

Article 1 **Development of an oral epithelial** *ex vivo* **organ culture model** ² **for biocompatibility and permeability assessment of biomateri-** ³ \mathbf{a} **ls**

Foteini Machla ¹ , Chrysanthi Bekiari ² , Paraskevi-Kyriaki Monou 3,4, Evangelia Kofidou ² , 5 **Astero-Maria Theodosaki ¹ , Orestis L. Katsamenis 5,6, Vasileios Zisis ⁷ , Maria Kokoti ¹ , Athina Bakopoulou 1,*,** 6 **Dimitrios Fatouros 3,4 and Dimitrios Andreadis 7,*** 7

- ¹ Department of Prosthodontics, Tissue Engineering Core Unit, School of Dentistry, Faculty of Health Sci- 8 ences, Aristotle University of Thessaloniki, Thessaloniki 54124, Greece 9
- ² Laboratory of Anatomy and Histology, Veterinary School, Aristotle University of Thessaloniki, Thessaloniki 10 54124 , Greece 11
- ³ Department of Pharmaceutical Technology, School of Pharmacy, Faculty of Health Sciences, Aristotle Uni-
¹² versity of Thessaloniki, Thessaloniki 54124, Greece 13 and 13
- ⁴ Center for Interdisciplinary Research and Innovation (CIRI-AUTH), Thessaloniki 57001, Greece 14
- ⁵ μ-VIS X-ray Imaging Centre, Faculty of Engineering and the Environment, University of Southampton, 15 Southampton SO17 1BJ, United Kingdom 16
- ⁶ Institute for Life Sciences, University of Southampton, Southampton SO17 1BJ, United Kingdom UK 17
- ⁷ Department of Oral Medicine/Pathology, School of Dentistry, Faculty of Health Sciences, Aristotle Univer- 18 sity of Thessaloniki, Thessaloniki 54124, Greece 19
- ***** Correspondence: A.B. abakopoulou@dent.auth.gr, Tel.: 0030 2310999540; D.A. dandrea@dent.auth.gr, Tel.: 20 0030 2310999538. 21

Abstract: In the present study, a customized device (Epi-ExPer) was designed and fabricated to fa- 22 cilitate **Epi**thelial organ culture, allowing controlled **Ex**posure to exogenous chemical stimuli, and 23 accommodating the evaluation of **Per**meation of the tissue after treatment. The Epi-ExPer system 24 was fabricated using a stereolithography (SLA)-based additive manufacturing (AM) method. Hu- 25 man and porcine oral epithelial mucosa tissues were inserted into the device and exposed to resin- 26 ous monomers commonly released by dental restorative materials. The effect of these xenobiotics 27 on the morphology, viability, permeability, and expression of relevant markers of the oral epithe- 28 lium was evaluated. Tissue culture could be performed with the desired orientation of air-liquid 29 interface (ALI) conditions, and exposure to xenobiotics was undertaken with a spatially guarded 30 and reproducible manner. Among the selected monomers, HEMA and TEGDMA reduced tissue 31 viability at high concentrations, while tissue permeability was increased by the latter. Xenobiotics 32 affected the histological image by introducing vacuolar degeneration of epithelial cells and increas- 33 ing the expression of panCytokeratin (pCK). Epi-ExPer device offers a simple, precise and repro- 34 ducible study system to evaluate interactions of oral mucosa with external stimuli, providing a bi- 35 ocompatibility and permeability assessment tool aiming to an enhanced *in vitro*/*ex vivo*-to-*in vivo* 36 extrapolation (IVIVE) that complies with European Union (EU) and Food and Durg Administration 37 (FDI) policies. 38

Keywords: organ/tissue culture model; oral mucosa *ex vivo* analogue; epithelial barrier; permeabil- 39 ity device the control of t

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1. Introduction 42

The oral mucosa, the mucous membrane lining the mouth cavity, consists of a com- 43 plex multilayered tissue with a protective barrier function, immune-related activity, and 44 specialized functions, such as the production and secretion of saliva. This mucosa 45

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comprises a superficial multilayered epithelium, which can be keratinized, parakeratin- 46 ized, or non-keratinized depending on the location in the oral cavity, separated from the 47 subepithelial compartment by the basement membrane. The subepithelial compartment 48 is composed of various cell types and tissue structures, including adipose, connective, 49 vascular, neural, osseous, and muscular tissues, as well as spherical structures, the minor 50 salivary glands, which are responsible for saliva secretion [1]. Microorganisms, food and 51 environmental components, chemicals, drugs, and dental materials, such as metals and 52 xenobiotics released by resin-based restorative materials, come into contact with the oral 53 epithelium and can permeate it, reaching the subepithelial layers and dispersing system- 54 ically via the blood vessels. Meanwhile, parameters, such as the temperature, time, saliva 55 pH, mechanical forces though mastication or chemical influence, contribute to a multifac- 56 torial environment, further triggering the release of xenobiotics from dental materials into 57 the oral cavity, and leading to significant impacts on local and systemic health and disease 58 $[2-4]$. 59

