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Augmentation of musculoskeletal regeneration: role for pluripotent stem cells

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The rise in the incidence of musculoskeletal diseases is attributed to an increasing ageing population. The debilitating effects of musculoskeletal diseases, coupled with a lack of effective therapies, contribute to huge financial strains on healthcare systems. The focus of regenerative medicine has shifted to pluripotent stem cells (PSCs), namely, human embryonic stem cells and human-induced PSCs, due to the limited success of adult stem cell-based interventions. PSCs constitute a valuable cell source for musculoskeletal regeneration due to their capacity for unlimited self-renewal, ability to differentiate into all cell lineages of the three germ layers and perceived immunoprivileged characteristics. This review summarizes methods for chondrogenic, osteogenic, myogenic and adipogenic differentiation of PSCs and their potential for therapeutic applications.

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Socioeconomic burden of musculoskeletal deterioration

Non-communicable disorders affecting the musculoskeletal system are a major cause of disability and morbidity. A decline in the function of bone, muscle and joint tissues is currently an inescapable consequence of ageing. Due to improved healthcare, longevity has increased; however, while lifespan has improved, a corresponding increase in healthy ageing has not been achieved. As a result, the incidence of musculoskeletal disorders has risen [1]. This has contributed to a huge financial strain on the healthcare systems, as well as on affected individuals [2]. The side effects of these disorders, such as intense and often chronic pain, coupled with decreased mobility, have a dramatic impact on the individual's quality of life. Current surgical and pharmacological treatments are limited in their efficacy [3-6]. Furthermore, the subsequent progressive deterioration of the musculoskeletal system results in an increased risk of falls and fractures [7,8]. The natural healing of fractures is often poor in the older population, and carries a higher risk of mortality [9]. Effective treatments for musculoskeletal disorders are therefore necessary to improve the quality of life of our ageing population, and decrease the burden placed on the healthcare system.

Current interventions for the treatment of major musculoskeletal diseases & their limitations Osteoarthritis

Osteoarthritis (OA) is the most common joint disease among older adults [10], with a high global prevalence [11] (Table 1). While the percentage of global prevalence remained constant between 1990 and 2010, the years of life lived with disability increased dramatically. Thus, demonstrating the impact of increased lifespan without a corresponding improvement in health span. OA is caused by the degradation of hyaline articular cartilage and the abnormal remodeling of the joint tissues, which results in loss of joint function. Cartilage is avascular, has low cellularity and, therefore, a limited capacity for repair. Daily wear and tear or injury leads to the structural deterioration of articular cartilage at the joint surface. The early stages of OA are characterized by the formation of partial thickness chondral defects. If left untreated, the defects will extend into the marrow spaces of subchondral



Disease	Incidence/risk	Treatments	Drawbacks
OA	 Worldwide incidence of knee OA estimated at 3.8%, and hip OA 0.85% [11] 	Total joint replacement	Carries some degree of risk [13], late-stage intervention treatment
	 Lifetime risk of developing symptomatic knee OA ~40% in men and ~47% in women, with higher risk for obese individuals [30] 	Reparative techniques: • Abrasion arthroplasty [14] • Debridement [15] • Microfracture [16]	Limited repair, and typically results in fibrocartilaginous tissue
		Restorative techniques: • Mosaicplasty • ACI [18] • MACI	Invasive procedure to procure chondrocytes, limited cell number, dedifferentiation during monolayer expansion, expensive, only recommended for patients with knee OA with no previous treatments, fibrocartilaginous tissue [31,32]
ОР	 Estimated 22 million women, and 5.5 million men being affected within the EU [19] Worldwide, OP results in over 8.9 million fractures each year 	Pharmacological agents: Antiresorptive: Oestrogen Selective oestrogen receptor modulators Bisphosphonates Denosumab Anabolic: Full-length parathyroid hormone (PTH1-8) Teriparatide (PTH1-34) Strontium ranelate Other: Calcium Vitamin D	Long-term administration is required, which can lead to poor compliancy Recommendation of taking bisphosphonate 'drug holidays' to reduce long-term adverse events can reduce benefits gained during treatment periods [33]
Myopathies	 4.6% of men and 7.9% of women with a mean age of 67 in an English cohort study were diagnosed with sarcopenia [25] 	Resistance exercise [35]	Poor adherence, difficulty to carry out without assistance due to inherent frailty of sufferers
	• Duchenne muscular dystrophy affects 1 in 3500 males worldwide [34]	Corticosteroids [36]	Delays symptoms only, multiple known severe side effects [36]
		Genetic interventions [37]	Large organ to treat. Need to target skeletal and cardiac muscle. Limited success [37]

bone, giving access to bone marrow stem cells (BMSCs). The repair tissue formed by infiltrating BMSCs is typically fibrous rather than hyaline [12].

Effective treatments for OA are currently lacking (Table 1). Total joint-replacement surgery is widely used, however, the surgeries carry significant risks that increase with patient age [13] and are a late-stage treatment option. Early-stage interventions are available and focus on initiating cell-based repair. Reparative techniques such as abrasion arthroplasty [14], debridement [15] and microfracture [16] aim to encourage infiltration of stem cells from the marrow spaces of the underlying subchondral bone, to stimulate repair of the damaged tissue. Restorative techniques such as mosaicplasty [17] involve removing cartilage plugs from non-load-bearing regions of the joint and implanting them into the osteochondral defect zone. Another restorative surgical technique is autologous chondrocyte implantation (ACI) [18]; here, patient-derived autologous chondrocytes are harvested from the non-load-bearing region of the articular cartilage, expanded in monolayer culture and implanted at the site of the defect underneath a periosteal flap. This technique often utilizes a collagen scaffold to support the implanted cells and is referred to as matrix-assisted ACI (MACI). Following recently published NICE guidelines (4th October 2017), ACI is now a recommended treatment; however, patient selection criteria are restrictive. While ACI has been relatively successful compared with other techniques such as mosaicplasty [17], there are a number of drawbacks associated with the treatment (Table 1).

