

1 **Effects of micro-alloying Ag on microstructure, mechanical properties and**
2 **corrosion behavior of extruded Mg-2Zn-0.2Ca-xAg alloys**

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10 **ABSTRACT**

11 The present work investigates effects of micro-alloying Ag on the microstructure,
12 mechanical properties and corrosion behavior of as-extruded Mg-2Zn-0.2Ca alloys.

13 The addition of Ag, up to 0.5 wt.%, induce limited difference on microstructural
14 characteristics such as slightly coarser microstructures due to the enhanced dynamic
15 recrystallization process and the presence of refined precipitates. The tensile properties
16 of the alloy were not significantly changed by Ag addition, i.e., all the alloys exhibited
17 exceptional elongation of ~30%, moderate tensile yield strength and ultimate strength
18 of ~140 MPa and ~240 MPa, respectively. The corrosion performance of the alloys was
19 progressively deteriorated with increasing Ag content i.e., the corrosion rate increased
20 from 0.40 ± 0.23 mm/y for Mg-2Zn-0.2Ca alloy to 3.27 ± 0.24 mm/y for the Mg-2Zn-
21 0.2Ca-0.5Ag alloy. The compromised corrosion performance was attributed to a large
22 electrode potential difference between the nobler $\text{Ca}_2\text{Mg}_6\text{Zn}_3$ phase and the α -Mg
23 matrix as well as a less protective corrosion film, by increasing Ag addition.

24
25 **Keywords:** Magnesium Alloys; Mg-Zn-Ca-Ag; Microstructure Characterization;
26 Corrosion Behavior; Mechanical Properties

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28 **1. Introduction**

29 As the population ages, an increasing number of individuals will become susceptible to
30 various degenerative diseases, such as arthritis, osteoporosis, and trauma. This trend
31 has sparked a significant global demand for orthopedic implants [1, 2]. Magnesium (Mg)
32 based alloys have attracted considerable attention as implant materials due to their
33 outstanding biocompatibility, elastic modulus closer to natural bone (compared with
34 bio-inert metals like titanium, stainless steel and cobalt-chromium alloys), and unique
35 biodegradability without the need for a second extraction surgery [1]. Nevertheless, the
36 rapid degradation of magnesium alloys can result in premature failure before the
37 completion of the healing process, limiting their application. Therefore, the
38 development of biocompatible magnesium alloys with superior mechanical properties
39 as well as controllable degradation rate is crucial [1].

40 Many magnesium alloys have been developed to explore their feasibility for biomedical
41 applications, of which Mg-Zn-Ca-based alloys attract increasing attention because of
42 their excellent biocompatibility and high mechanical properties [3-9]. Zinc emerges as
43 the most crucial alloying element, enhancing mechanical properties of Mg alloys
44 through both solution strengthening and precipitation hardening, while minimizing the
45 degradation rate by eliminating adverse effects of impurities in Mg alloys [8, 10, 11].
46 A biodegradable Mg-2.0Zn alloy had been clinically approved and its composition was
47 further optimized by adding a small amount of calcium [3, 12], considering that Ca, an
48 essential biological element, helps improving tensile strength and reducing the
49 corrosion rates of Mg-Zn based alloys by refining microstructure [5, 13]. For example,
50 it was found that a minor (0.2 wt.%) amount of Ca increased the tensile yield strength
51 (TYS) of a Mg-2Zn alloy by 115 MPa [12] and reduced the corrosion rate of a Mg-
52 2Zn-0.5Mn alloy by ~ 20% [5].

53 The incorporation of silver (Ag), a well-known antimicrobial agent, into Mg alloys was
54 reported to enhance their antibacterial activity [14-17], which is considered beneficial
55 to eliminate postoperative infections. Additional advantages induced by Ag addition to
56 Mg includes promoting secondary phase precipitation to strengthen Mg alloys and

57 reducing *c/a* ratio to the improve their ductility and deformability [18, 19]. For example,
58 the tensile elongation of a Mg-Zn alloy was significantly increased from 12.0% to 19.8%
59 with a minor (0.2 wt.%) addition of Ag [18].

60 Based on both the strengthening effects as well as the bio-functionality of Zn, Ca and
61 Ag, quaternary Mg-Zn-Ca-Ag alloys have been extensively studied for developing of
62 biodegradable Mg alloys [17, 20]. Optimizing the composition, especially the Ag
63 content, of the quaternary alloy is not an easy task, as inconsistent results have been
64 reported on how Ag could affect the biodegradation behavior of the magnesium alloys.
65 Some publications reported that adding Ag into Mg based alloys deteriorated their
66 corrosion performance [16, 18, 21, 22], while Ag was also reported to improve their
67 corrosion resistance [14, 20]. Moreover, it seems that the corrosion resistance of the
68 Mg-Zn-Ca alloys may either be improved or deteriorated depending on Ag content. For
69 instance, Yu et al. [20] added different amounts of Ag into a Mg-3Zn-0.2Ca alloy, and
70 found that an addition of 0.3 wt.% Ag yielded the optimum result in terms of reduced
71 biodegradation. Dragomir et. al. [14] claimed that a minimum of 2.5 wt.% Ag is needed
72 to improve the corrosion resistance of a biodegradable Mg-Zn alloy, which is contrary
73 to the results reported by Ma et al. [22] that the Ag content of >2 wt.% severely
74 compromised the corrosion resistance of the Mg-1Zn-0.2Ca alloy.

75 The inconsistency in the literatures on the effects of the Ag addition to the degradation
76 behavior of the Mg-Zn-Ca alloy motivates us to explore further this area. In the present
77 study, different amounts of Ag were added to a Mg-2.0Zn-0.2Ca, a clinically approved
78 biodegradable Mg alloy, to comparatively investigate their microstructure
79 characteristics, mechanical properties and corrosion performances.

80 **2. Materials and methods**

81 **2.1 Materials preparation**

82 Pure Mg (99.95 wt.%), pure Zn granules (99.995 wt.%) and Mg-25 wt.% Ca master
83 alloy were initially melted at approximately 740 °C in a steel crucible. Subsequently,
84 the temperature of the melt was raised to about 780 °C to facilitate the dissolution of

85 pure Ag (99.99 wt.%). The melt was then thoroughly refined to get a homogenized
 86 composition. Throughout the entire smelting process, the molten alloy was shielded by
 87 a flux to prevent burning. The melt was then cooled to 680 °C and transferred to the DC
 88 casting unit to produce ingots. Actual compositions of the prepared ingots were
 89 evaluated using inductively coupled plasma optical emission spectroscopy (ICP-OES,
 90 Spectro Blue Sop, Germany), the detection limit was better than 1 ppm, with a
 91 resolution of 16 picometers (pm) and an accuracy better than 0.5%. The chemical
 92 compositions of the studied alloys are summarized in Table 1.

93 **Table 1** Actual chemical composition of the studied alloys (wt.%).

Alloy Designation	Alloying Elements				Impurity Elements			
	Mg	Zn	Ca	Ag	Fe	Cu	Ni	Si
ZX20	<i>Bal.</i>	2.00	0.20	-	0.0110	0.0013	0.0008	0.0110
ZXQ0.1	<i>Bal.</i>	2.07	0.20	0.11	0.0047	0.0006	0.0028	0.0073
ZXQ0.3	<i>Bal.</i>	2.00	0.20	0.27	0.0083	0.0006	0.0004	0.0150
ZXQ0.5	<i>Bal.</i>	2.04	0.17	0.50	0.0091	0.0006	0.0027	0.0092

94 2.2 Microstructure characterization

95 The microstructural analysis of investigated alloys, both before and after corrosion, was
 96 conducted using scanning electron microscopy (SEM, Tescan Mira3, Czech) equipped
 97 with an energy dispersive spectroscopy detector (EDS). The grain size and orientation
 98 information were acquired using an Oxford Instruments C-Nano electron backscatter
 99 diffraction (EBSD) detector embedded in the SEM facility with a step size of 0.5 μm .
 100 The area fraction of the secondary phases in as-extruded alloys were obtained by
 101 analyzing corresponding SEM images using ImageJ software. Phase composition of the
 102 studied alloys was evaluated by X-ray diffraction (XRD) using a D/Max 2500VB
 103 diffractometer with Cu K_{α} radiation ($\lambda=0.154$ nm) operated in the Bragg-Brentano
 104 geometry. The diffraction was conducted in a 2θ range of 20°-80° with a scanning rate
 105 of 1 °/min, and a step size of 0.02°. The acquired XRD patterns were then analyzed
 106 using the simple search / match function incorporated in the MDI Jade Pro software
 107 (with PDF-4+ diffraction files). The surface potential of polished samples was
 108 examined by scanning Kelvin probe force microscopy (SKPFM) using a Bruker
 109 Dimension Icon instrument. All measurements were performed at room temperature in
 110 atmospheric conditions maintained with 40% relative humidity. The sample

111 microstructure was also characterized using a FEI Talos F200S transmission electron
112 microscope (TEM) with an accelerating voltage of 200 kV. As-extruded samples were
113 initially ground using progressively finer SiC papers up to 3500 grit, followed by
114 polishing with silica suspension for SEM characterization. The EBSD sample
115 preparation involved further electropolishing at a voltage of 25 mV in a perchloric acid
116 solution at -35 °C. The TEM specimen preparation involved mechanical grinding,
117 twin-jet electropolishing (using a solution of 95 vol% alcohol and 5 vol% perchloric
118 acid at -35 °C). The sample was finally thinned using a Gatan 691 ion thinner, by
119 bombardment with energetic Ar ions of 3 keV from a 3° cutting angle.

120 **2.3 Uniaxial tensile and compression tests**

121 The mechanical properties of as-extruded alloys along the extrusion direction (ED)
122 were determined through both tensile and compression tests. Tensile testing was
123 conducted in accordance with ASTM E8 specification using an Instron 3369 universal
124 testing machine with a tension rate of 2 mm/min. The gauge section in the tensile
125 sample had a length of 25 mm and a diameter of 5 mm. For compression testing, the
126 samples were cylindrical with dimensions of Ø8 mm×16 mm, and the compression
127 rate was 1 mm/min. Triple tests were performed to ensure the reliability and validity of
128 the results.