Taking into consideration the paramount barrier function of the oral mucosa and the 60 continuous development of novel dental materials, as well as drugs with an oral transmu- 61 cosal administration delivery pathway, an unmet need has risen during the past years to 62 develop reliable biocompatibility assessment systems that recapitulate the structure and 63 barrier function of the oral mucosa [5]. These systems aim to serve as alternatives to ani- 64 mal testing, in compliance with EU directives requiring the Replacement, Reduction, and 65 Refinement of laboratory animal use in research and development (3Rs rule) [6], as well 66 as the Food and Drug Administration (FDA) rendering testing in animals optional [7]. 67 While several efforts have been made to develop 3D oral mucosa analogues using tissue 68 engineering approaches, such as epithelial barriers [8–11], full-thickness gingival equiva- 69 lents [10,12–16], and biofabricated full-thickness gingiva-on-chip [17], these models, alt- 70 hough advantageous compared to conventional 2D culture systems, still fall short of fully 71 recapitulating the complex structure and function of the oral mucosa [18,19]. Therefore, 72 the greatest challenge is to develop *ex vivo* systems with an enhanced *in vitro*-to-*in-vivo* 73 (IVIVE) extrapolation ratio. 74

The state-of-the-art in *ex vivo* organ culture system development has employed vari- 75 ous technical approaches so far, such as the plasma clot or watch glass method, the agar 76 gel method, the raft method, and the grid method [20]. Τhese techniques may be used for 77 the *ex vivo* culture of epithelial tissues of different origins, such as intestine, upper respir- 78 atory tract, or skin, either in full contact with the nutrient medium, or in partial contact, 79 i.e. at the air-liquid interface (ALI), as schematically illustrated in Figure 1 [21–23]. Previ- 80 ous techniques for exposing tissue to external chemical stimuli have primarily relied on 81 the droplet (Figure 1F) or cylinder ring methods (Figure 1G) [24]. Unfortunately, the drop- 82 let approach risks displacement during plate transportation, and its geometry may hinder 83 uniform exposure across the tissue. Meanwhile, the cylinder ring method still carries the 84 risk of movement on the epithelial surface, and the grease residue may affect tissue per- 85 meation. The commonly used Franz vertical diffusion chamber system for tissue permea- 86 bility testing has also limitations, such as a high device-to-tissue volume ratio, requiring 87 large tissue samples (diameter > 6mm) that could unnecessarily damage and discomfort 88 the donor area, while also needing large volumes of culture reagents and space [25]. 89 Therefore, the key challenge is to develop a reliable and reproducible system for exposing 90 oral epithelial tissue to biomaterials and/or drugs through the epithelial barrier, followed 91 by accessible post-analysis for permeation studies. 92

Figure 1. Schematic representation of the existing organ/tissue culture models (A-Ε), exposure 94 methods (F, G), and typical permeation assessment model (H). The simplistic immersion of epithe- 95 lial tissue in culture medium (pink) (A) is improved by various culture methods accommodating 96 air-liquid interface (ALI) culture conditions (B-E). The latter included the plasma clot (orange) on 97 watch glass (B), the agar gel (C), the raft made by lens paper/rayon acetate floating on medium (D), 98 and metal grid (E) methods. For epithelial tissue exposure the chemical substances (green) are 99 placed on the outer surface of the epithelium either via the droplet technique (F) or with a cylinder 100 ring (G). Permeation assays are usually performed in Franz vertical chambers (H) where the perme- 101 ated substance (yellow) can be measured (Figure created using BioRender software). 102

Based on the above, in the present study, a customized device (Epi-ExPer) was de- 103 signed and validated to address the unmet need of oral Epithelial organ culture, while 104 allowing controlled Exposure to exogenous chemical stimuli, and facilitating the evalua- 105 tion of Permeation of the tissue after treatments. The Epi-ExPer system was fabricated 106 using a stereolithography (SLA)-based additive manufacturing (AM) method. Human 107 and porcine oral epithelial mucosa tissues were inserted onto the device and exposed to 108 resinous monomers commonly released by dental restorative materials. The effect of these 109 xenobiotics on the morphology, viability, permeability, and expression of relevant mark- 110 ers of the oral epithelium was evaluated. The innovative approach presented in this study 111 offers a simple, precise and reproducible study system of the natural oral mucosa to eval- 112 uate interactions with external stimuli, providing a biocompatibility assessment tool with 113 enhanced IVIVE that complies with EU and FDA policies. 114

