

Damage mechanisms at the cement-implant interface of polished cemented femoral stems

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1 ABSTRACT

- The occurrence of damage on polished femoral stems has been widely reported in the literature, and bone cement has been implicated in a tribo-corrosive failure process. However, the mechanisms of cement-mediated damage and the impact of cement formulation on this process are not well understood. In this study, thirteen Zimmer CPT polished femoral stems and corresponding cement specimens were retrieved at revision surgery and analysed using high-resolution imaging techniques. Surface damage attributed to tribo-corrosion was observed on all stems. Corrosion product, in the form of black flaky surface debris, was observed on the surface of cement specimens; both energy-dispersive x-ray spectroscopy (EDX) and inductively coupled plasma mass spectrometry (ICP-MS) confirmed the presence of cobalt and chromium, with the ICP-MS showing much higher levels of Cr compared to Co when compared to the original stem material. Agglomerates of ZrO₂ radiopacifier were also identified on the cement surface, and in some cases showed evidence of abrasive wear; the size of these particles correlated well with elliptical pitting evident on the surfaces of the corresponding stems. This evidence supports the hypothesis that agglomerates of hard radiopacifier particles within the cement may induce a wear-dominated tribo-corrosive interaction at the stem-cement interface that damages the surface of polished CoCr femoral stems.
- 19 Keywords: Bone Cement, Implant Retrieval, Failure Analysis, Cobalt-chromium alloys,
- 20 corrosion

1. INTRODUCTION

- 3 Damage to the surfaces of cemented femoral stems has been reported in a number of retrieval
- 4 studies involving a range of stem designs and cement formulations[1-6]. The damage has
- been attributed to abrasion [7], metallic shedding [8, 9], tribo-corrosion [4, 10, 11],
- 6 originating from micromotion between the stem and cement mantle[12], pores at the cement
- 7 surface [13], the radiopacifier and the cement chemistry [10, 14, 15], with the stem design,
- 8 cement formulation and location on the stem affecting the damage mechanisms[16, 17].
- 9 A great deal of work has been undertaken by Bryant et al. [4, 11, 14, 15, 18] to identify the
- origins and drivers of damage, and this has led to the proposal of a fretting-corrosion
- mechanism[18]. The mechanism describes how the oxide film on the surface of the CoCrMo
- stem and bone cement are in intimate contact when the stem is inserted. When loaded during
- the stance phase of the gait cycle, the contact pressures on the asperities of the two surfaces
- exceed the yield stress of the oxide film, bone cement and CoCrMo stem, causing oxide film
- fracture, transfer of the oxide to the cement surface and plastic deformation of the cement and
- stem surfaces. During the swing phase of the gait cycle the interface separates, exposing the
- depassivated metal surface to the body fluids enabling dissolution of the metal and the oxide
- film to reform. The repetition of this process results in a build-up of damage on the stem
- surface and an accumulation of the fractured oxide film between the cement and the stem
- 20 surfaces, seen as black deposits and flakes on the stem and cement surfaces. This mechanism
- 21 provides an explanation for the origins of the Cr₂O₃ film. However, the detailed analysis
- focused on the tribo-film and surface of the stem with no review of the cement surface and
- the mechanism stops short of explaining how the comparatively soft PMMA bone cement

- 1 (0.32GPa) can plough and plastically deform the surface of a hard CoCrMo alloy (6.0
- 2 GPa[19]).

- 3 The aim of this study was to conduct a detailed forensic examination of a selection of femoral
- 4 stems and the corresponding proximal cement mantles of failed large diameter MOM THA,
- 5 in order to investigate cement-mediated damage mechanisms at the cement-implant interface
- 6 of polished femoral components.

2. MATERIALS AND METHODS

- 8 Twelve Zimmer CPT polished, collarless tapered cobalt-chrome femoral stems, implanted
- 9 between 2002 and 2007, were retrieved during revision surgery. The implants were hybrid
- modular THA with cemented femoral components, both from mixed and matched
- manufacturer stem and head combinations, as described previously by [5]. Indications for
- 12 revision included adverse local tissue reactions (ALTR) aseptic loosening, pain and raised
- serum concentration of cobalt (Co) and chromium (Cr) ions. Time *in* vivo ranged from 52-97
- months. Detailed characteristics for each retrieved femoral stem are given in Table 1.
- Fragments of acrylic bone cement were retrieved for eight stems. Cement was collected from
- the proximal region of the cement mantle (corresponding to Gruen Zones 1 and 7), and were
- associated with both macroscopically damaged and undamaged surfaces of the stem; to avoid
- 18 artefacts arising from instrument damage only cement that was easily removed was included
- in the study. In the cases of high levels of damage the cement surfaces were covered with a
- 20 layer of black deposit. In each case, the retrieved cement was either vacuum-mixed Palacos
- 21 R40G (Schering Plough, Welwyn Garden City, UK) or Biomet Palacos (Biomet UK Ltd,
- 22 Bridgend, UK); these are poly(methylmethacrylate/methylacrylate) (PMMA) based
- formulations containing approximately 15% w/w zirconium dioxide (ZrO₂) radiopacifier and