129 **2.4 Immersion tests**

130 The corrosion behavior of the samples was evaluated using both immersion tests and
131 electrochemical techniques. The samples for immersion tests were cut from as-extruded
132 rods into dimensions of 10 mm × 10 mm × 5 mm. Prior to corrosion test, the samples
133 were ground using 3500 grit SiC papers, ultrasonically cleaned in ethyl alcohol and
134 finally dried in blowing air. All samples were immersed in 0.9 wt.% NaCl solution for
135 15 days at a temperature of 37 ± 1 °C. During the immersion test, hydrogen bubbles
136 released from the sample surface were collected, which volume of gas evolved
137 quantified using an inverted burette [23], and the corrosion rate was calculated using
138 Equation (1) in accordance with ASTM F3268-18a:

$$139 \quad P_H = 2.279V_H \quad (1)$$

140 where V_H ($\text{mL}\cdot\text{cm}^{-2}\cdot\text{day}^{-1}$) is the hydrogen evolution rate estimated by recording the
141 volume of water expelled from the burette at intervals of 12 hours. After immersion test,
142 the samples were sequentially washed using chromic acid, water, and ethyl alcohol to
143 remove the corrosion products. The weight loss (ΔW) in the immersion was also
144 converted into corrosion rate according to the Equation (2) in accordance with ASTM
145 G31-12a:

$$146 \quad P_W = \frac{8.76 \times 10^4 \times \Delta W}{A \times D \times T} \quad (2)$$

147 where ΔW (g) represents the weight loss of specimens following immersion, A (cm^2) is
148 the surface area of specimens, D ($\text{g}\cdot\text{cm}^{-3}$) is the density of alloys and T (h) is the
149 immersion time.

150 **2.5 Electrochemical measurements**

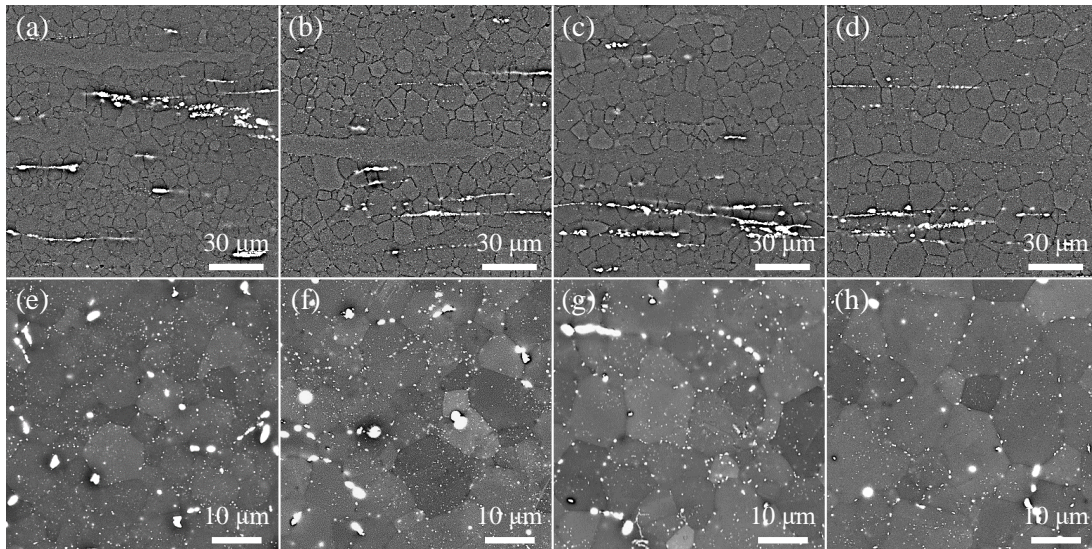
151 Electrochemical measurements were conducted in 0.9 wt.% NaCl solution by using a
152 three-electrode cell comprising a sample as the working electrode, a platinum plate as
153 the counter electrode and a saturated calomel electrode (SCE) as the reference electrode.
154 The exposed surface area of each sample was $10 \text{ mm} \times 10 \text{ mm}$. After 2 hours immersion,
155 the open circuit potential (OCP) was stabilized to allow the potentiodynamic
156 polarization (PDP) tests that were performed by scanning in the range of $-300 \sim +300$
157 mV (vs. OCP) with a rate of $1 \text{ mV}\cdot\text{s}^{-1}$. Electrochemical impedance spectroscopy (EIS)
158 was carried out after stabilization of the OCP value, with perturbation amplitude of 5
159 mV in the frequency range from 10^5 to 10^{-2} Hz.

160 **3. Results and discussion**

161 **3.1. Microstructure evolution after hot extrusion**

162 Fig. 1 displays SEM images of as-extruded alloys. The microstructure of all samples
163 comprised fine equiaxed grains and a limited number of elongated grains (Fig. 1(a-d)).
164 After Ag addition, the number of elongated grains reduced, and the size of equiaxed
165 grains increased, especially noticeable when the Ag content reached 0.5 wt.%.
166 Furthermore, the coexistence of coarse intermetallic along extrusion direction (ED)
167 (Fig. 1(a-d)) with fine intermetallic primarily located at grain boundaries and

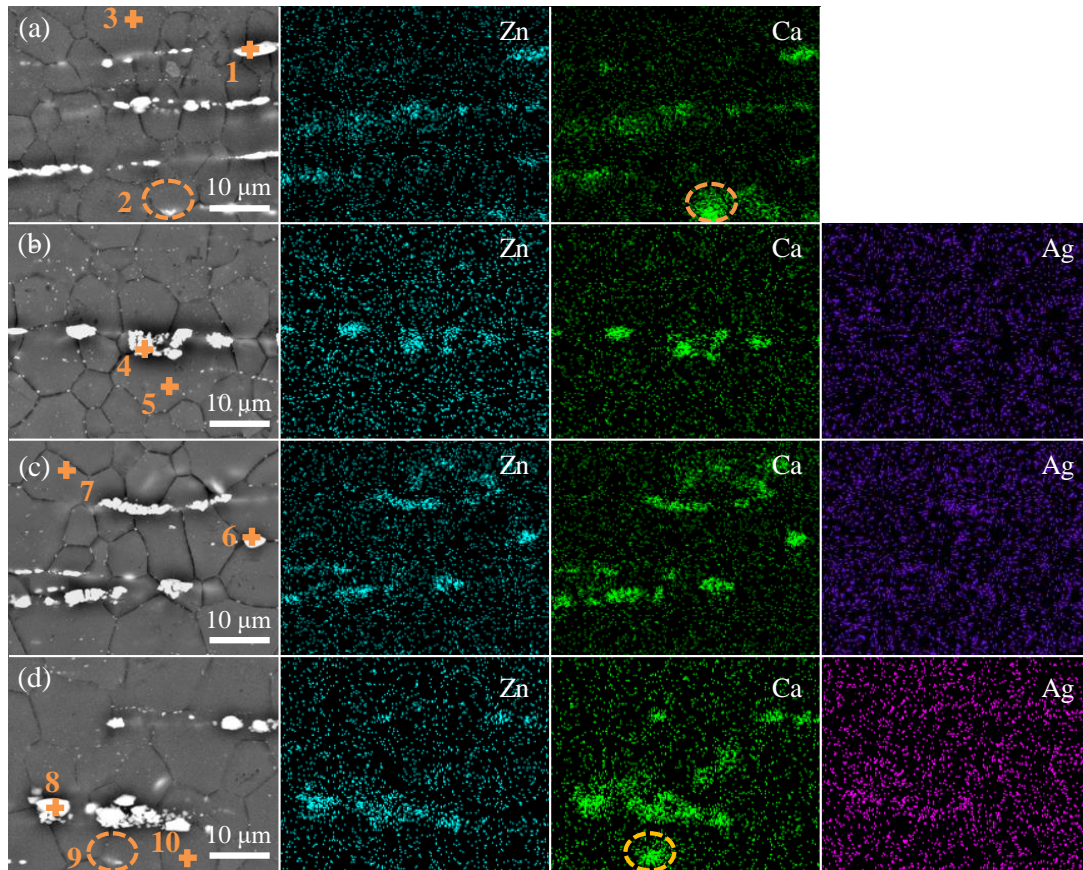
168 moderately within grains (Fig. 1(e-f)), was also observed. The coarse intermetallics
169 might have originated from the residual secondary phase after homogenization, while
170 the fine intermetallic might result from dynamic precipitation during hot extrusion.
171 Notably, all samples exhibited similar intermetallic volume fractions, approximately
172 1.2%, except that a fraction of $\sim 0.8\%$ was determined in the alloy containing 0.5 wt.%
173 Ag.



174
175 **Fig. 1.** Backscattered electron SEM images of the longitude (a~d) and transverse (e~h) sections of
176 as-extruded Mg-2Zn-0.2Ca-xAg (x=0, 0.1, 0.3 and 0.5 wt.%) alloys: (a, e) ZX20, (b, f) ZXQ0.1,
177 (c, g) ZXQ0.3 and (d, h) ZXQ0.5.

178 Chemical composition of the intermetallic was analyzed using EDS, and the results are
179 depicted in Fig. 2 and listed in Table 2. It is evident that both Zn and Ca are concentrated
180 in the secondary phases of as-extruded alloys. Notably, the addition of Ag did not alter
181 the distribution of Zn and Ca. Co-segregation of Ag with Zn and Ca in the secondary
182 phase was identified by a noticeably higher Ag content in those regions compared to
183 the surrounding α -Mg matrix (Table 2). Moreover, Ag concentration in the intermetallic
184 gradually increased with the rising Ag content in the alloy. Specifically, Ag content in
185 the secondary phases of the ZXQ0.1 alloy was measured at 0.3 at.% (Region 4 in Fig.
186 3(b)), increasing gradually to 0.7 at.% (Region 6 in Fig. 3(c)) and 1.3 at.% (Region 8)
187 for the ZXQ0.3 and ZXQ0.5 alloys, respectively. The consumption of Ag in the
188 secondary phases reduced its concentration in the α -Mg matrix, and Ag was even
189 undetectable in the α -Mg matrix of the ZXQ0.1 and ZXQ0.3 alloys when the bulk Ag

190 addition was apparently low. The atomic Zn/Ca ratio in the secondary phases of the
 191 alloys was calculated to vary around the stoichiometric 3/2 ratio in the intermetallic
 192 $\text{Ca}_2\text{Mg}_6\text{Zn}_3$. Therefore, the secondary phase observed in the alloy was preliminarily
 193 determined as $\text{Ca}_2\text{Mg}_6\text{Zn}_3$ as reported elsewhere [9, 12]. Additionally, there were minor
 194 traces of Ca-rich intermetallics in the ZX20 and ZXQ0.5 alloys (Region 2 and 9 in Fig.
 195 3), although their fraction was low enough to be neglected in the present study.