A. Epi-ExPer device 116

2.1. Design of the Epi-ExPer device 117

The Epi-ExPer device was designed using the computer-aided design (CAD) soft- 118 ware AutoCAD (Autodesk, CA, USA). It consisted of two interconnectable components: 119 a lower part and an upper part. The lower part aimed to position the tissue at an ALI state 120 and elevate it, allowing for the collection of permeated substances in the underlying well. 121 The upper part was designed to isolate the desired outer surface of the epithelium, ena- 122 bling it to be either left untreated or exposed to potentially toxic stimuli under investiga- 123 tion. Sealing rings were also incorporated through bonding with liquid resin on the cylin- 124 drical ridge of the upper Epi-ExPer part, where the tissue would be stabilized, to seal the 125 defined epithelial area at its periphery. 126

The Epi-ExPer device was designed to precisely fit within the wells of a standard 24- 127 well culture plate, allowing for easy placement of the tissue sample inside a cell incubator 128 during culture, exposure times, and sampling intervals for permeation studies. Addition- 129 ally, the CAD designs were exported as .stl files and imported into the 3D printing man- 130 agement software PreForm® (FormLabs, MA, USA), where mini rafts were generated to 131 provide support for any structurally unsupported components of the design. 132

2.2. Additive manufacturing and assembly of the Epi-ExPer device 133

The CAD device components were fabricated using the SLA 3D printer Form 3B+ 134 (Formlabs, MA, USA), with a layer thickness of 100 μm. The main parts, including the 135 upper and lower compartments, were manufactured using the biocompatible BioMed 136 Clear resin. The elastic sealing rings were produced with the Elastic Resin 50A (both resins 137 purchased from Formlabs, MA, USA). The printing time for the main parts of 10 devices 138 was approximately 40 minutes (min), while the sealing rings for 30 devices took around 139 30 min. 140

The printed parts were then washed with isopropyl alcohol (IPA) in the FormWash 141 washing chamber (Formlabs, MA, USA), with the main parts washed for 20 min and the 142 sealing rings for 10 min. After allowing the parts to fully dry from the IPA, the sealing 143 rings were attached to the edge of the cylinder on the upper parts that contact the tissue. 144 The sealing rings were then chemically bonded to the upper part using BioMed Clear liq- 145 uid resin, aided by a fine-tipped bonding applicator (Imicryl, Konya, Turkey). The assem- 146 bled parts were further polymerized in the FormCure polymerization device (Formlabs, 147) MA, USA) for one hour at 60 °C. The supporting raft of the lower parts was removed using 148 a clipper. 149

The Epi-ExPer devices underwent disinfection by immersing them in 70% ethanol for 150 15 min, followed by washing with sterile deionized water (3 times x 5 min) and exposure 151 to ultraviolet radiation for 30 min. Thereafter, the devices were stored in 24-well plates 152 until ready for use. 153

B. Evaluation of toxic stimuli on the Epi-ExPer device 154

This study was approved (protocol number 62460/2022) by the Ethics and Research 155 Committee of Aristotle University of Thessaloniki (AUTh) and the Ethics Committee of 156 the School of Dentistry, AUTh (protocol number 54/14-03-2022). 157

2.3. Epithelial organ/tissue biopsy and cultivation 158

Human normal oral mucosa tissues with non-keratinized/parakeratinized epithe- 159 lium from the adjacent alveolar mucosa of $3rd$ molars were obtained from healthy patients 160 during their routine extractions and after patients' informed consent in the Department of 161 Dentoalveolar Surgery, Implantology and Oral Radiology, School of Dentistry, AUTh. 162 Porcine oral buccal non-keratinized/parakeratinized epithelium was also provided and 163 excised by local slaughterhouse, during the first 2 h after exhaustion. Human or porcine 164 biopsies that were cultivated on the Epi-ExPer devices, were obtained using a 5 mm cir- 165 cular biopsy punch (Kai Medical, Solingen, Germany). 166