Osteoporosis

Osteoporosis (OP) is a prevalent osteodegenerative disease, with an estimated 22 million women, and 5.5 million men being affected within the EU [19]. Worldwide, it is estimated that OP results in over 8.9 million fractures annually (Table 1) [20].

OP is characterized by skeletal fragility, with the hallmark of low bone mass (T-score of -2.5 and below) or a prevalent radiographic vertebral fracture [21]. OP is caused by a disruption in bone turnover homeostasis, leading to accelerated trabecular bone loss that results in a more porous structure. OP is also associated with an increased fall risk and high incidence of fracture [7]. OP predominantly affects the older population, and with increased fracture risk there is a corresponding increase in the likelihood of morbidity. Unlike OA, there are a number of effective pharmacological treatments available for OP (Table 1). Treatment types can be divided into two categories: antiresorptive and anabolic agents. Antiresorptive treatments reduce bone turnover and preserve bone mineral density (BMD). Anabolic agents stimulate bone formation thereby increasing BMD. It has been shown that a combination of these had a synergistic effect on BMD [22]. While these treatments have been suggested to slow the progression of OP, they fail to offer long-term effective solutions [19] and are associated with multiple severe side effects [23,24], and patients are typically subjected to lifelong administration.

Myopathies

Myopathies (muscular diseases) are another key group of diseases that affect a large percentage of the population [1,2]. A common myopathy is sarcopenia [25] (age-related loss of muscle mass and strength); a disease associated with frailty and has a high incidence in the older population (Table 1). There are also numerous genetic diseases such as muscular dystrophies (MD) [26], for example, Duchene muscular dystrophy (DMD), and limb girdle MD. As with the aforementioned bone and joint diseases, there are limited effective treatments to combat the progression of muscular degeneration. Muscle itself has a resident population of stem cells, known as satellite cells [27]. These cells are responsible for the regeneration of muscle fibers following exercise or injury. However, the satellite cell-mediated repair mechanism can become compromised. For example, DMD is characterized by continuous rounds of degeneration and regeneration of muscle fibers that results in a depletion of the muscle stem cell pool [28], leading to a loss of skeletal muscle mass. Currently, there are no approved drugs that consistently result in an increase in both muscle mass and strength making treatment for myopathies extremely limited [29].

Challenges for musculoskeletal regeneration strategies harnessing adult stem cells

There is a clear paucity in the current available treatments for musculoskeletal diseases, and while for some diseases such as OP, pharmacological interventions have been shown to provide some patient benefit, there is an overall need for improved treatments. Stem cell therapy has emerged as a potential treatment option for a plethora of diseases. However, stem cell therapies are not yet offered as routine treatments for musculoskeletal diseases by health services. Stem cell treatment for musculoskeletal disorders typically utilizes adult stem cells (ASCs; Figure 1) such as bone marrow stromal tissue-derived mesenchymal stem cells (MSCs; synonymously referred to as skeletal stem cells) and satellite cells/myoblasts [38,39]. These SCs are multipotent and, therefore, have a broader treatment potential compared with somatic cells. One of the most widely researched cell types for stem cell therapy are MSCs; these can be obtained from a number of different sites (bone marrow, adipose tissue, muscle, dental pulp and umbilical cord blood) [40] with relative ease, making them a favorable candidate for cell therapy. They are also able to differentiate into many major cell types of the musculoskeletal system due to their mesodermal origin [41]. However, heterogeneity between MSCs from different donors is high [42] as demonstrated by variability between growth properties and osteogenic potential; furthermore, their capacity to proliferate and differentiate declines considerably with increasing patient age [43,44]. MSCs are also considered to have an immunomodulatory capacity, and there is evidence to suggest that in vivo their primary function is modulation of repair rather than differentiation into tissue-specific cells, which then contribute directly to tissue regeneration [45].

Injection of undifferentiated MSCs into patients suffering from OA has been shown to improve joint motion and decrease pain [46]. However, another study reported that benefits are transient and that long-term amelioration of the condition is not achieved [47]. Also, MSCs undergoing chondrogenic differentiation (*in vitro*) have a propensity to become hypertrophic, expressing markers such as type X collagen and alkaline phosphatase [48,49]. Stem cell-based therapies for diseases such as DMD have been prominent research areas for many years. The first stem cell transplant into a DMD patient was performed in 1990 using myoblasts and held great promise for this type of treatment due to the apparent safety of the procedure, and the production of dystrophin (the affected protein in DMD) following