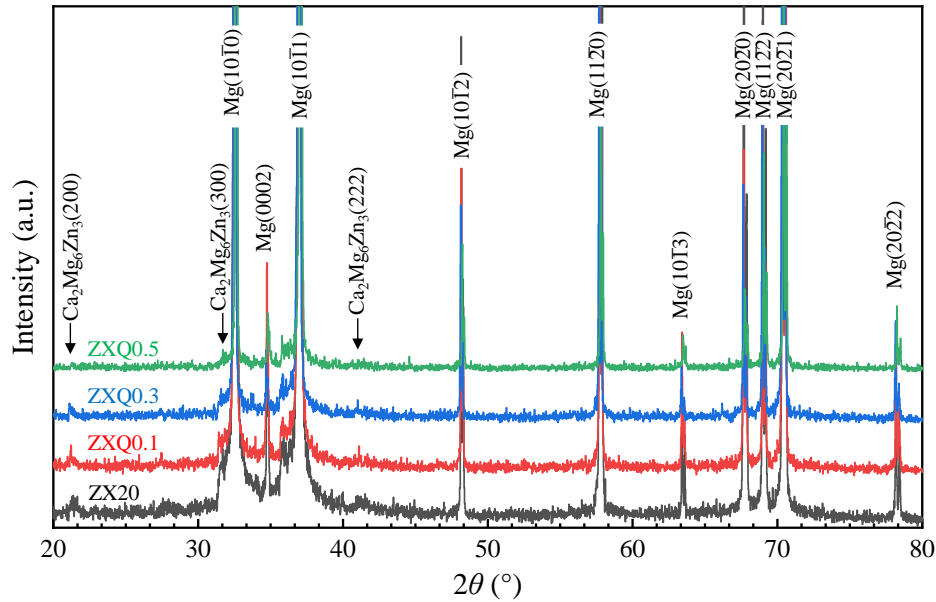
196
 197 **Fig. 2.** SEM-EDS mapping results of as-extruded Mg-2Zn-0.2Ca-xAg (x=0, 0.1, 0.3 and 0.5
 198 wt.%) alloys: (a) ZX20, (b) ZXQ0.1, (c) ZXQ0.3 and (d) ZXQ0.5.

199 **Table 2** EDS results (at.%) from matrix and the second phase particles in as-extruded Mg-2Zn-
 200 0.2Ca-xAg (x=0, 0.1, 0.3 and 0.5 wt.%) alloys of Fig. 2.

Elements	ZX20			ZXQ0.1		ZXQ0.3		ZXQ0.5		
	1	2	3	4	5	6	7	8	9	10
Mg	82.0	83.5	99.2	82.8	99.0	80.2	99.3	78.1	91.7	99.0
Zn	11.7	2.5	0.7	10.6	1.0	11.9	0.6	12.0	2.9	0.7
Ca	6.2	14.0	0.1	6.2	0.1	7.2	0.1	8.7	5.2	0.2
Ag	-	-	-	0.3	-	0.7	-	1.3	0.3	0.1

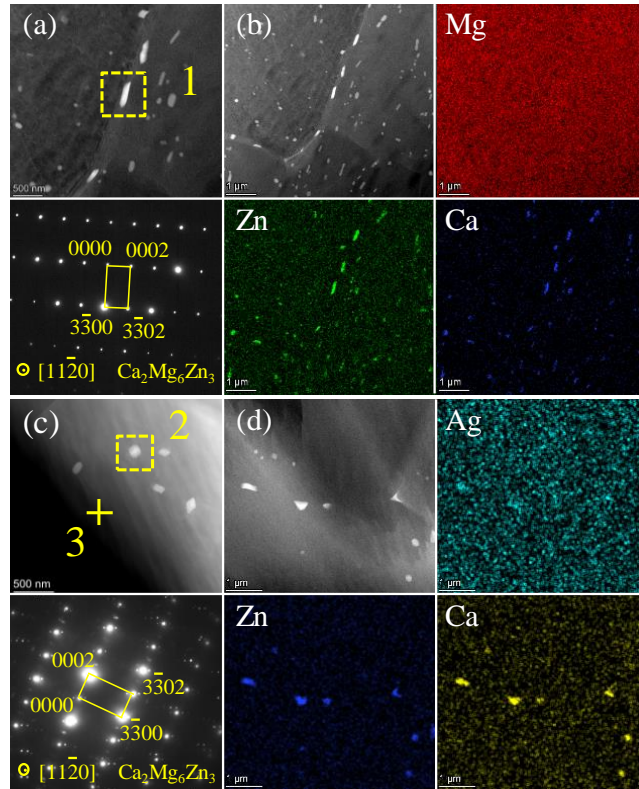
201 Fig. 3 illustrates the XRD results of as-extruded alloys. The coexistence of α -Mg and
 202 $\text{Ca}_2\text{Mg}_6\text{Zn}_3$ phases was observed in all the specimens. The presence of the α -Mg phase

203 was straightforward, while the $\text{Ca}_2\text{Mg}_6\text{Zn}_3$ phase was determined by the diffraction
 204 peaks at $2\theta=21.1^\circ$ and $2\theta=41.2^\circ$. Consistent with EDS analysis, small additions of Ag
 205 did not induce any new phases in the alloy. The relative intensity of the peaks associated
 206 with the $\text{Ca}_2\text{Mg}_6\text{Zn}_3$ phase decreased with increasing Ag content, particularly evident
 207 in the ZXQ0.5 alloy.



208
 209 **Fig. 3.** XRD patterns of as-extruded Mg-2Zn-0.2Ca-xAg ($x=0, 0.1, 0.3, 0.5$ wt.%) alloys.

210 Fig. 4 displays TEM images, selected area electron diffraction (SAED) patterns, and
 211 elemental distributions of as-extruded ZX20 and ZXQ0.3 alloys. In line with the results
 212 shown in Fig. 1, fine intermetallics distributed within the grains and at the grain
 213 boundaries in both the Ag-free and Ag-containing alloys. Notably, the precipitates
 214 situated at grain boundaries exhibited larger dimensions than those within the grains.
 215 This size discrepancy was attributed to a higher energy of grain boundaries, leading to
 216 preferential segregation of solute atoms and subsequent formation of larger precipitates
 217 [24]. The area fraction of precipitates in the ZX0.3 alloy was, $1.1 \pm 0.3\%$, slightly lower
 218 than that of ZX20 ($1.2 \pm 0.3\%$). Chemical analysis of the secondary phases was
 219 conducted to reveal co-segregation of Zn, Ca and Ag in the secondary phases (Fig. 4
 220 and Table 3). The SAED indexing results depicted in Figure 4, along with the chemical
 221 analysis outlined in Table 3, determined further that the secondary phases observed in
 222 the ZX20 and ZXQ0.5 alloys were $\text{Ca}_2\text{Mg}_6\text{Zn}_3$, consistent with those documented in
 223 [9].



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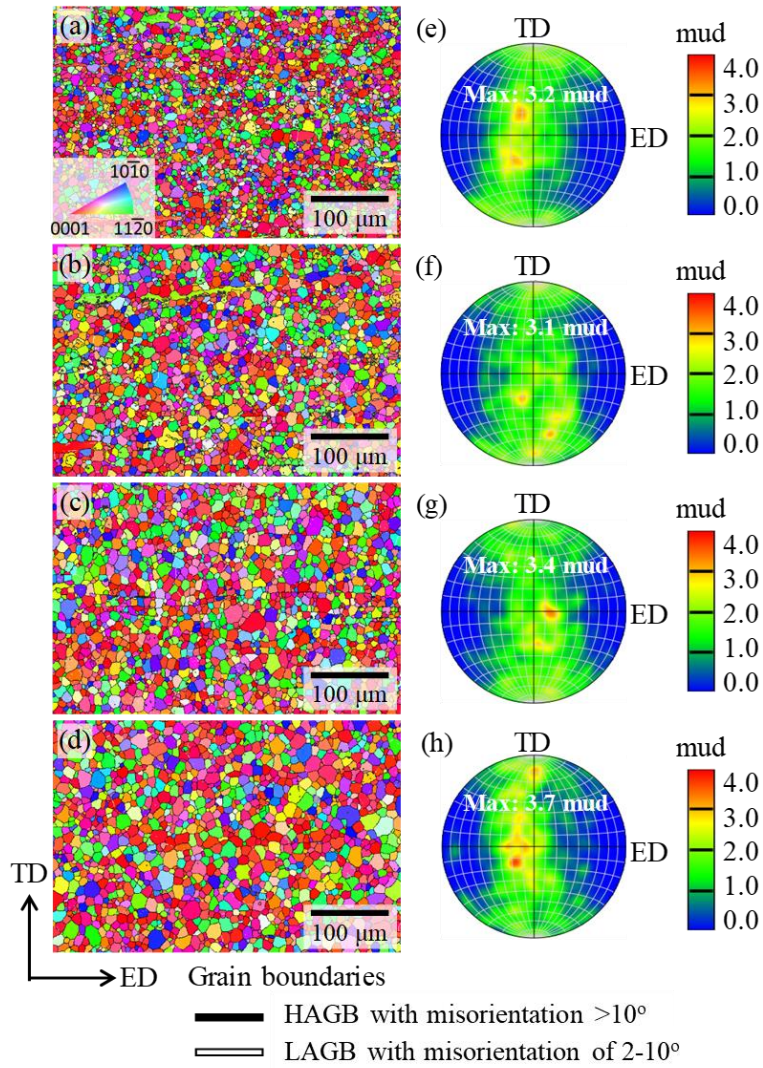
Fig. 4. Higher magnification dark field images (a, c) with corresponding selected-area electron diffraction (SAED) images of the precipitates of yellow box, lower magnification dark field images and corresponding EDS mappings (b, d): ZX20 (a, b) and ZXQ0.3 (c, d).

Table 3 EDS results (at.%) collected from the points marked in Fig. 4.

Elements	ZX20		ZXQ0.5	
	1	2	2	3
Mg	85.92	73.14	99.22	
Zn	10.28	17.05	0.09	
Ca	3.80	9.09	0.02	
Ag	-	0.72	0.09	

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Fig. 5 represents the inverse pole figure (IPF) maps as well as the (0002) pole figures of as-extruded alloys. Consistent with the SEM images shown in Fig. 1, as-extruded alloys comprised mainly fine equiaxed grains and minor elongated grains. After analyzing the grain orientation spreads (GOS) following widely accepted criteria [25], the fine equiaxed grains possessing a GOS of $<2^\circ$ were considered to be formed through the dynamic recrystallization (DRX) process during hot extrusion, and therefore, assigned as DRXed grains. On the other side, the elongated grains possessed high GOS values ($\text{GOS} > 2^\circ$) were determined to be deformed grains.