- 1 a variable amount of gentamicin sulphate in the powder component(depending on the
- 2 manufacturer).
- 3 Femoral stems were imaged using an Alicona InfiniteFocus microscope (Alicona Imaging
- 4 GmbH, Graz, Austria). The technique uses optical microscopy and focus variation technology
- 5 to extract 3D morphology and depth information from the surface with a resolution of 10 nm.
- 6 Cement fragments were imaged using a JEOL JSM6500F field emission gun scanning
- 7 electron microscope (SEM) (JEOL USA Inc. Peabody, MA). Specimens were sputter-coated
- 8 with a thin layer (~15 nm) of gold prior to imaging. A low accelerating voltage (5-10 kV)
- 9 was employed in order to minimise artefacts arising from beam-induced polymer
- degradation, and imaging at very high magnifications (> 5000 x) was interpreted with
- caution. Elemental analysis of the surface of the cement specimens was conducted using
- 12 energy-dispersive x-ray spectroscopy (EDX).
- 13 A sample of the black deposit on the surface of one of the cement samples was removed
- using tweezers. The sample was weighed in a Teflon digestion vessel and subjected to a
- sequential digestion in concentrated HCl at 130°C overnight, followed by a concentrated
- 16 HNO₃/HF at 130°C overnight and finally an Aqua Regia digest at 130°C overnight. Despite
- 17 this aggressive digestion, a small amount of solid dark residue remained in the base of the
- digestion vessel. This residues was investigated using EDX and shown to contain Cr and Fe
- 19 (although the amount of material was too low and too fine-grained to obtain quantitative
- data). The dissolved samples were then evaporated to dryness and redissolved in 3% HNO₃
- 21 spiked with 20ppb Be and 5ppb of In and Re to act as internal standards. Mass Spectroscopy
- was carried out using a X-SERIES 2 ICP-MS (Thermo Fisher Scientific, Bremen, Germany).
- Data was acquired for all isotopes of interest in peak-jumping mode (4 x 30 second repeats
- per sample). After each sample analysis, a wash solution containing 3% HNO₃ was run until

- 1 background levels were achieved. The raw data was blanked and internally corrected and
- then calibrated against synthetic standards (Inorganic Ventures, Virginia, USA).
- 3 3. RESULTS
- 4 Stem Surface
- 5 The location and severity of damage varied between stems. All stems showed evidence of
- 6 macroscopic material loss on the posteromedial aspect, ranging from one or two isolated
- 7 spots a few millimeters in diameter, to extensive patches extending to the under neck region,
- 8 as shown in Figure 1.Damaged regions were also frequently observed on the anterolateral
- 9 regions of the stems, and occasionally on the anterior face. Surface deposits, in the form of
- 10 black or brown plaques, were also noted.
- Microscopically, the appearance of damaged regions at the proximal end of the cement stem
- 12 interface was indicative of fretting corrosion (Figure 2). Extensive deformation and damage
- of the stem surface was noted, with 'islands' of apparently undamaged material. Damaged
- 14 regions occurring on the medial side of the posterior surface frequently demonstrated a
- unidirectional alignment, approximately 45° to the long axis of the stem (Figure 2).
- 16 Cement Surface
- 17 Fragments of the full thickness cement mantle were obtained. The surface of the cement in
- 18 contact with the stem was easily identified by the presence of a typically smooth, uniformly
- 19 flat or curved surface (Figure 3a) and/or black deposits with a flaky appearance(Figure 3b).
- The green colouring of the cement is consistent with the formulation of Palacos R+G due to
- 21 the addition of chlorophyll.