The oral epithelial tissues were transferred to the laboratory, in ice-cold complete 167 culture medium (CCM) containing 2X antibiotics/antimycotics, where they were asepti- 168 cally treated in a laminar flow cabinet and cultivated in cell culture incubator (37°C, 5% 169 CO2, relative humidity). The CCM consisted of DMEM: F-12 medium, enriched with 10% 170 fetal bovine serum (FBS), 100 U/ml penicillin, 0.1 mg/ml streptomycin and 0.25 μg/ml am- 171 photericin B (all from PAN Biotech, Aidenbach, Germany). 172

The cultivated tissues were placed inside the lower part of the Epi-ExPer device. The 173 upper part was then assembled on top of the tissue, and three rubber bands were used to 174 secure it in place, holding the upper part, tissue, and lower part together. Each tissue- 175 loaded Epi-ExPer device was then placed in a 24-well plate. CCM was added to each well 176 surrounding the device, so the tissue was in contact with but not submerged in the CCM. 177 During the exposure-free culturing period, the outer surface of the epithelial tissue was 178 left exposed to air, allowing the tissue to be cultured under ALI conditions. 179

2.4. Exposure of the epithelial tissue to common toxic stimuli 180

Epithelial tissues were placed on Epi-ExPer devices and were exposed to commonly 181 released toxic resinous monomers, i.e. (Hydroxyethyl)methacrylate (HEMA) and Tri- 182 ethylne glucol dimethacrylate (TEGDMA). Two monomer concentrations were evaluated: 183

0.5 mM (TEGDMA-low), and 3 mM (TEGDMA-high) for TEGDMA, and 1 mM (HEMA- 184 low) and 4 mM (HEMA-high) for HEMA. Both monomers were firstly dissolved in etha- 185 nol (EtOH) to create a 2 M stock solution. Then, the selected final concentrations were 186 reached by diluting the 2 M solutions at minimum 1: 400 to CCM, ensuring the final eth- 187 anol concentration did not exceed 0.25% v/v. Tissues loaded on the Epi-ExPer devices 188 were exposed to 30 μl monomer per tissue. The receptor compartment volume of the Epi- 189 ExPer device was 2.4 ml and was filled either with CCM for tissue culture or with Hank's 190 balance salt solution (HBSS) for permeation studies. 191

2.5. Transepithelial permeation of Calcein 192

The effect of the resinous monomers (HEMA-low, HEMA-high, TEGDMA-low, and 193 TEGDMA-high) on the permeability of porcine epithelial tissues was evaluated via the 194 transepithelial permeation of calcein. Porcine oral epithelial tissues were mounted on the 195 Epi-ExPer devices $(n=3)$, and the external surface of the epithelial tissues was exposed for 196 2.5 or 24 h to 30 μl of each of these substances. Tissues exposed only to CCM, or to 0.25 197 v/v % EtOH in CCM acted as blank (CCM) and negative controls (Control) respectively. 198 The lower part of the tissue was in contact with CCM. Then, the monomers were replaced 199 by the same amount of calcein solution (1 μ g/ml), while the CCM of the lower compart- 200 ment was replaced by HBSS. Samples of the permeated calcein in the lower compartment 201 were taken at 10-, 20-, 30-, 60-, 90-, 120-, 180-, and 240-min intervals, and were analyzed 202 using a spectrofluorometer (RF-5301-PC Fluorescence Spectrophotometer, Shimadzu, 203 Kyoto, Japan). The parameters of steady-state flux (Jss) and apparent permeability coeffi- 204 cient (Papp) were calculated and analyzed. Jss indicated the slope of the plot of the per- 205 meated calcein against time and the Papp calculated as dividing the Jss by the Cd, where 206 Cd indicates the concentration of calcein of the upper compartment. 207

2.6. Effects of resinous monomers on tissue viability 208

The effect of HEMA-low, HEMA-high, TEGDMA-low, and TEGDMA-high on the 209 viability, as expressed by the measurement of the metabolic activity of the porcine epithe- 210 lial tissue was evaluated via the MTT [3-(4,5-dimethylthiazol-2-yl)-2,5-diphenyltetrazo- 211 lium bromide] assay. At first, the tissues were weighted, then placed on Epi-ExPer de- 212 vices, and exposed to the monomers for 2.5- or 24h. Tissues exposed only to 0.25 v/v % 213 EtOH in CCM acted as the Control, while tissues exposed to absolute 100° EtOH acted as 214 positive control (PC). After exposure, the specimens were treated with 5 mg/mL ΜΤΤ so- 215 lution (Life Technologies, California, USA) for 4 h, and then, the formed formazan was 216 dissolved in dimethyl sulphoxide (DMSO), for 1 h, at 37 °C. Optical density (OD) was 217 measured at 545 nm with a reference filter of 630 nm against blank (DMSO) using a mi- 218 croplate reader (Epock, Biotek, Vermont, USA). The percentage (%) OD/tissue weight val- 219 ues compared to the baseline OD of the Control were calculated and statistically analysed 220 (*n*=4). 221