237

238 **Fig. 5.** EBSD inverse pole figure (IPF) maps (a~d) and corresponding (0002) pole figures (e~h) of

239 as-extruded Mg-2Zn-0.2Ca-xAg (x=0, 0.1, 0.3 and 0.5 wt.%) alloys: (a, e) ZX20, (b, f) ZXQ0.1,

240 (c, g) ZXQ0.3, (d,h) ZXQ0.5.

241 The volume fraction of DRXed grains (V_{DRX}), as well as their average grain size (AGS)

242 were calculated, and the results are summarized in Fig. 6. All samples had been

243 recrystallized to a high extent with V_{DRX} values higher than 90%. Moreover, a trend for

244 V_{DRX} to increase along with the Ag content was also confirmed. To be specific, the V_{DRX}

245 value increased slightly from 90.6% to more than 93.7%, for the ZX20 and ZXQ0.5

246 alloy, respectively. Meanwhile, the AGS values of the two alloys were measured to be

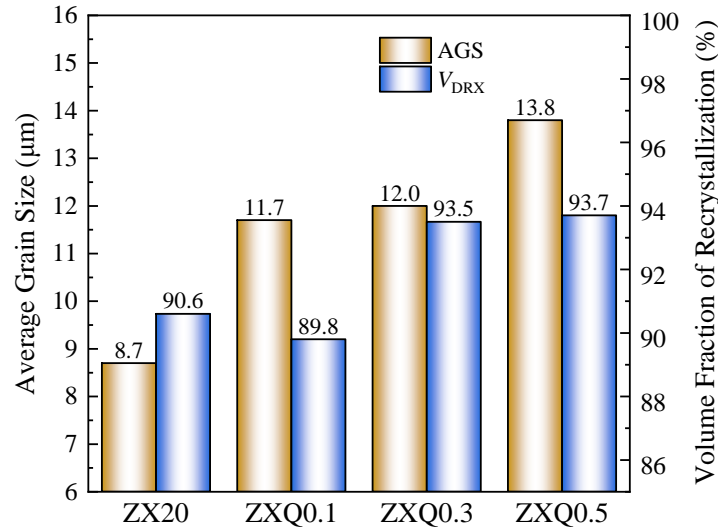
247 $8.7 \pm 2.8 \mu\text{m}$ and $13.8 \pm 4.6 \mu\text{m}$, respectively. These observations suggested that Ag

248 addition promoted the DRX process and facilitated subsequent grain growth. According

249 to the (0002) pole figure (Fig. 5), all as-extruded samples exhibited rather similar

250 texture characteristics, with a similar maximum pole intensity among them, irrespective

251 of the Ag content in the alloy. To be specific, each of as-extruded alloys exhibited a
 252 typical fiber texture, characterized by the majority of grains aligning their c -axis ($\langle 0001 \rangle$
 253 direction) perpendicular to ED, albeit spreading unevenly in the radial directions.



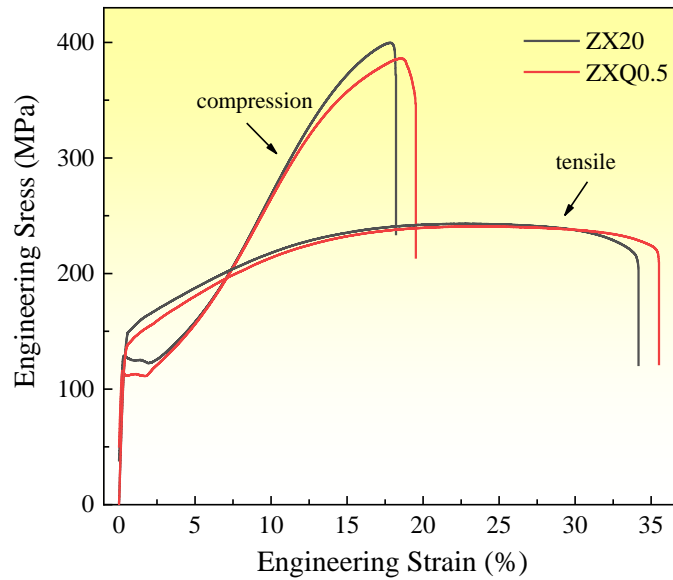
254 **Fig. 6.** Comparison of V_{DRX} and AGS values among as-extruded Mg-2Zn-0.2Ca-xAg ($x=0, 0.1,$
 255 0.3 and 0.5 wt.%) alloys.
 256

257 3.2 Tensile and compression properties

258 Fig. 7 depicts the engineering stress-strain curves obtained from both tensile and
 259 compression tests of the as-extruded alloys at room temperature. Whilst the curves in
 260 Fig. 7 were derived from a single experiment, the mean average results of three parallel
 261 tests are summarized in Table 4. All the samples exhibited conventional hardening type
 262 stress-strain tensile curves. The stress corresponding to a 0.2% strain was considered as
 263 the yield strength. All specimens exhibited exceptional fracture elongation (FE) around
 264 30%, in tensile test, irrespective of the Ag content. Nevertheless, Ag addition slightly
 265 reduced the TYS of the alloys, while the ultimate tensile strength (UTS) maintained
 266 roughly the same (~ 240 MPa). The reduction in TYS was primarily attributed to
 267 coarsening the microstructure (Fig. 5-6) which compromised the precipitation
 268 strengthening effect due to lower amounts of the secondary phase particles (Fig. 1). The
 269 ZX20 alloy exhibited the highest strength and considerable ductility under the tensile
 270 tests, with the values of TYS, UTS and FE being approximately 151.5 MPa, 244.1 MPa
 271 and 29.9% respectively.

272 On the other hand, the compressive stress-strain curves possessed sigmoidal shapes

273 with significant yielding plateau related to the deformation twinning [26]. In contrast
 274 to that observed in tensile tests, the introduction of Ag resulted in a moderate
 275 enhancement in the strength and fracture strain of as-extruded alloys during
 276 compression tests. A dramatically higher yield strength was derived in tension
 277 compared to compression (Fig. 7 and Table 4), irrespective of the Ag contents in the
 278 alloys, exhibiting the typical yielding asymmetry of highly textured Mg alloys [27, 28].
 279 Notably, the ultimate compressive strength increased from 361.8 ± 13.0 MPa to 381.9
 280 ± 7.8 MPa, and the fracture strain increased from $18.6 \pm 0.8\%$ to $21.1 \pm 2.2\%$ when 0.5
 281 wt.% Ag was added to the Mg-Zn-Ca alloy.



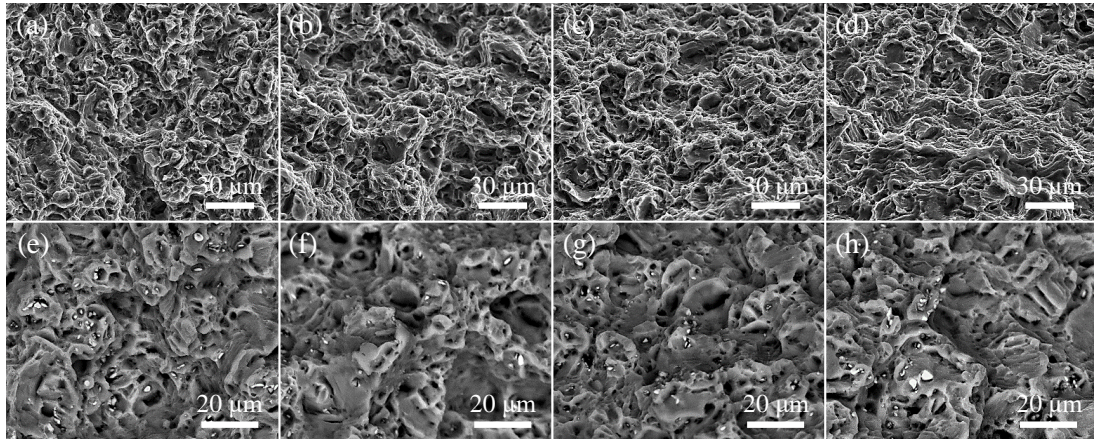
282
 283 **Fig. 7.** Tensile and compressive stress-strain curves of as-extruded ZX20 and ZXQ0.5 alloys.
 284

285 **Table 4** TYS, UTS, EF, CYS, UCS, and FS of as-extruded Mg-2Zn-0.2Ca-xAg (x=0, 0.1, 0.3 and
 286 0.5 wt.%) alloys.

Alloys	Tension			Compression		
	TYS (MPa)	UTS (MPa)	FE (%)	CYS (MPa)	UCS (MPa)	FS (%)
ZX20	151.5 ± 6.2	244.1 ± 2.8	29.9 ± 0.9	107.0 ± 11.2	361.8 ± 13.0	18.6 ± 0.8
ZXQ0.1	144.1 ± 7.0	239.7 ± 3.2	30.4 ± 1.6	106.1 ± 9.7	373.7 ± 16.8	19.6 ± 1.3
ZXQ0.3	143.3 ± 5.6	239.4 ± 1.3	28.7 ± 2.3	106.4 ± 5.7	371.8 ± 19.4	20.7 ± 1.9
ZXQ0.5	135.8 ± 3.0	239.3 ± 1.1	29.8 ± 2.9	108.1 ± 3.9	381.9 ± 7.8	21.1 ± 2.2

287 The fracture morphology of the four alloys after tensile tests is illustrated in Fig. 8.
 288 Abundant dimples, indicative of ductile fracture, were clearly observed, contributing to
 289 the outstanding elongation of the studied alloys (Fig. 7). The secondary phase particles

290 participated in the dimpling process, as revealed by closer examination of the dimples
291 (Fig. 8(e-h)). Actually, it has been documented that the micro-voids preferably
292 nucleated at the interface between the secondary phase and the matrix, the propagation
293 and coalescence of adjacent voids would eventually lead to fracture of the samples [29].