- 1 Examination of bone cement fragments using SEM demonstrated differing degrees of
- 2 damage at the cement surface according to the region of contact with the stem. Agglomerates
- 3 of zirconium dioxide (Zr0₂) particles, typically 5μm in diameter and with a cauliflower-like
- 4 appearance, were visible within the cement; the identity of these agglomerates was verified
- 5 using EDX. The undamaged regions showed evidence of micropores at the surface of the
- 6 cement (Figure 4). EDX within the pores showed evidence of ZrO₂ particles (Figure 4).
- 7 On the moderately damaged regions of the cement (Figure 5) both radiopacifier and metallic
- 8 debris were identified via EDX. Although traces of Co and Mo were noted, Cr was found to
- 9 be the dominant metallic species. Inspection of the highly damaged regions showed the ZrO₂
- agglomerates standing proud from the underlying cement (Figure 6a, b), with the surfaces of
- the agglomerates flattened (Figure 6c, d); the cement also appeared to have been abraded,
- with evidence of directional wear (Figure 6a).
- 13 The sample of corrosion product analyzed by ICP-MS identified a number of metallic
- 14 elements within the corrosion product (Table 2). Comparison of the three main elemental
- 15 constituents of the stem, i.e. Cr, Co and Mo, revealed a very high concentration of Cr in the
- 16 corrosion product, ten times greater than the concentration of Co, while the Mo concentration
- was found to be negligible.

19 4. DISCUSSION

- 20 This study is the first to review the surface of retrieved bone cement from THRs and relate it
- 21 to the damage seen on the corresponding femoral stem components. The location and
- morphology of the damage to the femoral stem components in this study is in keeping with
- that of previous retrieval work. The major regions of material loss were on the posterior and

medial sides of the implants, with directionality to the deformation within Gruen zones 1 and 7 in agreement with the findings of previous studies [2-4]. The directionality in the damage is a reflection of the motion and peak loading between the cement and the stem in-vivo [20] and provides evidence for the tribocorrosive damage having a primarily mechanical origin. Examination of the retrieved cement surfaces has highlighted that the radiopacifier may have a more detrimental role than previously hypothesized in the damage seen at the proximal end of the cement-stem overlap. Howell et al. 2004[3] found no significant difference between the presence of radiopacifier in the cement and the stem wear score, although the number of stems with radiolucent cement in the study was comparatively small. Zhang et al. 2012 [17] did a comparative study between 3 different cements (Simplex P, Palacos R and CMW 3) and demonstrated no significant difference in the stem surface damage generated by the different cements. The study attributed the damage to their previous hypothesis [13, 17, 21-24] that it was the pores at the interface which initiated the damage. However, the EDX traces of voids demonstrated the presence of radiopacifier particles as observed in this study, but it was not commented upon by the authors[17]. The study also hand mixed the cement in a bowl, which is likely to have introduced a higher density of voids compared to the standard vacuum mixing method used clinically to produce the cement reviewed in this study. These observations were used as a justification by Bryant et al. [4, 11] to rule out the radiopacifier as having an abrasive effect. The undamaged regions of the cement within this study revealed voids at the stem cement interface. The origins of these voids are not clear, but as the cement was vaccum mixed, they are likely due to shrinkage during the curing of the cement after insertion. Investigations of the surface voids in this study showed the presence of radiopacifier particles in the voids and

in close proximity to the surface. However there was no damage on the stems of this study

- which matched the reported damage patterns presented by Zhang et al.[13, 17, 21-24] and
- 2 Blunt et al.[25].
- 3 The cement from the areas of high stem surface damage had rough surfaces with zirconium
- 4 dioxide radiopacifier agglomerates not only protruding from the surface, but also worn flat.
- 5 The hard, abrasive radiopacifier agglomerates would have been in direct contact with the
- 6 stem surface and would have had the ability to plough and plastically deform the stem
- 7 surface, disrupting the passive oxide film and repassivation process, increasing the
- 8 susceptibility to corrosive attack.
- 9 The ICP-MS analysis of the corrosion product in this study showed the presence of a range of
- ions, with the majority of trace elements from the CoCrMo alloy of the stem. The ICP-MS
- analysis results show that the make-up of the film was 90.3% Cr, 9.3% Co, 0.11% Zr,
- 12 0.007% Mo with the rest of the elements making up the difference. The result implies that the
- film is Cr rich, with evidence of the radiopacifier within the film. These findings are
- consistent with the compacted Cr₂O₃ film seen in the analysis performed by Bryant et al.
- 15 (2014) [15]. The detailed compositional analysis conducted in their study only considered the
- metallic species associated with the stem alloy and signs of protein, and didn't look for
- evidence of the barium sulphate radiopacifier within the film. However, their earlier work
- 18 [11-12] highlighted that the cement chemistry, particularly sulphates from the BaSO₄
- 19 radiopacifier, can enhance corrosion of the stem surface. The disparity between the level of
- 20 Co in the film compared to the 60-70% Cobalt content of the stem alloy is linked to the
- thermodynamic stability of the species within the cement stem interface. The study by Lewis
- 22 et al. [24]investigated the effects of different fluids on the dissolution and corrosion of
- CoCrMo alloys. The study provided values of the Gibb's free energy (ΔG^{o}) for the formation
- of Cr₂O₃, Cr(OH)₃ and CoO as -1058, -984 and -214 kJmol-1 respectively. The more negative