2.7. Histological assessment 222

The effect of the resinous monomers on the morphology and structure of human and 223 porcine epithelial tissues assessed on the Epi-ExPer device was evaluated via Hematoxy- 224 lin and Eosin (H&E staining). Human and porcine tissues were exposed to the relevant 225 monomers for 2.5- or 24 h, respectively. Tissues exposed in 0.25 v/v % EtOH in CCM acted 226 as Control. The tissues were fixed using 4% paraformaldehyde (PFA) solution for 72 h, 227 gradually dehydrated using serial EtOH dilutions, and embedded in paraffin blocks. 228

2.8. Whole mount architecture evaluation via 3D X-ray Histology 229

X-ray microfocus Computed Tomography (μCT)-based 3D X-ray Histology 230 (https://xrayhistology.org) [26], was employed to conduct whole -block imaging and 231 study the microstructure of the specimen prior to any physical sectioning. XRH imaging 232

was performed at 80 kVp using a custom Nikon XTH 225 ST system (Nikon Metrology, 233 UK) at an isotropic voxel size of 6 μm; a geometric magnification of 25x. After acquisition, 234 the raw radiographic data were reconstructed into 32-bit .vol files using the system's built- 235 in filtered back projection reconstruction software. 236

Following reconstruction, a 3D median filter with a $2 \times 2 \times 2$ kernel was applied to the 237 dataset, followed by a 2D unsharp mask with a Gaussian blur factor of 2 pixels. These 238 filtering steps, conducted using custom scripts, were essential for enhancing the signal- 239 to-noise ratio, which is crucial for visualisation. The pre-processed datasets were then im- 240 ported into Dragonfly software (Comet Technologies Canada Inc.) for visualisation. In 241 Dragonfly, an image moments filter (Kernel size 11) was applied to further denoise the 242 dataset and improve the contrast-to-noise ratio, allowing for clearer visualisation and de- 243 lineation of the tissue from the surrounding wax. 244

Trained researchers, experienced in interpreting XRH data, inspected the volumetric 245 histology images using orthogonal cross-sectional views and 3D volume visualisations. 246 Representative cross-sectional views passing through the middle of the exposed area were 247 selected for presentation, as they capture both exposed and unexposed regions. These 248 planes clearly show the epithelium as well as the underlying lamina propria. 249

Additionally, Maximum Intensity and Minimum Intensity 2.5D (thick slice modes) 250 images with a slice thickness of 200 μm were used to capture attenuation information 251 across multiple slices. These modes offer a valuable overview of tissue features that it is 252 otherwise invisible in single-slice renderings. Thick-slice viewing is a technique that al- 253 lows the voxel intensity of multiple consecutive slices within a 3D dataset to be rendered 254 onto a single slice, based on specific criteria or operations; here the Average Intensity and 255 Minimum Intensity projections [26]. A thick-slice image represents the result of these cri- 256 teria or operations. 257

2.9. Histological sectioning and imaging 258

Paraffin blocks, after scanned with the 3-D X-RAY μCT system, were sectioned with 259 the use of a paraffin microtome (Microm, LabX, Canada). Obtained 10 μm thick sections 260 were stained with H&E and observed under a light microscope (Nikon Eclipse 80i micro- 261 scope, Nikon Instruments Inc, Japan). 262

High resolution, Η&Ε stained, whole slide images were captured after scanning the 263 whole section with the Microvisioneer software (Microvisioneer GmbH, Germany) and a 264 Nikon D-eclipse C1 camera (Nikon Instruments Inc. Melville, USA) was used for captur- 265 ing images at higher magnifications (x 10 and x 20). 266

2.10. Immunofluorescence (IF) 267

The effect of the monomers on the expression of specific markers of human or porcine 268 epithelial tissue was evaluated via IF. Sections of the above-mentioned paraffin embedded 269 tissues were further assessed. The anti-pCK primary antibody was used for overnight in- 270 cubation of the specimens at $4^{\circ}C$ (1:50, mouse, IgG monoclonal AE1/AE3, Origene Tech- 271 nologies Inc., MD, USA). Then, the following secondary antibody in a buffer of 2 % Bovine 272 serum albumin in PBS was conjugated to the relevant primary antibody for 1 h at RT: anti- 273 mouse, goat IgG, Ex/Em: 490/ 525 nm at a 1: 500 dilution (Biotium, Hayward, CA, USA). 274 The tissue was finally observed under a confocal laser scanning microscope (Nikon EZ- 275 C1, CLSM), and further analyzed by the Ez-C1-3.20 software (Nikon Instruments Inc., 276 Amstelveen, The Netherlands). 277