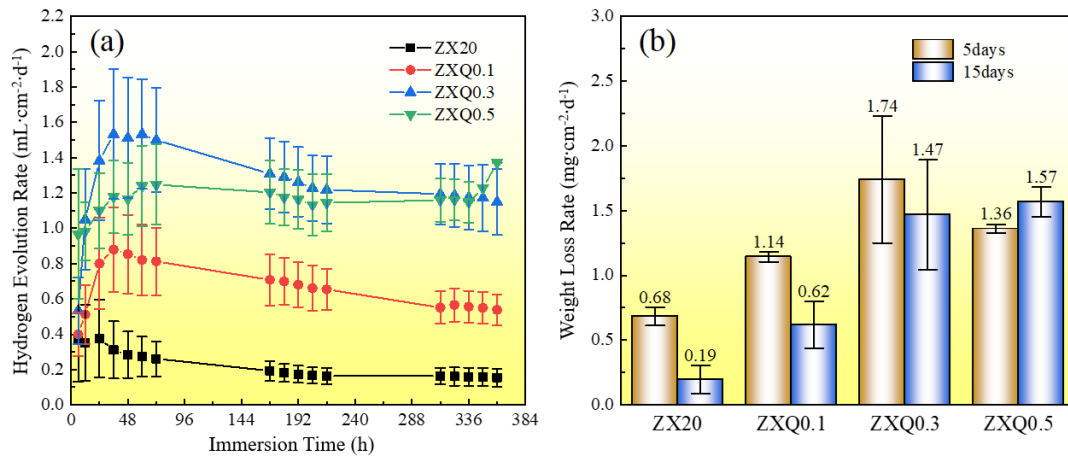
294
295 **Fig. 8.** Second electron images (a~d) and Backscattered electron images (e~h) of tensile-fractured
296 as-extruded Mg-2Zn-0.2Ca-xAg (x=0, 0.1, 0.3 and 0.5 wt.%) alloys: (a, e) ZX20, (b, f) ZXQ0.1,
297 (c, g) ZXQ0.3 and (d,h) ZXQ0.5.

298 3.3 Immersion tests

299 The corrosion rates of the samples were assessed by recording hydrogen evolution and
300 weight loss during immersion tests, and the results are illustrated in Fig. 9. As shown
301 in Fig. 9(a), the hydrogen evolution rate (HER) increased within the first 36 hours of
302 immersion, followed by a gradual decrease. Finally, the HER values remained almost
303 unchanged (except for the abrupt HER rise observed from the ZXQ0.5 alloy). This trend
304 could be attributed to the formation and gradual accumulation (and thickening) of
305 corrosion products that partially protect sample surface. Moreover, the HERs noticeably
306 increased with increasing Ag content in the samples. Converting HER values into
307 corrosion rates (mm/y), the Ag-free ZX20 alloy exhibited the slowest corrosion of
308 around 0.35 ± 0.12 mm/y after 15 days' immersion. A minimum addition of 0.1 wt.%
309 Ag dramatically increased corrosion rate to 1.23 ± 0.20 mm/y, which further climbed
310 up to 3.04 ± 0.40 mm/y and 3.13 ± 0.12 mm/y when the Ag content increased to 0.3 wt.%
311 and 0.5 wt.%, respectively.

312 The corrosion rate represented by the weight loss rate (WLR) aligned well with that
313 illustrated by HER. For alloys with Ag content below 0.3%, lower WLR were observed

314 after the long-term (15 days) immersion compared to the short-term (5 days) one.
 315 However, an inversed WLR trend was observed from the ZXQ0.5 alloy, where a higher
 316 WLR was recorded after 15 days' immersion (Fig. 9(b)). The corrosion rates (P_w) of
 317 as-extruded alloys, converted from the WLR, were 0.40 ± 0.23 mm/y, 1.29 ± 0.38 mm/y,
 318 2.74 ± 0.95 mm/y, and 3.27 ± 0.24 mm/y, for the ZX20, ZXQ0.1, ZXQ0.3 and ZXQ0.5,
 319 respectively.

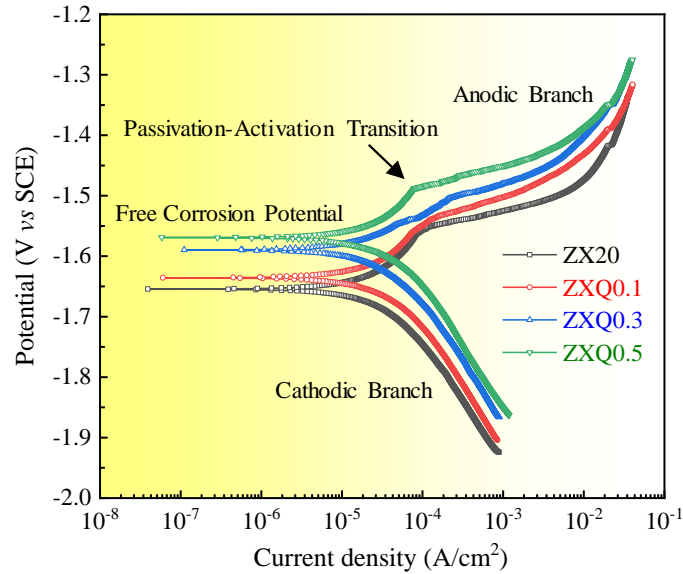


320
 321 **Fig. 9.** (a) Hydrogen evolution rate and (b) Weight loss rate of as-extruded Mg-2Zn-0.2Ca-xAg
 322 (x=0, 0.1, 0.3 and 0.5 wt.%) alloys immersed in 0.9 wt.% NaCl solution for different times at 37 ± 1
 323 $^{\circ}\text{C}$.

324 3.4 Electrochemical measurements

325 Fig. 10 depicts the potentiodynamic polarization (PDP) curves of as-extruded alloys
 326 in a 0.9 wt.% NaCl solution at 37 ± 1 $^{\circ}\text{C}$. It was clear that the free corrosion potential
 327 (E_{corr}) of the sample progressively increased with the increasing Ag content in the alloy,
 328 which is consistent with the existing literature [20, 21]. The increased E_{corr} suggested
 329 that Ag addition might be beneficial for reducing corrosion susceptibility of Mg-Zn-Ca
 330 alloy from the thermodynamics aspect. As expected, all the samples were partially
 331 passivated when anodically polarized, possibly due to the accumulation of the corrosion
 332 product film on the sample surface [20]. Then passive-active transitions illustrating
 333 breakdown of the corrosion film were observed on the anodic branches of PDP curves
 334 for all samples. The breakdown potential increased as well with the Ag content. For
 335 instance, the breakdown potential of the ZX20 alloy was determined to be -1.56 V vs.
 336 SCE, while that of the ZXQ0.5 alloy was -1.49 V vs. SCE. The stability of the corrosion

337 film was assessed by the difference between the free corrosion potential (E_{corr}) and the
 338 breakdown potential (E_{break}), with the higher potential gap indicating the better stability.
 339 From this aspect, the film on ZX20 alloy possessed superior stability as the highest
 340 potential gap was determined to be 0.1 V vs. SCE from Fig. 10, while the stability of
 341 the ZXQ0.5 alloy was the lowest, with a potential difference of 0.08 V.



342
 343 **Fig. 10.** Potentiodynamic polarization plots of as-extruded Mg-2Zn-0.2Ca-xAg (x=0, 0.1, 0.3 and
 344 0.5 wt.%) alloys immersed in 0.9 wt.% NaCl solution at 37 ± 1°C.

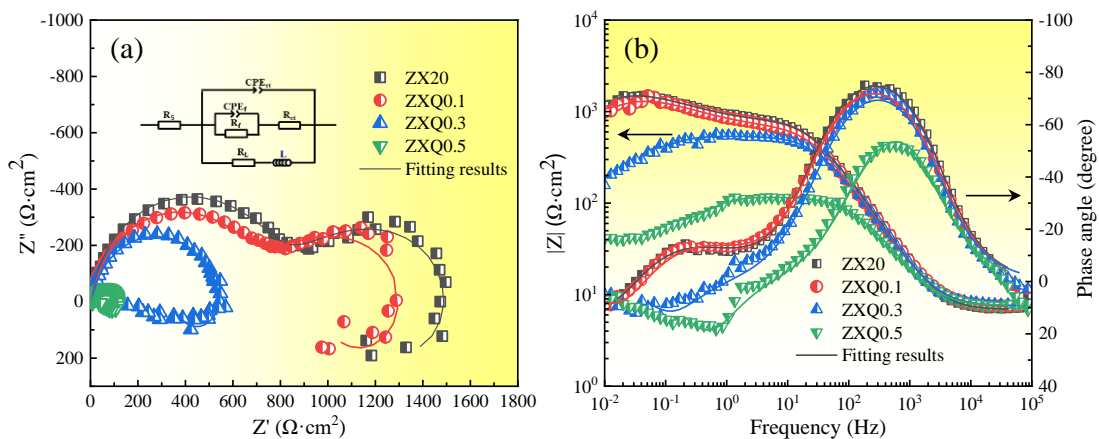
345 **Table 5** Fitting results from the PDP plots for as-extruded Mg-2Zn-0.2Ca-xAg (x=0, 0.1, 0.3 and
 346 0.5 wt.%) alloys after immersion for 30 min.

Alloys	E_{corr} (V vs. SCE)	B_c (mV/decade)	i_{corr} ($\mu\text{A}/\text{cm}^2$)
ZX20	-1.65 ± 0.01	-199.57 ± 7.15	39.82 ± 3.66
ZXQ0.1	-1.64 ± 0.01	-204.54 ± 5.07	46.54 ± 1.83
ZXQ0.3	-1.60 ± 0.01	-205.83 ± 0.99	48.20 ± 10.86
ZXQ0.5	-1.57 ± 0.01	-229.68 ± 7.19	50.14 ± 7.86

347 The passive film instability on the Ag-containing alloys led to their deteriorated
 348 corrosion resistance. Because the PDP curves did not present any well-defined Tafel
 349 region on the anodic branch, the corrosion current density of the alloys were derived
 350 through the Tafel extrapolation of the cathodic branches in accordance with that
 351 suggested in the literature [30], and the results are summarized in Table 5. The corrosion
 352 current density value inversely correlated with the corrosion resistance of the alloys. In
 353 this study, the ZX20 alloy exhibited the lowest corrosion current density compared to

354 the Ag-containing alloys. Moreover, a marginal increase in Ag content was associated
 355 with a slight elevation in corrosion current density, indicating a detrimental effect on
 356 corrosion resistance due to the addition of Ag to Mg-Zn-Ca alloys. The current density
 357 followed the same order as the hydrogen evolution and weight loss rates presented in
 358 Fig. 9.