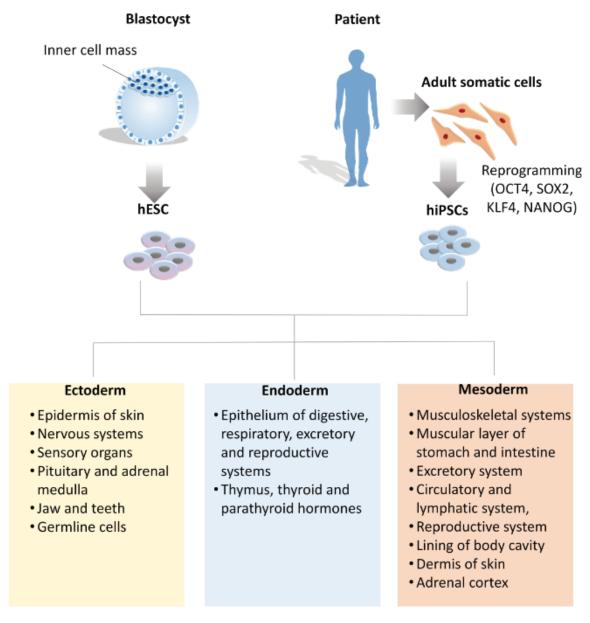


Figure 1. Benefits and drawbacks of using adult stem cells and pluripotent stem cells for clinical applications. Comparison of the advantages and disadvantages of BM-MSCs, hESCs and hiPSCs for application in regenerative medicine.

BM-MSC: Bone marrow-derived mesenchymal stem cell; hESC: Human embryonic stem cell; hiPSC: Human-induced pluripotent stem cell.

transplantation [39]. However, in subsequent clinical trials, the results were inconsistent, with some, but not all, reporting dystrophin production and no significant clinical benefits [50,51].

While MSC/ASC therapy is an appealing prospect, it is clear that its application is problematic. One major drawback of using ASCs is that in order to prevent an immunological response, the cells must be autologous (patient derived), which can be challenging due to potentially low cell numbers, poor viability due to age and disease state. There is also the potential for donor site morbidity.

Pluripotent stem cells: a promising alternative for musculoskeletal regeneration

It is of significant clinical benefit to develop a method of restoring damaged tissue that maximizes quality of repair and minimizes the risk to the patient. To this end, there has been a surge of interest in the potential of pluripotent

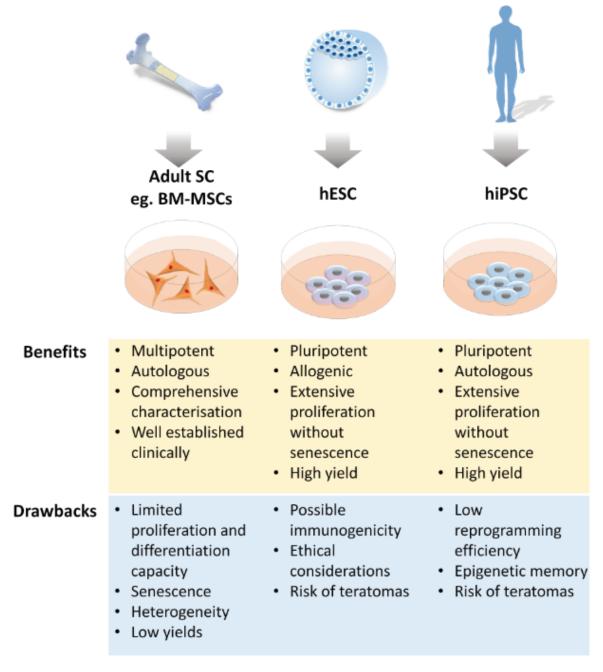


Figure 2. Derivation of pluripotent stem cells and subsequent tissue generation ability. hESCs can be derived from the inner cell mass of a blastocyst at the final stage of preimplantation development. hiPSCs can be reprogrammed from somatic cells using the forced expression of OCT4, SOX2, KLF4, NANOG. These cells can subsequently be differentiated into any derivative of the three germ layers (ectoderm, endoderm and mesoderm). hESC: Human embryonic stem cell; hiPSC: Human-induced pluripotent stem cell.

stem cells (PSCs) for the treatment of skeletal disorders. PSCs have the ability to differentiate into all three germ layers (endoderm, mesoderm, ectoderm; Figure 2) and can, therefore, provide a source for any somatic cell in the body. PSCs can also proliferate indefinitely *in vitro*, without showing signs of cellular senescence. Therefore, PSCs have tremendous potential as a viable source of cells for musculoskeletal repair as they can be differentiated into cells of the mesodermal lineage, and therefore have the potential to generate tissues such as cartilage, bone, muscle and fat for clinical application (Figure 3).

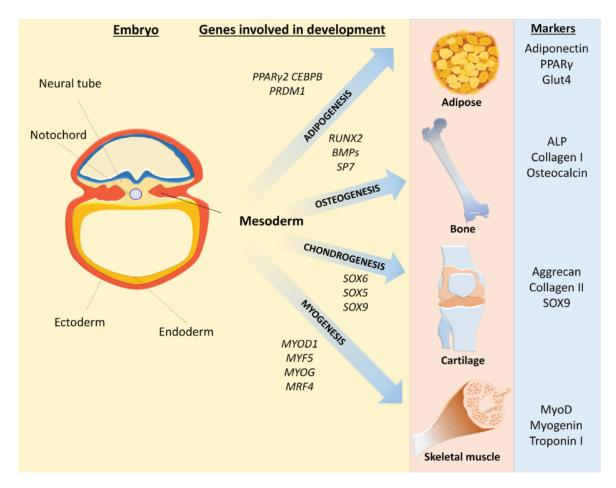


Figure 3. Differentiation of mesoderm into adipose, bone, cartilage and skeletal muscle during development. During embryonic development, the embryo undergoes gastrulation and forms three germ layers: ectoderm, endoderm and mesoderm. The mesoderm gives rise to musculoskeletal tissues via the activation of key genes. In developed tissues, specific proteins can be used as markers.