2.11. Statistical analysis 278

Statistical analysis was performed using the Prism 8 (GraphPad, California, USA) 279 software. The statistical significance was set at $p < 0.05$. Two-way ANOVAs for the factors 280 of time and treatment were performed, to analyze the results of calcein permeation and 281

MTT assays, that were followed by Tukey's post-hoc tests. Data were expressed as means 282 ± standard deviation (SD). 283

3. Results 284

3.1. Design of Epi-ExPer device 285

The CAD schemes of the Epi-ExPer device, designed to precisely fit into a 24-well 286 plate, are illustrated in Figure 2. The upper part (Figure 2A) features an open cylinder 287 with an inner diameter of 3 mm, which provides a free surface area of 28.3 mm² for ALI 288 culture or exposure of the multilayered epithelium to tested substances in solution. The 289 outer diameter of the cylinder is 4.5 mm, resulting in a 1.5 mm width between the inner 290 and outer surfaces. On this area, an elastic sealing ring is attached to stabilize the tissue 291 (Figure 2 A.c). 292

The lower part was designed with a 3 mm-diameter free area (Figure 2B.c), allowing 293 the tissue to receive nutrients from the culture medium (CCM) that fills the culture well 294 up to the tissue level. This enabled the permeated substances to perfuse through the entire 295 tissue and be collected in the underneath area for further quantification. Additionally, the 296 upper part was designed with an inner diameter of 5 mm (Figure 2B.a), allowing the open 297 cylinder to glide inside during the assembly of the tissue and device (Figure 2H). 298

299

Figure 2. CAD designs of the Epi-ExPer device. The upper (A) and lower (B) parts with their com- 300 partments (A.a-c and B.a-e) and their role are described. Scale bars indicate 3 mm. The relevant 301 position (C) of the upper and lower part, where the assembling direction is indicated with yellow 302 dash line, and the placement of the rubber bands with the yellow circles. The upper view of the 303 upper (D) and lower (E) parts, and the side views (F and G) are depicted. The assembled device 304 with an animated epithelial tissue is illustrated (H). 305

3.2. Manufactured and assembled Epi-ExPer device 306

The manufactured parts of the Epi-ExPer device are shown in Figure 3 (A-C), and 307 then as assembled with the tissue and placed in the 24-well (Figure 3 D-F). The receptor 308 compartment, which is the space under the lower part and restricts the movement of the 309 upper part, can accommodate a 2.4 ml volume of liquid. Similarly, 2.4 ml of HBSS is ex- 310 pected to be added to the 24-well plate surrounding the Epi-ExPer device to measure the 311

permeation of substances under study. The open well of the upper part can hold up to 30 312 μl of liquid. 313

Figure 3. Photographs of the additively manufactured via stereolithography Epi-ExPer device. Up- 315 per (A), lower (B, C) parts, and the assembled device loaded with epithelial tissue (D-E) inside a 24- 316 well plate (F). 317

3.3. Transepithelial permeation of Calcein assay 318

The permeation of calcein results for the different treatments of the porcine epithelial 319 tissues on the Epi-ExPer device are shown in Figure 4. During the 2.5 h of treatment, no 320 statistically significant differences at the amount of the permeated calcein, and the rele- 321 vant Jss and Papp parameters were observed among the groups (p>0.05). During the 24 h 322 exposure period, the permeation of calcein was increased between the PC and all the other 323 groups at the 90 min measurement and continuing thereafter (all p<0.0001). Additionally, 324 the TEGDMA-high group exhibited significantly elevated calcein permeation at the 240- 325 minute timepoint compared to every other group (p<0.0001). The effect of TEGDMA-high 326 on the permeability of the porcine epithelial tissue was confirmed by the parameters of 327 Jss and Papp, that were statistically significant compared to the Control (p<0.0001). 328

Figure 4. Permeation of calcein on porcine tissue loaded on Epi-ExPer device after 2.5 and 24 h of 330 exposure to HEMA-low, HEMA-high, TEGDMA-low, and TEGDMA-high. Treatment with the un- 331 der study resinous monomers after 2.5 h (A) and 24 h (B), and the Jss (C) for both time points are 332 depicted. The CCM group was exposed only to culture medium, the Control group was exposed to 333 0.025% EtOH/CCM, which is the diluent of HEMA and TEGDMA, while the positive control (PC) 334 group was treated with 100° EtOH. Asterisks indicate statistically significant differences between 335 the tested materials compared to the relevant Control (****p \leq 0.0001). 336