- 1 the ΔG^{o} the more thermodynamically favorable the reaction and hence the chromium remains
- 2 in the interface, reforming the oxide film, while the Co ions are removed in solution. The
- 3 study also reviewed the effects of proteins on the corrosion by looking at the first equilibrium
- 4 constants (K) for the polydentate ligand EDTA, the values for Co and Cr were $K_{Cr} = 2.5 \text{ x}$
- 10^{23} and $K_{Co} = 1.2 \times 10^{16}$, indicating that Cr ions are more likely to complex with proteins
- 6 than Co. This was demonstrated experimentally by Clark and Williams [25] using metal
- 7 powders; the presence of protein increased the corrosion rate of cobalt and chromium by 30
- 8 to 40 times and 2 to 4 times respectively, with the metals forming protein-metal complexes.
- 9 On the basis of the present work, a new mechanism is proposed for the proximal surface
- damage. After implantation the stem sits within a close fitting cement mantle. The initial
- loading of the implant results in the stem sinking into the cement mantle and the formation of
- hoop stresses which hold the stem in the mantle. This initial sinking can range from 0.32-
- 13 1.2mm over 2 years depending on the stem design [26]. The surface finish of the stems is
- polished, but there is a roughness (Ra) of 0.1 µm and between the sinking in and the millions
- of loading cycles resulting in micromotion at the interface, the 0.1 µm CoCrMo asperities on
- the stem wear and deform the PMMA cement surface. This process results in the subsurface
- 17 radiopacifier agglomerates within the cement reaching the surface and forming asperities
- 18 similar to those observed on the retrieved cement surfaces in this study. These asperities are
- 19 harder (12-13 GPa) than the CoCrMo surface (6.0 GPa), and the subsequent cyclical
- 20 micromotion results in regular depassivation and deformation of the stem surface.

21 5. CONCLUSIONS

- This study investigated the surface of retrieved bone cement in relation to the damage seen on
- 23 matched retrieved stems. The retrieved cement surfaces all showed evidence of radiopacifier
- 24 agglomerates protruding from or at the surface which was in contact to the stem. The ICP-MS

- 1 results indicate that a tribocorrosive mechanism was the cause of the damage to the stems,
- 2 however, the depassivation and plastic deformation of the stem surface is attributable to
- 3 micromotion between the radiopacifier agglomerates and the stem surface.

4 6. CONFLICT OF INTEREST

- 5 Jeremy Latham is a consultant for Zimmer, DePuy and Lima LTO
- 6 Richard Cook has undertaken paid consultancy for Biomet

7 7. ACKNOWLEDGEMENTS

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- 10 All data supporting this study are openly available from the University of Southampton
- 11 repository at http://dx.doi.org/10.5258/SOTON/393917

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Table 1: Patient and implant characteristics

Number	Femoral Head	Patient age at primary	Patient gender	Indication for primary	Time in vivo (months)	Indication for revision	Stem Loose at Revision?	Cement obtained?	Blood Co (nmol/L)	Blood Cr (nmol/L)
1	BHR	64	M	OA	56	Aseptic loosening, lesser troch fracture	Yes	No	159	111
2	BHR	70	M	OA	86	Aseptic loosening. Raised metal ions	Yes	No	177	129
3	BHR	44	F	Dysplasia	80+	pain + raised metal ions	No	Yes	61	23
4	BHR	68	F	OA, dysplasia	85	pain + raised metal ions	Yes	Yes	218	191
5	BHR	68	M	OA	89	pain + raised	No	No	168	66

						metal ions				
6	Adept	57	F	OA, dysplasia	52	pain + raised metal ions	No	No	72	113
7	Adept	60	M	AVN	81	pain + raised metal ions	Yes	Yes	191	256
8	BHR	74	F	OA	94	Pain + recurrent troch bursitis	No	Yes	79	40
9	BHR	56	F	OA	97	pain + raised metal ions	No	Yes	185	151
10	BHR	59	F	Unknown	96	Pain	No	Yes	159	111
11	BHR	79	F	Unknown	88	Pain + raised metal ions	Yes	Yes	177	129
12	BHR	69	F	Unknown	69	Pain	No	Yes	70	32