There are two distinct types of PSCs, embryonic and induced PSCs (iPSCs; Figure 1). Embryonic stem cells (ESCs) are derived from the inner cell mass of the blastocyst [52], and were the only known source of PSC until 2006 when Takahashi and Yamanaka developed a technique of reprogramming somatic cells into iPSCs [53], for which Yamanaka was awarded the Nobel Prize. iPSCs offer the potential for personalized regenerative medicine therapy as they can be derived from the patient's own cells. More recently, multilineage differentiating stress enduring cells have been discovered as a potential source of PSCs within adult tissues [54]. Multilineage differentiating stress enduring cells are found within most adult connective tissues, are able to withstand extreme stress, express markers for pluripotency and can be isolated by SSEA-3 expression.

Human ESCs

Human ESCs (hESCs) were first derived in 1998 by Thomson *et al.* [52]. These cells derived from the preimplantation or peri-implantation embryo display prolonged undifferentiated proliferation, and stable developmental potential to form derivatives of all three embryonic germ layers even after prolonged culture [52]. This pluripotent potential can be tested *in vitro* via embryoid body (EB) formation, or *in vivo* via teratoma formation.

Since their discovery, hESCs have been heralded as a potential panacea for regenerative medicine. However, there has also been some debate over whether or not hESCs present an immunogenic risk. There is evidence to suggest that hESCs trigger an immune response [55], however, there is also contrasting evidence to suggest that they are immunoprivileged [56], or have negligible immunogenicity [57]. If hESCs do indeed elicit an immune response, this would hinder clinical application. Banks of clinical-grade hESC lines that can be human leukocyte antigen-matched to groups of individuals could ameliorate potential issues with immunogenicity and make hESCs a viable option

for regenerative medicine [58]. However, the additional challenge of aneuploidy arising from prolonged culture of hESCs is an issue that must be addressed before clinical application of hESCs [59].

Just 12 years after their discovery, hESCs were used in a clinical trial. Geron used hESCs for treatment of spinal cord injuries, however, this trial was prematurely halted [60]. Current trials are underway for the treatment of Stargardt's macular dystrophy, dry age-related macular dystrophy and diabetes [60,61].

Induced PSCs

Human iPSCs (hiPSCs) were first generated via the reprogramming of somatic cells to a pluripotent state by overexpressing a set of key transcription factors: OCT3/4, SOX2, KLF4, and C-MYC [62]. iPSCs have been found to be similar to hESCs in their morphological characteristics, self-renewal capacity, differentiation potential and gene expression profile (although there is some controversy regarding the latter [63]). The use of the patient's own cells place iPSCs at the forefront of personalized medicine by overcoming the possible immunogenicity of ESCs. The reprogramming of the cells was initially performed via retroviral or lentiviral transduction of the key factors. However, reprogramming efficiencies are low, and the process of creating patient-specific cell lines slow and costly. A further significant drawback is the potential for insertional mutagenesis, tumor formation and genetic dysfunction.

To overcome these limitations, non-integrating adenovirus, sendai virus, episomal vector or completely DNA-free techniques have been developed [64–67], with the first in-human iPSC clinical trial taking place in 2014 [68]. The successful implantation of iPSC-derived retinal pigment epithelium cells into a patient with age-related macular dystrophy was reported; however, the trial was prematurely suspended when it was found that the second patient's differentiated cells contained multiple mutations [60]. This raises important safety concerns. It has been suggested that an alternative trial using allogeneic hiPSCs may be a possibility [60].

While iPSCs display many of the characteristics of ESCs such as high proliferation under continuous culture without senescence, and the ability to form teratomas *in vivo*, there are also some fundamental differences. Once reprogrammed, iPSCs retained the epigenetic signature of the somatic parent cell [69], and exhibited altered methylation patterns in some of the key pluripotency genes such as Oct4 [63]. This 'epigenetic memory' can influence the behavior of the reprogrammed cells by directing them toward their lineage of origin, and thus affecting their potency. This could potentially hinder attempts to differentiate iPSCs toward a designated lineage for clinical applications.

A comparison of the benefits and drawbacks of different SC sources is shown in Figure 1. Over recent years, much research has concentrated on the development of potential treatments for musculoskeletal disorders using PSCs.

PSCs & chondrogenic differentiation

Chondrogenesis in EBs

There are numerous techniques that have been developed to induce the *in vitro* differentiation of PSCs into chondrocytes. One method is via the formation of embryoid bodies [70,71]. One study found that hypoxia and morphogenetic factors had synergistic effects on chondrogenesis in EBs [71]. It is established that ESCs are more pluripotent when cultured under hypoxic conditions [72], and *in vivo* cartilage is subjected to hypoxia, and thus may account for the enhanced chondrogenesis observed under hypoxic conditions. While the 3D environment of EBs partially recapitulates the *in vivo* developmental process, the resulting cell population is typically heterogeneous due to the emergence of endoderm and ectoderm lineage-derived cells as well as the desired mesoderm, making downstream processes such as cell sorting essential for achieving a purer cell population. Interestingly, the ability of the TGF-β family to induce chondrogenic differentiation in EBs has produced conflicting results, with inhibitory effects when added at some stages of EB differentiation [70,73,74]. This is despite the TGF-β family being potently prochondrogenic, something that remains true during MSC differentiation [75]. This highlights the distinct differences that exist between ASCs and ESCs in terms of chondrogenic differentiation, and gives an insight into the potential complexity of generating chondrocytes from PSCs. Chondrogenic differentiation of EBs has been achieved via various culture methods, such as pellet or micromass culture [71] methods, also used for cartilage generation using primary chondrocytes and MSCs [76].