The parameters Jss and Papp for the permeation of calcein are presented in Table 1. 337

314

Group	$Js \cdot 10^{-4} \pm SD$	P_{app} \cdot 10 ⁻⁶ \pm SD
	$(\mu g \times cm^{-2} \times min^{-1})$	$(cm \times h^{-1})$
$CCM - 2.5h$	0.72 ± 0.18	1.97 ± 0.14
$Control - 2.5h$	0.49 ± 0.04	2.90 ± 0.71
$HEMA$ -low $-$ 2.5h	0.55 ± 0.05	2.19 ± 0.21
$HEMA-high-2.5h$	0.44 ± 0.05	1.76 ± 0.20
$TEGDMA$ -low – 2.5h	0.53 ± 0.10	2.11 ± 0.42
$TEGDMA$ -high $-2.5h$	0.72 ± 0.46	2.87 ± 1.85
$EtOH - 2.5h$	0.66 ± 0.21	2.66 ± 0.84
$CCM - 24h$	0.98 ± 0.58	3.94 ± 2.31
Control – 24h	0.61 ± 0.04	2.46 ± 0.14
HEMA-low - 24h	0.85 ± 0.45	3.40 ± 1.80
$HEMA-high-24h$	2.56 ± 2.73	10.25 ± 10.92

Table 1. The steady-state flux (Jss) and the apparent permeability coefficient (Papp) for the calcein 338 permeation through porcine oral buccal mucosa loaded on the Epi-ExPer device, after 2.5 and 24 h 339 of exposure to two concentrations of the resinous monomers HEMA and TEGDMA. 340

3.4. Effect of resinous monomers on tissue viability 341

The viability of the epithelial tissues (Figure 5) was affected by the tested resinous 342 monomers in a concentration- and time-dependent manner. After 24 h of treatment, 343 HEMA-high reduced tissue viability to 74.4 ± 7.6 %, while TEGDMA-high decreased it to 344 53.1 ± 3.1% (both p ≤ 0.0001). The positive control, treated with absolute ethanol, exhibited 345 a drastic reduction of tissue viability down to $10.8 \pm 1.1\%$ (p ≤ 0.0001). However, no statis-346 tically significant changes in viability were observed during the 2.5-hour treatment period 347 $(p > 0.05)$. 348

TEGDMA-low – 24h $\begin{array}{|c|c|c|c|c|} \hline 0.44 \pm 0.07 & 1.77 \pm 0.27 \hline \end{array}$ **TEGDMA-high – 24h** $\begin{array}{|l} 7.38 \pm 0.50 \end{array}$ 29.51 \pm 1.98 **EtOH** – 24h 16.73 ± 5.50 66.91 ± 21.98

Figure 5. Tissue viability (*n* = 3) after exposure to HEMA and TEGDMA for 2.5 h (black columns) 350 and 24 h (grey columns). Mean values are annotated above each column and asterisks indicate sta- 351 tistically significant differences between the tested materials compared to the relevant control (****p 352 \leq 0.0001). 353

3.5. Whole mount architecture evaluation via 3D X-ray Histology 354

XRH results are presented in Figure 6 for both the human and porcine tissue experi- 355 ments, comparing the control and the most damaged sample exposed to high concentra- 356 tion TEGDMA treatments. The 3D micrographs (Figure 6 – bottom row) illustrate the tis- 357 sue delineated from the wax in relation to the histology cassette, prior to any physical 358 sectioning. In all images, the indentation of the cylindrical well is clearly visible, outlining 359 the exposed epithelium area in the centre, with the unexposed tissue surrounding this 360 confined space. 361

A comparison between the Control and TEGDMA-high treatments for both human 362 and porcine specimens indicate the influence of the chemical compounds on the epithe- 363 lium; also see supplementary video A1. Additionally, the underlying deeply located con- 364 nective tissue shows areas of lower attenuation, which result from the presence of loosely 365 packed collagenous/fibrous tissue components and adipose tissue. These darker, lower- 366 density areas are particularly apparent in the 200 μm Average Intensity projection and the 367 Minimum Intensity projections across all TEGDMA-high samples. 368

