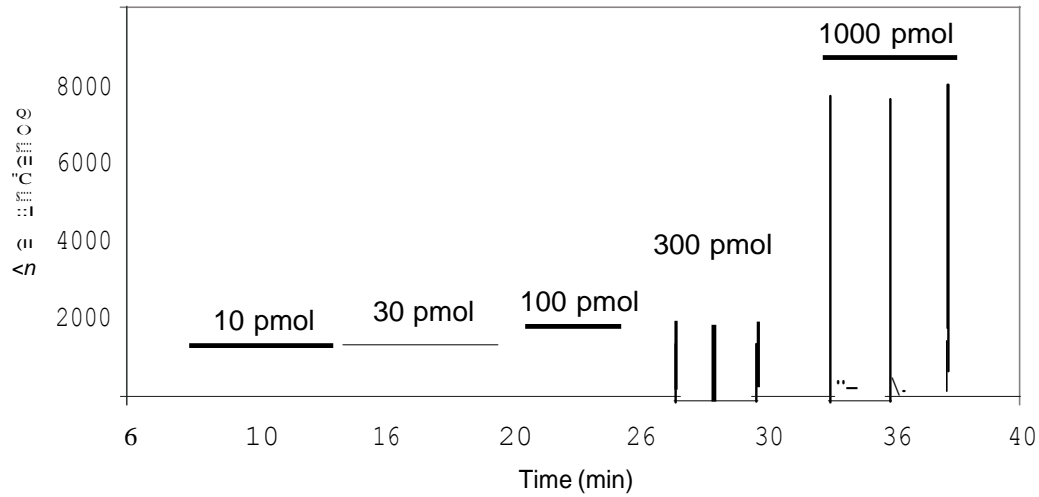
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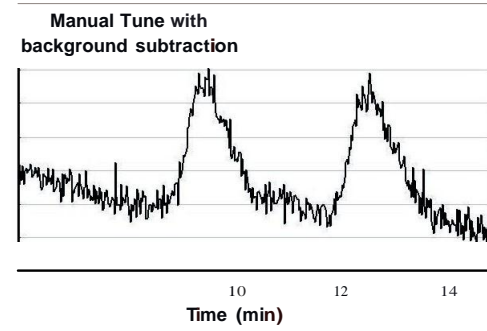
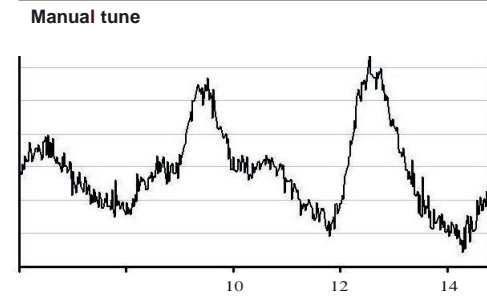
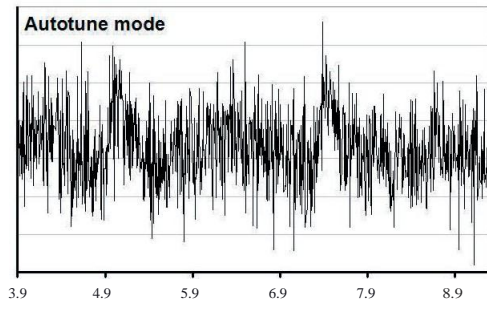