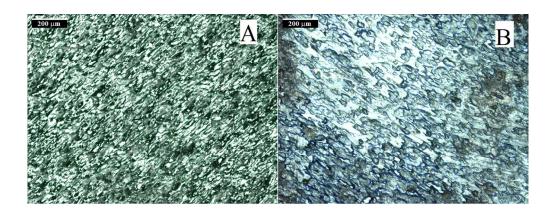
Table 2. ICP-MS results from the corrosion product of stem 8

Element	Cr	Со	Zr	Mn	Fe	W	Mo
Concentrati on (ppm)	114000	11700	142	103	97.2	17.2	8.5





Figure 1: Photographs of the posterior and medial views of two stems demonstrating the variation in severity of damage to the stem surfaces 72x73mm (300 x 300 DPI)



Optical micrographs of damage to stem 4 (A) and stem 8 (B) surface showing directionality to the proximal surface damage.



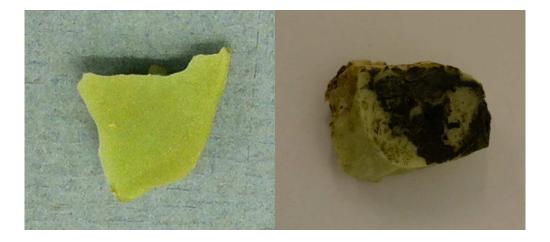


Figure 3: a) Cement fragment from a region of low cement and stem damage showing a smooth and uniformly flat surface b) Cement fragment from a high damage region with corrosion product visible on the surface of the cement.

211x92mm (300 x 300 DPI)



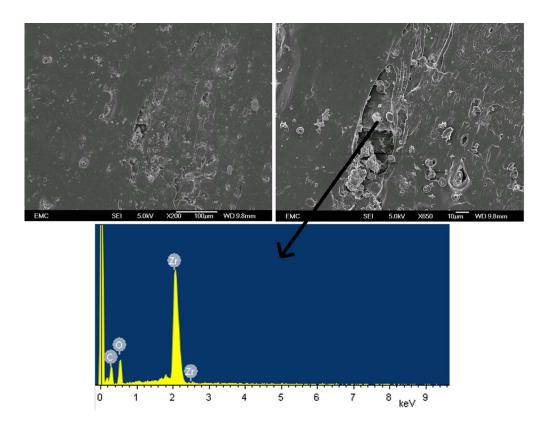


Figure 4: SEM and EDX demonstrating the presence of zirconium dioxide particles within the surface voids of the undamaged regions of the cement $97x75mm (300 \times 300 DPI)$

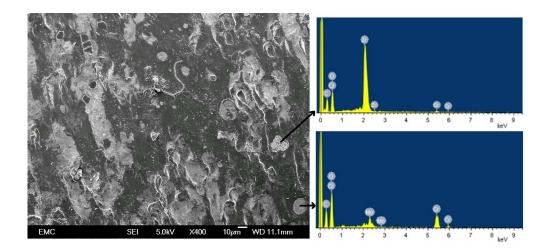


Figure 5: SEM and EDX of the moderately damaged cement surface showing deformation of the cement and the presence of ZrO2 particles and transferred Cr and Mo 192x89mm (300 x 300 DPI)



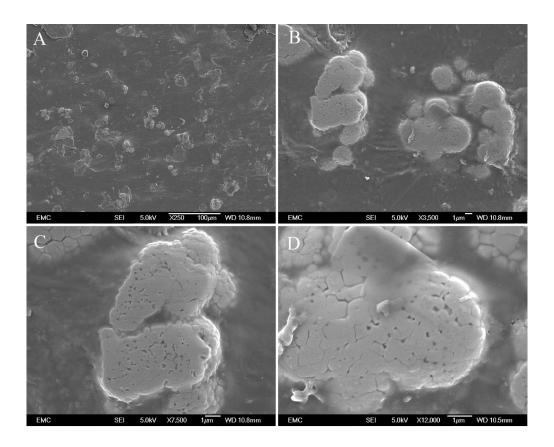


Figure 6: SEM micrographs the cement surface from a highly damaged stem, showing the ZrO2 particles protruding from the surface of the cement. Images are increasing magnification of the same particle A: x250 magnification, B: x3500 magnification, C: x7500 magnification, D: x12500 magnification 217x175mm (300 x 300 DPI)