As with ESCs, it has been shown that iPSCs can be used to generate EBs, which could subsequently be directed to differentiate into cartilaginous tissue [77]. Reprogrammed osteoarthritic-chondrocytes have also been used to generate hiPSCs, and subsequently differentiated to chondrocytes using TGF-\(\beta\)1 supplementation [78]. Cartilage markers, namely, type II collagen and aggrecan, were expressed by the differentiated hiPCs. This could indicate



that retaining an epigenetic memory may be beneficial for differentiation. However, it is beneficial to have an understanding of the iPSC methylation state as altered methylation patterns in certain genes, such as *COL10A1*, can be beneficial in promoting chondrogenesis and preventing hypertrophy [79].

Chondrogenesis in co-cultures

An alternative differentiation method is to co-culture PSCs with mature chondrocytes. This co-culture can be either direct or indirect [80,81]. In each case, secreted factors from the adult chondrocyte population created an extracellular milieu that enhanced chondrogenic differentiation. One of the factors secreted by mature chondrocytes is parathyroid-related hormone that plays an important role in chondrogenesis and the prevention of hypertrophy [82]. Fibrocartilaginous differentiation has also been shown using hESCs separated from a fibrocartilage-derived chondrocyte cell layer via nylon cell strainers; here indirect co-culture was combined with growth factor supplementation (BMP-4, TGF-\beta3), which improved differentiation significantly [83]. Direct co-culture in the form of high-density pellet culture of hESCs with mature chondrocytes was also shown to enhance differentiation along chondrogenic lines [84]. However, clinical applications of these methods would be difficult due to the need for an autologous chondrocyte population. Furthermore, these culture systems are difficult to scale up as larger cultures often result in poor nutrient diffusion leading to necrotic cores [85,86].

Chondrogenesis via MSC intermediates

Another technique involves differentiating hESCs, or hiPSCs, into chondrocytes via MSC intermediates. hESCs cultured on a monolayer of murine OP9 cells were differentiated toward MSCs [87]. The cells were analyzed following 40 days of culture, and CD73⁺ cells were replated without a feeder layer. These cells were found to express adult MSC markers, and were subsequently successfully differentiated along chondrogenic, osteogenic, adipogenic and myogenic lineages [87]. However, due to the initial use of an animal feeder layer, this method of deriving ESC–MSCs is not clinically compliant and thus may introduce xenoantigens. Clinically compliant MSCs have been derived from hESCs [88]. Cells expressed MSC antigens and gene expression profiles similar to BM-MSCs and could be differentiated into chondrocytes. The hESC-derived MSCs were able to proliferate *in vitro* for at least 35 population doublings without developing any karyotypic abnormalities that would normally occur in *in vitro* cultures of BM-MSCs. This suggests that hESC-derived MSCs may have a much more robust karyotype than adult BM-MSCs.

Chemically defined methods for chondrogenesis

While the aforementioned methods have demonstrated success in the derivation of chondrocytes from PSCs, few systems were clinically compliant. For clinical applications, a fully defined feeder/serum-free culture method is required. To this end, Oldershaw et al. [89] have developed an effective, chemically defined protocol for deriving chondrocytes from hESCs [89,90]. This protocol is based on the sequential signaling pathways involved in the developmental process of chondrogenesis. Growth factors are used to direct differentiation of the hESCs toward chondrocytes over the course of 14 days. A substantial expansion of the cell population was reported during the differentiation protocol (8.5-fold), and between 75 and 97% SOX9-positive cells were obtained with four different hESC lines [91]. The protocol was also applied to two iPSC lines with similar success [91]. Following the 14 day protocol, there was no evidence of pluripotent cells remaining; this was particularly encouraging as residual pluripotent cells following transplantation could result in teratoma formation. This high efficiency and purity makes this a potentially useful protocol for both clinical and laboratory applications. To test the potential for clinical application of this technique, hESC-derived chondroprogenitors embedded in a fibrin gel were transplanted into an osteochondral defect in athymic RNU rats [91]. The transplanted cells formed hyaline cartilage, identifiable from 4 weeks, and fully developed by 13 weeks postimplantation. Defect repair was significantly improved by ESC-derived chondroprogenitors, compared with fibrin-only controls, and they reported significant cell survival of the transplanted population. However, as an osteochondral defect model was used here, it is unclear whether the repair was orchestrated by the implanted cells or the resident SCs from the bone marrow cavity.

PSCs & osteogenic differentiation

Osteogenesis in EBs

As with chondrogenesis, early methods of *in vitro* osteogenic differentiation from PSCs involved EB formation from ESCs and iPSCs [92,93]. However, enhanced osteogenic differentiation has been reported to occur without EB formation [94].

Early studies that utilized EB formation generally relied on *in vitro* assays to study the extent of osteogenic differentiation. However, the reliability of such assays is questionable as they frequently yield positive results despite only a small percentage of cells having been differentiated along the osteogenic lineage. One technique that is used to overcome this is use of flow cytometry to isolate osteoblast cells using lineage-specific markers; however, the markers used for isolation vary between groups. Incorporation of fluorescent reporters such as Col2.3GFP (2.3 kb fragment of the rat Col1a1 promoter) [95] has improved this technique and helped to reduce variation between research groups. Despite this improvement, *in vitro* assays are still not a reliable predictor of bone formation [96]. Techniques such as organotypic culture, and *in vivo* ectopic bone formation are more robust measures of osteogenic capacity.

Osteogenesis in co-culture

Osteogenic differentiation of hESCs has also been shown using direct and indirect co-culture with a variety of different cell types.