359 The corrosion behavior of the studied alloys was also evaluated using the
 360 electrochemical impedance spectroscopy technique, and the results are presented in Fig.
 361 11. The Nyquist plots (Fig. 11(a)) of the studied alloys comprised two capacitive loops
 362 in the first quadrant and one inductive loop (with positive imaginary component of the
 363 impedance) in the fourth quadrant. The size of these loops shrunk, as Ag content in the
 364 alloy increased, suggesting deterioration of the corrosion resistance. When the Ag
 365 content was higher than 0.3 wt.%, the capacitive loop in the middle frequency region
 366 had shrunk so much that the two capacitive loops could hardly be differentiated.
 367 However, its presence could be indirectly verified from the variation of the phase angle
 368 Bode plots shown in Fig. 11(b). The capacitive loop at high frequency originated from
 369 charge transfer process across the double-layer, and the capacitive loop at middle
 370 frequency referred to the mass transfer through the corrosion product. The inductive
 371 loop at low frequency was associated with the desorption and adsorption of corrosion
 372 by-products from the sample surface [31].



373
 374 **Fig. 11.** (a) Nyquist plots and (b) Bode plots of as-extruded Mg-2Zn-0.2Ca-xAg (x=0, 0.1, 0.3 and
 375 0.5 wt.%) alloys immersed in 0.9 wt% NaCl solution at $37 \pm 1^\circ\text{C}$.

376 Fig. 11(b) shows the Bode plots for the modulus and phase angle variation as a function

377 of frequency. The peak in phase-angle Bode plots and the elevation in modulus Bode
378 plots were corresponding to the capacitive loop in Nyquist plots [32]. The first phase-
379 angle peak (at high frequency) was smaller and narrower, and the second phase-angle
380 peak (at low frequency) almost diminished when the Ag addition was ≥ 0.3 wt.%,
381 suggesting Ag addition was not helpful for the formation of protective film on the
382 surface of studied alloys. The impedance modulus $|Z|$ of all samples coincided quite
383 well in the high frequency domain (10^3 - 10^5 Hz) because of similar double-layer
384 geometries. As frequency reduced to $<10^3$ Hz, $|Z|$ curves departed from each other, i.e.,
385 much lower $|Z|$ curves were observed from the Ag-containing alloys. Considering that
386 $|Z|$ values were inversely proportional to the corrosion rate of the alloys, it could be
387 inferred that Ag addition compromised the corrosion performance of the Mg-Zn-Ca
388 alloy. The reduced corrosion resistance could be attributed to less protective corrosion
389 films accumulated on the sample surface after comparative analysis of the $|Z|$ values in
390 different frequency domains, which is consistent with the analysis of the PDP curves
391 shown in Fig. 10.

392 **Table 6** Fitting results of EIS data for as-extruded Mg-2Zn-0.2Ca-xAg (x=0, 0.1, 0.3 and 0.5
393 wt.%) alloys.

Alloys	R_s / $\Omega \cdot \text{cm}^2$	R_{ct} / $\Omega \cdot \text{cm}^2$	CPE_{ct-T} / $\mu\Omega \cdot \text{cm}^{-2} \cdot \text{s}^n$	n_1	R_f / $\Omega \cdot \text{cm}^2$	CPE_f-T / $\mu\Omega \cdot \text{cm}^{-2} \cdot \text{s}^n$	n_2	R_L / $\Omega \cdot \text{cm}^2$	L / $\text{H} \cdot \text{cm}^2$	χ^2
ZX20	6.9	786.8	11.7	0.95	996.0	1215.6	0.64	3163.0	45163.0	0.0014
ZXQ0.1	7.3	692.0	14.6	0.93	836.0	1144.7	0.65	2681.0	29394.0	0.0033
ZXQ0.3	7.5	493.2	15.4	0.92	42.0	200.0	0.80	1033.0	1643.0	0.0092
ZXQ0.5	7.6	90.4	19.4	0.92	19.2	185.3	0.81	99.5	47.6	0.0100

394 An equivalent circuit model shown in Fig. 11(a) was proposed in the present study to
395 quantitatively fitting the EIS results. The physical validation of the equivalent circuit
396 was rationalized by examining cross-sectional morphologies of corroded specimens
397 (shown later). In the circuit, R_s represents the solution resistance, mainly depending on
398 the distance between the working electrode and the Luggin capillary orifice of the
399 reference electrode. Connected in parallel R_{ct} and CPE_{ct} represent the charge transfer
400 resistance and the double layer capacitance of the electrode/solution interface,
401 respectively [32, 33]. The $R_f || CPE_f$ couple analogies impedance associated with the

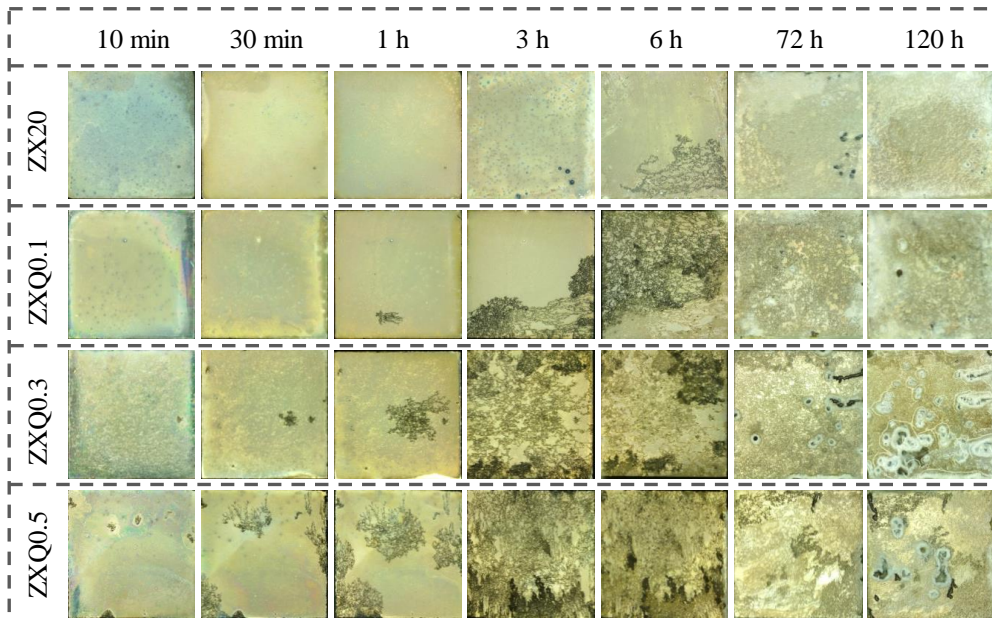
402 mass transfer across the corrosion product film [33]. L and R_L in series represent the
403 inductance and its resistance related to the desorption and adsorption of the corrosion
404 products from the corrosion pits.

405 Using the equivalent circuit, the experimental EIS diagrams were adequately fitted (as
406 verified by the Chi-square χ^2 less than 0.01), and the fitting results were also included
407 as solid lines in Fig. 10. Corresponding fitting parameters are summarized in Table 6.
408 Clearly, both R_{ct} and the R_f decreased dramatically as the Ag content increased in the
409 alloy. R_f and CPE_{f-T} were closely related with the geometries of the pores in the
410 corrosion film, and larger and thicker pores in the corrosion film normally resulted in
411 lower R_f and CPE_{f-T} [34]. In this regard and based on the data shown in Table 6, more
412 porous corrosion films might have been accumulated on the alloys with higher Ag
413 contents. Such porous films were unable to provide sufficient protection from corrosion
414 attack, thus, worse corrosion performance was identified in the alloys with higher Ag
415 contents.

416 **3.5 Corrosion morphology**

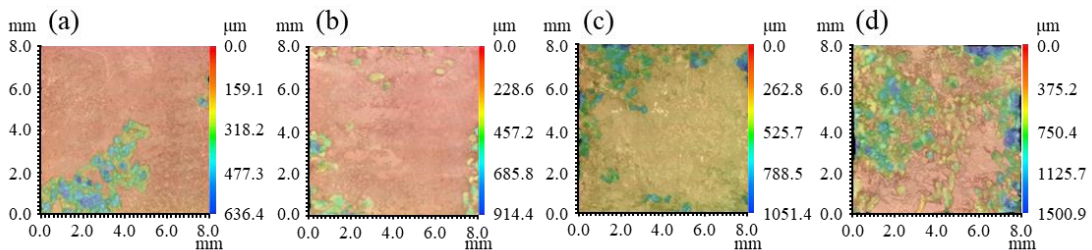
417 Fig. 12 shows the optical images of as-extruded alloys after being immersed for 5 days
418 in 0.9 wt.% NaCl solution at 37 ± 1 °C, to uncover their corrosion behavior. The
419 corroded areas increased with immersion time regardless of Ag contents in the alloys.
420 It took approximately 3 hours to visually observe noticeable changes, such as black
421 corrosion filaments on the surface of the Ag-free ZX20 alloy. In contrast, only 1 hour
422 of immersion was sufficient to generate visible changes on the surface of the Ag-
423 containing ZXQ0.1 alloy. This incubation time was further shortened to less than 10
424 minutes when the Ag content increased to 0.5 wt.%. When the immersion time for the
425 first sight of such changes was taken to evaluate the corrosion resistance of the alloys,
426 a longer duration (raised from the more sustained corrosion product on the surface)
427 indicated better corrosion resistance of the sample with less Ag content. This
428 observation agreed with the breakdown potential analysis of the PDP curves shown in
429 Fig. 10. Moreover, the propagation rate of those initial corrosion sites varied among the
430 samples depending on the Ag content. To be specific, after 3 hours of immersion, the

431 entire surface of the alloy with more than 0.3 wt.% Ag was badly corroded, while only
 432 less than 50% of the surface area of the ZXQ0.1 alloy had been attacked. Therefore, Ag
 433 addition to Mg-Zn-Ca alloys may shorten the incubation period of localized corrosion
 434 and enhance the corrosion propagation in 0.9 wt.% NaCl solution at $37 \pm 1^\circ\text{C}$.