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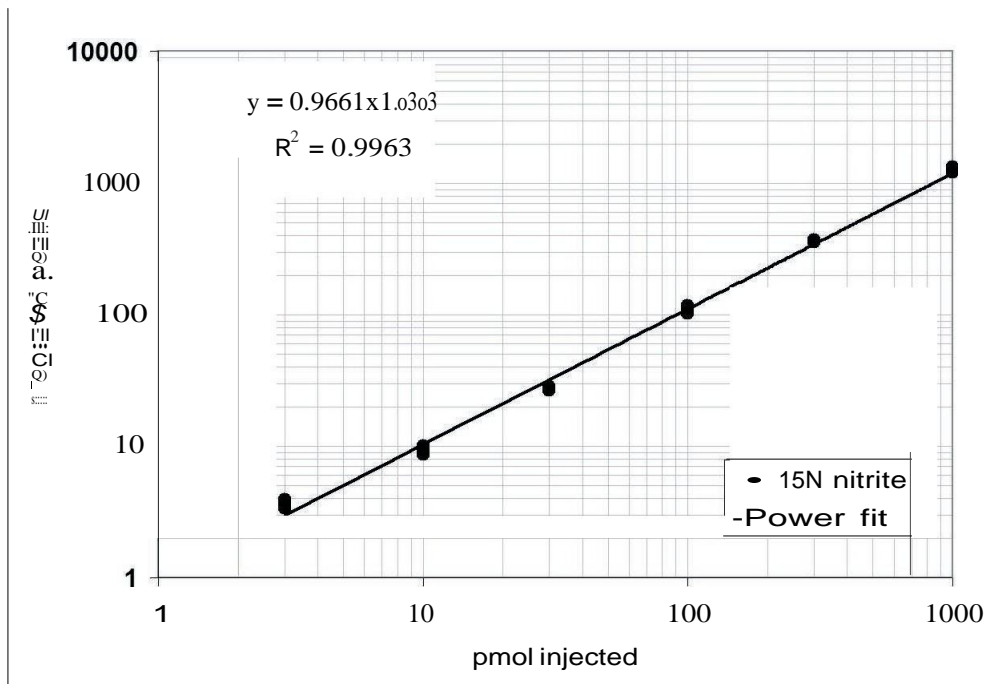
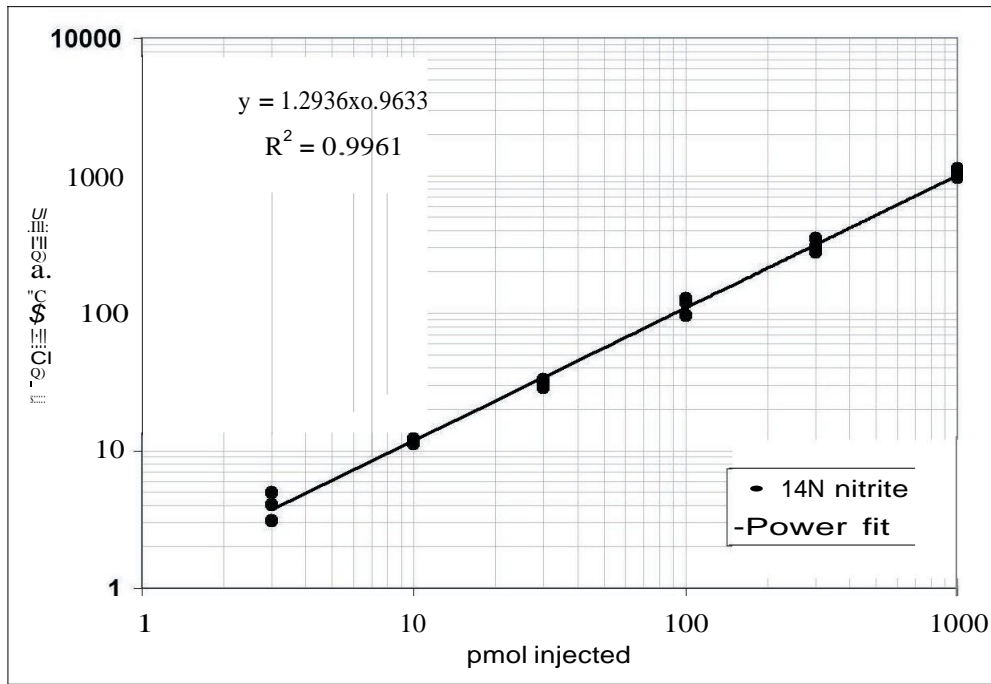
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