Direct co-culture of EBs with primary bone-derived cells was performed, after 14 days of co-culture mineralization and nodule formation was detected [97]. During direct co-culture with human periodontal ligaments fibroblasts *in vitro* mineralization occurred, suggesting that human periodontal ligaments fibroblasts have osteogenic-inducing potential [98].

Indirect co-culture of hESCs has also been performed using the transwell co-culture system [99]. Osteogenic differentiation of EBs was induced by the addition of osteogenic medium. Indirect co-culture with human bone marrow stromal cells (hBMSCs) for 28 days was then initiated 7, 14 or 24 days postdifferentiation. While there was a slight trend toward increased mineral deposition following co-culture compared with controls, the difference was not statistically significant. Furthermore, expression of the osteoblastic markers were more pronounced in hESCs exposed to osteogenic culture medium without co-culture, compared with hESCs co-cultured with differentiated hBMSCs. It is difficult to determine to what extent, if at all, co-culture with hBSCs was beneficial as there did not seem to be any significant improvement in osteogenic differentiation compared with supplementation with osteogenic media alone.

An interesting alternative to traditional co-culture techniques involves culturing hESCs with an autologous osteogenic-inducing culture supplement extracted from hESC-derived osteogenic cells [100]. This novel approach was devised in order to overcome the cost associated with large-scale bioreactor cultures for commercial applications, as the resultant cost of supplementing cultures with growth factors, cytokines and extracellular matrix (ECM) would prove to be prohibitively expensive. Here, a proof-of-principle investigation was performed to demonstrate a potential alternative to culture supplementation proposed to be useful for clinical application. They found that the whole-cell lysate from hESC-derived osteogenic cells promoted aggregation of the hESCs into nodules, and enhanced *in vitro* osteogenic differentiation compared with controls. However, due to the costs that would arise from serum-free culture, they used animal products in their cell culture media. This would have to be addressed for clinical translation.

PSCs & myogenic differentiation

Transplantation of myoblasts from satellite cells or other myogenic populations has been attempted in an effort to treat diseases such as MDs [101–103]; while this work has been promising, the drawbacks of using ASCs prevail. Transplantation of PSC-derived satellite cells into muscle is appealing as this could help simultaneously replenish a depleted resident satellite cell pool, as well as regenerate the muscle tissue itself.

Unlike chondrogenesis and osteogenesis, it has proved very difficult to induce *in vitro* myogenesis via EB formation. While it has been shown that the early stages of myogenesis occur in EBs [104,105], generating cells with the desired regenerative capacity for tissue engineering purposes have proved elusive. It has been postulated that this is because *in vitro* cultures do not form the notochord or neural tube, and so the key signaling events that are orchestrated by these structures *in vivo* cannot occur [106].



Myogenesis in co-culture

Techniques such as co-culture [87,107], and the addition of myogenic medium [108] have demonstrated some success in deriving myogenic cells from ESCs, and have shown some evidence of engraftment when the cells were transplanted into mice [108]. However, assessments were limited to qualitative detection and did not assess the functional capabilities of the engrafted tissue.

Myogenesis via genetic manipulation

An effective myogenic differentiation method includes the application of genetic manipulation techniques to induce expression of myogenic master regulators Pax3 or Pax7 [106] during development of early mesoderm. This bypasses the requirement for early inductive signals from the notochord and neural tube, and provides a method for generating larger quantities of myogenic progenitors, compared with non-genetic techniques. Cells derived from both ESCs and iPSCs have been transplanted into models of MD with some success, demonstrating an overall improvement in functional capacity in terms of muscle force generation [106,109-111]. Myogenic induction of ESCs and iPSCs has also been shown by inducing expression of Met Activating Genetically Improved Chimeric Factor-1 [112]. The myogenic regulatory factor Myo-D has also proved to be useful for the induction of myogenesis in iPSCs [113]. Here, transplantation of the differentiated cells ameliorated the dystrophic phenotype, restored depleted progenitors and improved functional capacity of the muscle. This method could potentially be used to treat various different forms of MD in humans, with the aspect of gene correction offering a personalized approach for patients with inheritable diseases.

While PSCs are particularly amenable to genome editing as they are able to undergo multiple culture manipulations without losing their pluripotency, this method of derivation can be extremely time consuming, and the use of certain vectors carry risks such as mutagenesis, and therefore limit their clinical use. Excisable, non-integrating vectors overcome these issues but are typically less efficient. However, use of animal sera remains an issue, as serum is frequently used as a stimulus for terminal myogenic differentiation [106,110,111], and is therefore a limiting factor in clinical application.

Myogenesis via MSC intermediates

As with chondrogenesis and osteogenesis, MSCs have also been derived from PSCs to facilitate myogenesis. Multipotent iPSC-derived MSCs have been demonstrated to attenuate limb ischemia in mice [114]. Transplantation of iPSC-derived MSCs via intramuscular injection was found to increase myogenesis and neovascularization, and improve limb function compared with injection of BM-MSCs or vehicle only.

Epigenetic memory of iPSCs is often considered to be disadvantageous when comparing iPSCs and ESCs. However, as previously mentioned with regard to in vitro chondrogenesis, epigenetic memory of the parent cell may improve differentiation of the iPSC; this phenomenon has also been reported for iPSCs derived from mesangioblasts [115], suggesting a more robust myogenic lineage commitment when iPSCs are derived from the same lineage.