435
 436 **Fig. 12.** Optical micrographs showing the surfaces of as-extruded Mg-2Zn-0.2Ca-xAg (x=0, 0.1,
 437 0.3 and 0.5 wt.%) alloys after immersion for various times up to 120 h

438 Fig. 13 illustrates 3D tomographic maps of the studied alloys after 15-days immersion
 439 with the corrosion products removed. The corrosion filaments and pits were visible on
 440 the sample surfaces. As Ag content increased to 0.5 wt.%, the localized corrosion area
 441 expanded, and its local depth notably increased from 636.4 μm to 1500.9 μm . This
 442 outcome suggested an augmented inclination toward vertical corrosion, leading to a
 443 deterioration in the corrosion resistance of Ag-containing alloys.

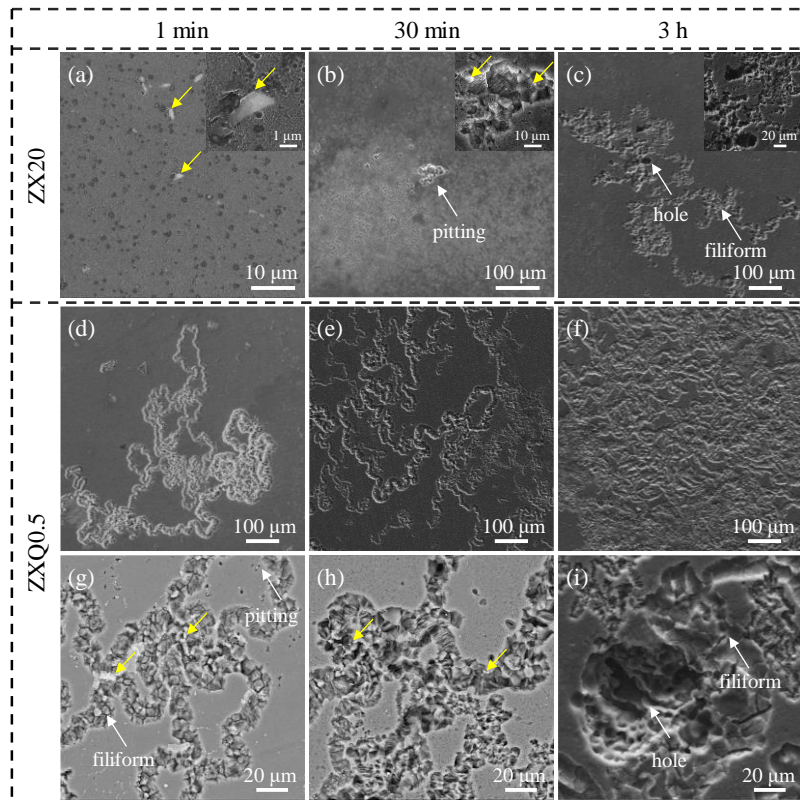


444
 445 **Fig. 13.** 3D tomographic maps of as-extruded Mg-2Zn-0.2Ca-xAg (x=0, 0.1, 0.3 and 0.5 wt.%)
 446 alloys without corrosion products: (a) ZX20, (b) ZXQ0.1, (c) ZXQ0.3 and (d) ZXQ0.5.

447 The above analysis provides additional evidence that adding Ag to the ZX20 alloy

448 significantly compromised its corrosion resistance, particularly when the Ag content
449 exceeded 0.3 wt.%. Fig. 14 displays corrosive morphologies of ZX20 and ZXQ0.5
450 alloys after immersion for 1 minute, 30 minutes, and 3 hours with the corrosion
451 products removed. Discrete localized corrosion sites were observed on the ZX20 alloy
452 after the initial 30-min immersion. The examination of corroded morphology revealed
453 that corrosion initiated at the vicinity of the secondary phases (marked by yellow arrows
454 in Fig. 14(a)). The signs of filiform corrosion became apparent when the immersion
455 times prolonged to 3 hours. As for the ZXQ0.5 alloy, the footprint of filiform corrosion
456 could be observed shortly after the beginning of immersion test (<1 min), which
457 propagated rapidly to form larger and deeper corrosion pits with extended immersion
458 durations. It was speculated that the addition of Ag accelerated the corrosion process
459 by hastening the onset of pitting corrosion and creating more local corrosion sites.
460 Besides, regardless of the addition of Ag, the ultimate corrosion type manifested as a
461 blend of pitting corrosion vertically and filamentous corrosion horizontally (Fig. 14(c,
462 i)). Such observation was consistent with that depicted in Fig. 12.

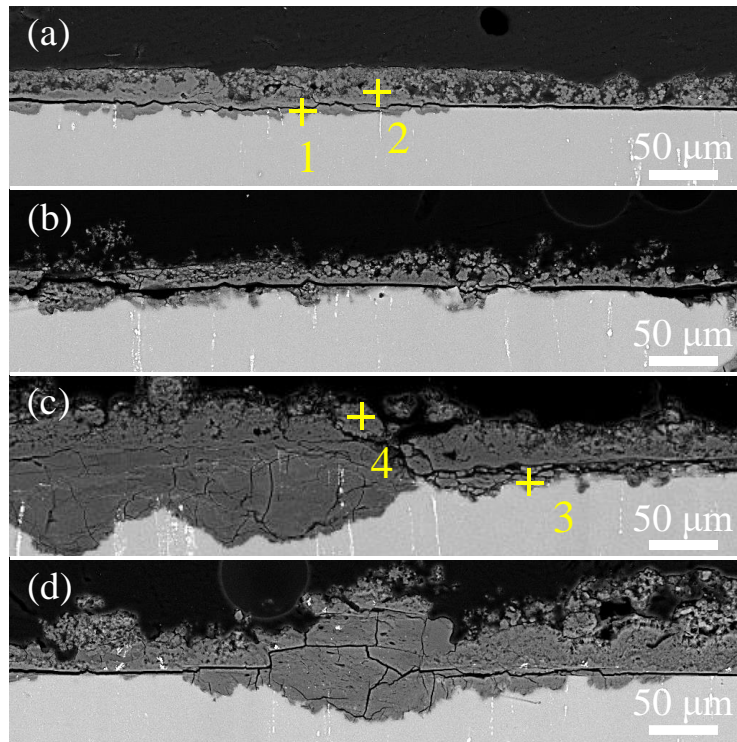
463 Cross-sectional SEM images of the studied alloys after 5 days of immersion in a 0.9
464 NaCl solution, with corrosion products retained, are displayed in Fig. 15. All alloys
465 were covered by corrosion products, whose morphologies depended on Ag content. To
466 be specific, a relatively uniform product film was formed on the surface of Ag-free
467 alloy with a thickness of $\sim 45 \mu\text{m}$, while the product film on Ag-containing alloys was
468 uneven with the maximum thickness up to $\sim 154 \mu\text{m}$. Correspondingly, a relatively
469 uniform interface between the substrate and the corrosion film had been observed in
470 the ZX20 alloy, and the surface of ZX20 alloy roughly maintained its integrity except
471 for some discrete corrosion pits expanded deep towards the substrate (Fig. 15(a)).
472 Nevertheless, the scenario was dramatically different when a trace amount (0.1 wt.%)
473 of Ag was added into the alloy. The corrosion product became more porous, and the
474 surface of the substrate was aggressively attacked, leaving some deeper pits (Fig. 15(b))
475 compared with that observed from the ZX20 alloy.



476

477 **Fig. 14.** SEM images without corrosion products of ZX20 and ZXQ0.5 after immersion for
 478 various times up to 3 h in 0.9 wt.% NaCl solution at $37 \pm 1^\circ\text{C}$ (Yellow arrows were used to mark
 479 the intermetallic).

480 Further increasing the Ag content in the alloy resulted in a thicker and nonuniform
 481 corrosion film, and almost the entire surface of the samples had been corroded. Then
 482 corrosion pits propagated even deeper towards the substrate with a maximum pitting
 483 depth of around $40 \mu\text{m}$ being measured in the ZXQ0.3 alloy. Additionally, the corrosion
 484 cracks were more evident in the Ag-containing alloys. It was worth noting that the
 485 cracks referred to here were not in a straight style alike that formed due to dehydration
 486 caused by electron bombardment of specimens during SEM observation, but rather in
 487 an irregular form (formed by the lower Pilling-Bedworth ratio of Mg). The porous
 488 corrosion film was only loosely attached to the sample surface (consistent with the EIS
 489 analysis), through which the corrosion medium easily penetrated towards the substrate
 490 to compromise its corrosion resistance. Furthermore, similar to that observed in Fig. 14,
 491 the initiation and propagation of corrosion sites around and along the secondary phases
 492 is also evident in Fig. 15, suggesting possible occurrence of micro-galvanic corrosion
 493 during immersion.



494
495
496
497

Fig. 15. Cross-section BSE images of as-extruded Mg-2Zn-0.2Ca-xAg (x=0, 0.1, 0.3 and 0.5 wt.%) alloys immersed in 0.9 wt.% NaCl solution for 5 days at $37 \pm 1^\circ\text{C}$: (a) ZX20, (b) ZXQ0.1, (c) ZXQ0.3 and (d) ZXQ0.5.

498 Chemical composition of the corrosion film was investigated using EDS technique, and
499 the results are shown in Table 7. Mainly O and Mg were detected from the corrosion
500 film of the studied alloys ZX20 and ZXQ0.3. However, the atomic O to Mg ratio
501 appeared to vary along the thickness of the corrosion film. To be specific, the chemical
502 data obtained near the substrate revealed an atomic O/Mg ratio of roughly 1/1,
503 indicating the presence of MgO. This ratio was significantly increased to around 1.6/1
504 in the outer layer of the corrosion film, suggesting partial hydration of MgO to form
505 Mg(OH)₂.

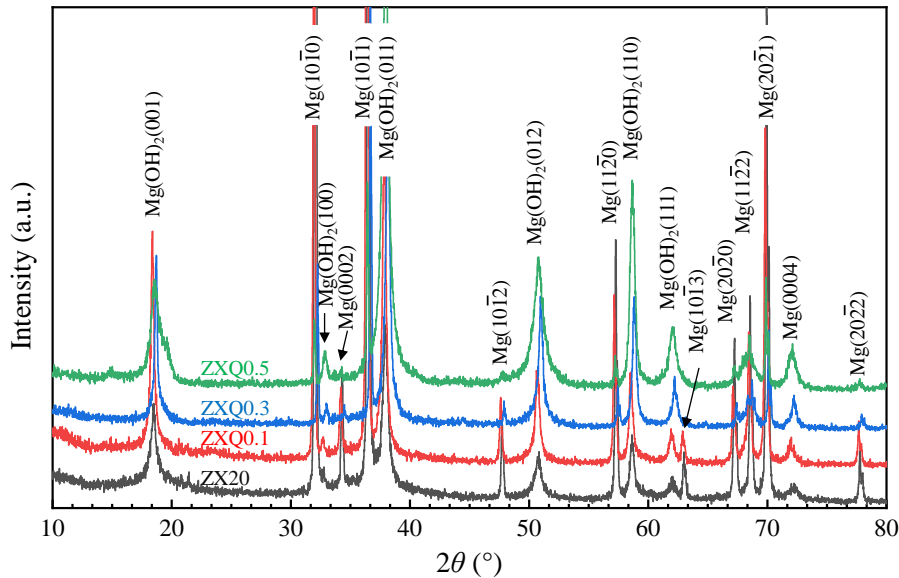
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Table 7 EDS results (at.%) collected from the points marked in Fig. 14.

Elements	ZX20		ZXQ0.3	
	1	2	3	4
O	57.5	61.0	47.1	62.1
Mg	41.7	38.8	52.1	37.8
Zn	0.6	0.1	0.6	0.1
Ca	0.2	0.1	0.2	0.1
Ag	-	-	0.1	0.0

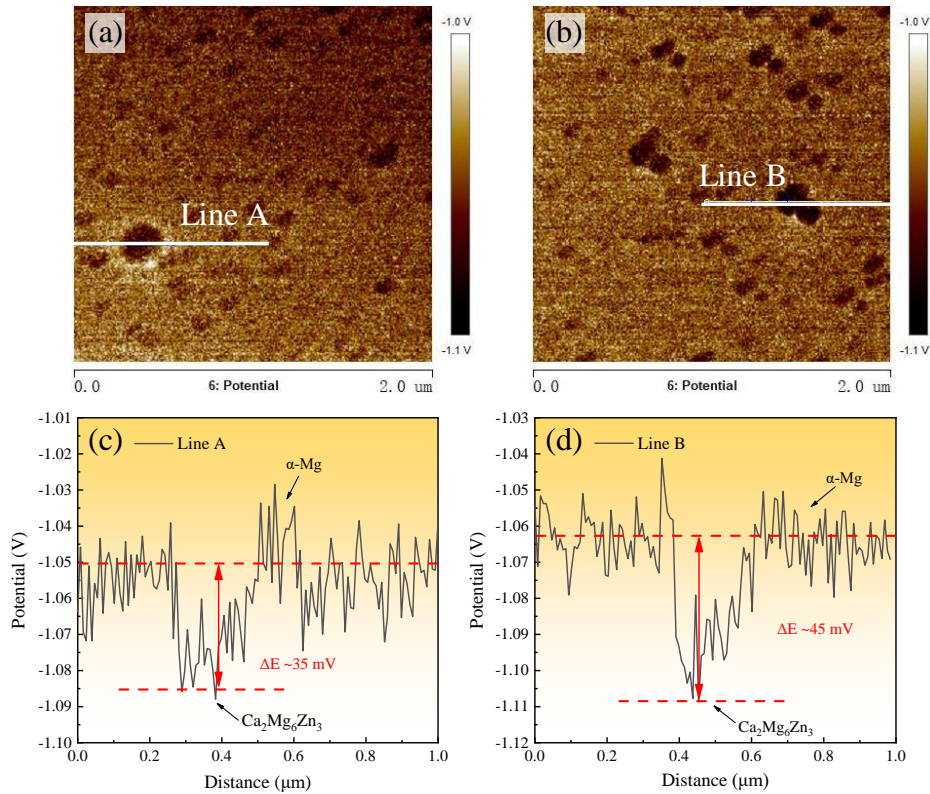
507 XRD results shown in Fig. 16 confirmed the formation of Mg(OH)₂ in the corrosion
508 tests by the presence of characteristic peaks around $2\theta=18.6^\circ$, 50.8° and 62.0° . Thicker

509 corrosion film had been formed on the alloys with a higher Ag content (Fig. 14),
 510 therefore, diminishing the XRD signals from the substrate. Consequently, the relative
 511 intensities of $\text{Mg}(\text{OH})_2$ peaks to α -Mg increased in Fig. 16.



512
 513 **Fig. 16.** XRD patterns of surface films on as-extruded Mg-2Zn-0.2Ca-xAg (x=0, 0.1, 0.3, 0.5
 514 wt.%) alloys after immersion in 0.9 wt.% NaCl solution for 15 days.

515 After characterizing the corroded morphologies of the studied alloys (Fig. 14-15), it
 516 became apparent that the corrosion initiated and propagated around the secondary
 517 phases. The comparative microstructural characterization (Fig. 1-2) suggested less
 518 populous and more refined secondary phases after adding Ag in the Mg-Zn-Ca alloy.
 519 The electrode potential variation across secondary phase particles was measured by
 520 Kelvin probe technique, and the results are shown in Fig. 17. For the Ag-free ZX20
 521 alloy, the potential difference between the secondary phase and the α -Mg matrix was
 522 about 35 mV, whereas incorporating Ag enlarged the value to about 45 mV for the
 523 ZXQ0.5 alloy. It is clear that the micro-galvanic couples were more readily formed in
 524 the Ag containing alloys because of the larger potential differences. A more refined and
 525 populous distribution of the secondary phase in the grain interior of Ag-containing
 526 alloys increased the number of micro-galvanic couples, leading to the increased
 527 corrosion rates for those alloys.



528

529

530

Fig. 17. SKPFM images of as-extruded (a, c) ZX20 alloy and (b, d) ZXQ0.5 alloy: (a, b) surface Volta potential maps and (c, d) corresponding Volta potential profiles

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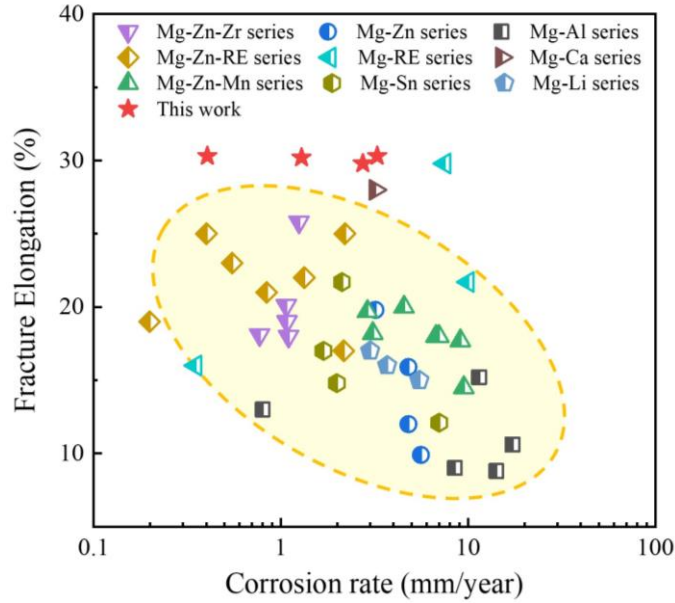
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Fig. 18 provides a comprehensive comparison of mechanical properties (fracture elongation) and corrosion resistance of magnesium alloys reported in the literature [8, 18, 31, 35-42]. The present results indicated that a minor addition of Ag to the Mg-Zn-Ca alloy was detrimental to its corrosion resistance while the mechanical properties maintained roughly unchanged. Nevertheless, the corrosion resistance of the studied alloys was still similar to, and in some cases outperformed, the averaged degradation performance of other magnesium alloys including pure Mg, Mg-0.3Sc and Mg-1.4Al-0.4Mn-0.4Ca-0.3Er alloys known for their superior corrosion resistance. As suggested in the literature [43], a temporary implant should possess balanced mechanical properties and corrosion resistance, with UTS > 200 MPa, FE > 10%, and the corrosion rate < 7 mm/y. Although the corrosion rate of the Mg-Zn-Ca alloy has been increased by Ag addition, it is still suitable for biomedical applications from the standpoint of degradation and mechanical performance.



544

545 **Fig. 18** Elongation to failure of Mg alloys as a function of their corrosion rates [8, 18, 31, 35-42].

546 Additionally, the studied alloys presented superior ductility compared to other Mg
 547 alloys, bringing about additional advantages for biomedical applications associated
 548 with increased ease of manufacturing implants with complex geometries (like stents),
 549 eliminated risks of brittle fracture to improve the reliability of the bioimplants. Overall,
 550 as-extruded Mg-2Zn-0.2Ca-xAg (x=0, 0.1, 0.3, 0.5 wt.%) alloys studied in this work
 551 show favorable combination of mechanical and corrosion properties, making them
 552 promising materials for biodegradable implants.

553 **4. Conclusions**

554 The effects of Ag addition on the microstructure, mechanical properties as well as
 555 corrosion performance of as-extruded Mg-2Zn-0.2Ca (wt.%) alloy were
 556 comprehensively studied. The following conclusions could be drawn:

557 (1) The microstructure of Mg-2Zn-0.2Ca alloy remains almost unchanged with Ag
 558 addition even though Ag promotes dynamic recrystallization, refines the secondary
 559 phase and reduces its volume fraction. Consequently, all studied alloys exhibited
 560 roughly similar mechanical strength, i.e., TYS of ~140 MPa and UTS of ~240 MPa and
 561 exceptional fraction elongation of ~30%.

562 (2) Ag addition enlarged the electrode potential difference between the nobler
 563 secondary phase and the α -Mg matrix, which, together with a less stable corrosion film

564 covering the sample surface, resulted in corrosion resistance progressively deteriorating
565 with increasing Ag content.

566 (3) The ZX20 alloy possessed the lowest corrosion rate (0.40 ± 0.23 mm/y) compared
567 with the Ag-containing counterparts, and an eight-fold higher corrosion rate ($3.27 \pm$
568 0.24 mm/y) was observed for the alloy containing 0.5 wt.% Ag.

569 (4) The corrosion performance as well as the mechanical properties of the Ag-
570 containing Mg-2Zn-0.2Ca alloy exceeded most other Mg alloys. Therefore, it is worth
571 exploring further its feasibility for biodegradable implants.

572 **Data availability statement**

573 The raw and processed data required to support the findings will be made available
574 from the authors upon reasonable request.

575 **Originality statement**

576 The authors confirm that the article has not been submitted to peer review, nor has been
577 accepted for publishing in another journal. The authors also confirm that the research
578 in this work is original, and that all the data given in the article are real and authentic.
579 If necessary, the article can be recalled, and errors corrected.

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