PSCs & adipogenic differentiation

Adipose tissue is generally thought to develop from the mesoderm. The ability to derive white adipocytes (the most abundant fat cell type in the body) in vitro from stem cells would be of particular benefit to patients requiring surgical reconstruction of soft tissues, something that is often required following trauma caused by disease or injury. Application of PSC-derived adipose tissue would be of significant benefit to patients as current reconstructive methods such as autologous grafting can result in donor site morbidity [116].

Adipogenesis in EBs

In vitro adipogenesis from PSCs has so far relied on the generation of EBs from ESCs and iPSCs, and subsequent differentiation into adipocytes [117-119]. Retinoic acid (RA) is well documented as being an inducer of adipogenesis. Using RA as the differentiation stimulus, a comparison of the adipogenic potential of ESCs and iPSCs has been performed [119]. The authors reported no significant variation between the adipogenic potential of hESCs and hiPSCs overall, however, there was heterogeneity between different iPSC cell lines, despite having the same genetic origin. While RA has been shown to have potent effects on adipogenic differentiation, it is not a standard component of adipogenic medium. Other growth factor combinations such as BMP-2, TGF-ß1, insulin and ascorbic acid are more commonly used [120].

Adipogenesis via genetic manipulation

Another method for inducing adipogenic differentiation in PSCs is to use genetic reprogramming techniques to induce expression of genes involved in adipogenesis. Brown adipose tissue is far less abundant within the body and functions to produce heat through non-shivering thermogenesis. It has been discovered that adults have depots of brown adipose tissue that are inversely correlated in size with BMI [121–123]. This finding has led to considerable interest in the potential therapeutic benefits of brown adipocytes. Retroviral transduction of the *PPARy 2*, *CEBPB* and *PRDM1* genes into hESCs and hiPSCs has been shown to induce adipocyte differentiation into brown adipocytes [117]. Here, the authors found variable adipocyte differentiation potential between cell lines and also reported that efficiency was less in PSCs compared with adipose-derived stromal vascular cells. However, following derivation of both white and brown adipocytes, it was found that *in vivo* transplantation resulted in the formation of tissues with functional and morphological similarities to primary cells, and importantly they reported no teratoma formation after 4–6 weeks.

Adipogenesis via addition of growth factors

Differentiation into functional brown adipocytes has also been achieved without exogenous gene transfer [118]. Supplementation with the cocktail comprising of KITLG, IL6, FLT3LG and VEGF was found to be essential for brown adipose differentiation of hPSCs, both hESCs and hiPSCs. One of their most interesting findings was that inhibitor analyses revealed that p38 MAPK signaling played a role in brown adipose differentiation in hESCs, but MEK signaling did not; however, in hiPSCs MEK signaling was involved in differentiation. This highlighted a distinct difference between hiPSC and hESC-derived brown adipocytes.

From cell-based strategies to tissue engineering 3D constructs

Cell-based therapies for regenerative medicine have not yet demonstrated a full restoration of the damaged tissue to its original state. A tissue engineering approach provides an alternative method to introducing differentiated cells directly into damaged tissue, which incorporates cells, appropriate growth factors, biomaterial scaffold-based/scaffold-free approaches in combination with bioreactor technology to generate a 3D issue construct *in vitro*, before implantation. Thus, mitigating the risk of transferring undifferentiated cells to the patient. 3D culture also aims to recapitulate the *in vivo* environment and facilitates the successful generation of tissues such as cartilage, bone and muscle *in vitro*. Furthermore, this approach ensures that suitable tissue constructs with the appropriate physiological and biomechanical properties are formed, thus providing a level of control that is not possible with cell transplantation.

The use of biomaterial scaffolds in the generation of cartilage tissue is well documented [78–81,84,91], and shares similarities with current clinical interventions for OA (MACI). However, since the native tissue has a low capacity for self-repair, it is desirable to create *in vitro* constructs that are functionally and morphologically identical to native cartilage to improve the ease of integration. Scaffold-free techniques for cartilage tissue engineering have been successful in producing *in vitro* cartilage constructs via chondrogenic differentiation of hPSCs in 3D pellet culture [71,79,81,84,87]. However, limited testing of these cartilage constructs has been performed in a physiologically relevant environment, for example, load-bearing animal model. In one study, hiPSC-derived cartilage pellets were shown to promote healing when introduced into osteochondral defects in the palate groove of immunosuppressed rats [79].

Unlike cartilage which has a very limited capacity for self-repair, bone is a dynamic tissue that is constantly undergoing remodeling and has a much higher repair capacity. Here, scaffolds and various biomaterials have provided an invaluable tool for bone tissue engineering as they can enable a greater level of control over form and structure, and can also be supplemented with osteoinductive agents. Mineralized tissue formed by differentiated PSCs has been shown using various different scaffold materials [93,124–127]. In these studies, the engineered tissue was subcutaneously implanted in animal models and *in vivo* mineralization capacity was evaluated; however, there is a lack of studies that have investigated the *in vivo* reparative effects of the PSC-derived engineered tissue. A stumbling block for bone tissue engineering is the inability to generate/bioengineer a functional blood supply.

For skeletal muscle and adipose tissue trauma such as volumetric muscle loss, or damage that occurs as a result of surgical procedures, tissue engineering using scaffolds has been shown to be of significant clinical benefit [128]. Tissue engineering for such purposes may be either *in vitro* or *in vivo*. There are numerous difficulties associated with *in vitro* construct formation, for example, producing large enough constructs for the affected area takes a long time. It is also difficult to attain good vascularization of muscle constructs and physiologically relevant contraction

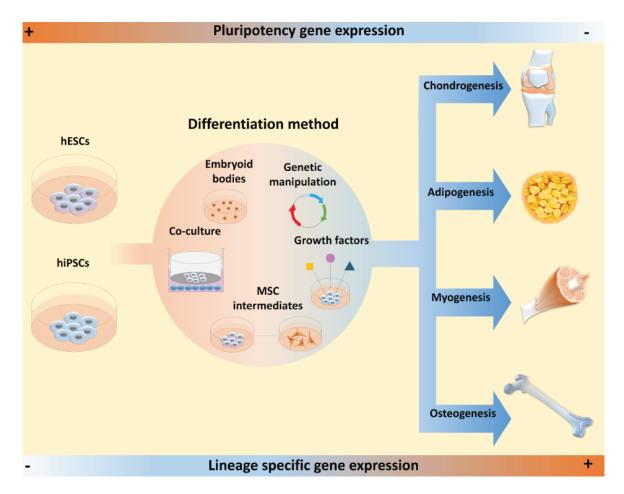


Figure 4. Schematic summarizing methods used to generate cells of mesodermal lineages, namely, chondrogenic, adipogenic, myogenic and osteogenic, from human embryonic stem cells and human-induced pluripotent stem cells. A wide range of methods, including embryoid body generation, genetic manipulation, application of appropriate growth factors, co-culture and differentiation via MSC intermediates, have been applied to generate chondrogenic, adipogenic, myogenic and osteogenic lineages from hPSCs for musculoskeletal regeneration. hESC: Human embryonics stem cell; hPSC: Human pluripotent stem cell; MSC: Mesenchymal stem cell.

forces. The *in vivo* approach to muscle and adipose generation is, therefore, generally more favorable. Here, cells are transplanted with, or into, a biomaterial scaffold that can integrate with the host tissue and form a niche where tissue regeneration may occur [128].

Conclusion & Future perspectives

Musculoskeletal regeneration has become a prominent research area, no doubt due to the sociological and economic pressures imposed by the current ageing population. The ability of PSCs to self-renew and differentiate into any somatic cell type may well prove to be a highly effective tool in the treatment of such diseases. With regard to iPSCs, their potential is irrefutable, and the opportunity to derive allogenic cells from patients is extremely enticing. However, several issues remain to be addressed, such as the efficiency of reprogramming using non-viral vectors and the impact of 'epigenetic memory' on therapeutic treatments. In contrast, hESCs are not associated with these problems.

Regarding differentiation protocols, cells of mesodermal origin have been derived via a variety of methods (Figure 4); however, it is clear that there is a requirement for clinically compliant, chemically defined methods of deriving specific cell types while keeping costs as low as possible. This review has gone some way toward showing that such protocols are a possibility, for instance, Oldershaw *et al.* developed a protocol for the directed differentiation of hESCs/hiPSCs to chondrocytes that resulted in a high cell yield, and was fully chemically defined which would ease generation of a clinically compliant protocol [89]; however, to make such treatments accessible, cost would

likely remain an issue. It is also prudent to acknowledge that protocols using PSCs to derive cells for application in drug testing, for example, myogenic progenitors and myotubes [129], are also of value for tissue engineering and knowledge gained from such studies is of significant value to the field.

Treatment approaches in the future are likely to focus on tissue engineering as this would enable the existence of a quality control system, whereby 3D explants that are generated can be assessed in terms of their morphological, mechanical and physiological properties prior to implantation. Use of bioreactors is likely to increase in popularity as they allow for precise and accurate manipulation of environmental factors that allows for a more physiological culture setting. However, for clinical purposes, more high-throughput systems will ultimately be required. Importantly, to fully elucidate the functional capacity of tissue-engineered musculoskeletal constructs, it is vitally important that these are tested in appropriate *in vivo* models, and the parameters relating to their function are fully assessed.

Executive summary

Socioeconomic burden of musculoskeletal deterioration

- Diseases affecting the musculoskeletal system are a major cause of disability and morbidity.
- Effective long-term treatment options are lacking, resulting in increased strain on healthcare systems and individuals.

Current interventions for the treatment of major musculoskeletal diseases & their limitations

- Osteoarthritis: Current surgical interventions such as mosaicplasty and autologous chondrocyte implantation
 produce fibrous repair cartilage, and do not offer long-term treatment solutions. Joint replacement surgery is a
 late-stage treatment option.
- Osteoporosis: Current pharmacological interventions may be effective but typically require life-long administration and can have side effects.
- Myopathies: Currently, there are no approved drugs or exercise interventions that consistently result in an increase in both muscle mass and strength.

Pluripotent stem cells: a promising alternative for musculoskeletal regeneration

- There are two known types of pluripotent stem cells (PSCs): embryonic stem cells and induced PSCs.
- Due to their capacity to differentiate into any somatic cell type, and ability to proliferate indefinitely *in vitro* without undergoing cellular senescence, PSCs are an idea candidate cell type for regenerative medicine.

PSCs & chondrogenic, osteogenic, myogenic & adipogenic differentiation

- The most commonly used methods for differentiation into mesodermal lineages are:
 - via embryoid body formation
 - via mesenchymal stem cell intermediates
 - co-culture
 - genetic manipulation
 - growth factor addition.
- There is a requirement for clinically compliant differentiation protocols for clinical translation.

From cell-based strategies to tissue engineering 3D constructs

• A tissue engineering approach mitigates the risk of transferring undifferentiated cells to the patient, and enables the assessment of tissue quality prior to implantation.

Future perspective

• Future work will most likely involve tissue engineering rather than cell transplantation, and will require clinically compliant methods of cell derivation.

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