A closer examination of the zoomed-in inserts (outlined with dashed lines) reveals 369 that this looser organization of stromal tissues is more apparent by lower attenuation ar- 370 eas (darker regions in the exposed to the resinous monomers areas (Figure 6 b2), as com- 371 pared to the control (Figure 6 a), and in situ control samples (Figure 6 b1), depending on 372 the site of the biopsy. 373

Figure 6. 3D X-ray Histology imaging of Human and Porcine Oral Mucosa. Comparison of control 375 and high-concentration TEGDMA-treated tissues for both human and porcine oral mucosa samples. 376 The top and middle rows $(a-g)$ show 200 μ m thick slice projections for Average Intensity (top row) 377 and Minimum Intensity (middle row), highlighting tissue microstructure. Insets provide zoomed- 378 in views of the dash-line outlined areas. Insets (b1, b2) provide zoomed-in views of the exposed (b2) 379 and adjacent unexposed ("in situ control," b1) areas of the human TEGDMA high sample shown in 380 b. 3D reconstructions (h –k) illustrate the whole tissue, delineated from the wax before any physical 381 sectioning, where the indentation of the cylindrical well is clearly visible, outlining the exposed 382 epithelium area in the center. 383

Whole section histological imaging was performed to further elucidate the XRH find- 384 ings and the nature of the lower attenuation areas. This microscopic evaluation assessed 385 the effect of the resinous monomers on the tissue integrity of the previously $3D X-ray \mu CT$ 386 scanned oral mucosa specimens, from both human and porcine origins. The scanning re- 387 vealed that resinous monomers evoked severe disorganization and cell damage in the ep- 388 ithelial layer, while having no effect on the underlying lamina propria. The collagen fibers 389 in the lamina propria maintained their normal orientation, architecture, and density. 390 Furthermore, a well-organized area of connective tissue was observed in close proximity 391 to the basal epithelial membrane of all samples, excluding the possibility of connective 392 tissue destruction by TEGDMA and HEMA. The areas of loose organization in the deeper 393 layer of the lamina propria are a result of the tissue's physiological architecture, further 394 accentuated by the surgical handling and experimental procedures. These areas became 395 more obvious in the exposed samples, most likely due to the disorganization of the epi- 396 thelial layer, which made them frailer during handling. 397

Figure 7. Whole section histological scanning images of human (A) and porcine (B) oral mucosa 399 specimens exposed to high concentrations of resinous monomers, previously scanned with the 3D 400 X-ray μCT (Figure 6). The human mucosa exhibited severely altered cell morphology and cell dam- 401 age due to extensive vacuolation in the upper two-thirds of the epithelium, (a1). Similar, though less 402 pronounced (covering only half of the epithelium), lesions were observed in the porcine epithelium 403 $(b1)$. In contrast, the underlying lamina propria was not substantially affected in either the human 404 or porcine mucosa respectively (a2 and b2), and there were no significant alterations in collagen 405 band density or tissue disruption**.** 406

3.6. Histological and IF analyses of exposed human epithelial tissues 407

H&E staining of human epithelium revealed that treatment with HEMA led to mild 408 disorganization of the superficial epithelial layer, as well as focal intraepithelial edema 409 and epithelial vacuolation in the lower epithelial layers. In contrast, treatment with 410 TEGDMA, particularly at higher concentrations, resulted in a more diffuse disruption of 411 the upper epithelial layer and extended vacuolation and degeneration of epithelial cells 412 in the lower epithelial layers, compared to the control. 413

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Figure 8. H & E photomicrographs of 10 μm human oral mucosa sections, treated with 0.25 % v/v 415 EtOH in CCM (A and a), HEMA-low (B and b), HEMA-high (C and c), TEGDMA-low (D and d) or 416 TEGMA-high (E and e). Treatment with HEMA and TEGDMA for 2.5 h resulted in severe disorgan- 417 ization of normal tissue architecture $(C - E)$ with altered cellular morphology of epithelial cells (c - 418) e). Vacuolar degeneration of epithelial cells was observed at high HEMA and TEGDMA 419

concentrations (c and e) pointing to their dose-dependent effect, as higher concentrations of both 420 resins resulted in more severe cellular and tissue damage. Scale bar = 100μ m. 421

The observed effects on epithelial tissue were more evident with IF, after staining 422 with the pCK marker and visualization by CLSM. Specifically, the dose-dependent corro- 423 sive impact of HEMA and the even more pronounced effect of TEGDMA, causing severe 424 disruption of epithelial architecture and induction cellular vacuolation, were clearly evi- 425 dent as compared to normal human epithelial tissues. 426

Figure 9. CLSM photomicrographs of 10 μm human oral mucosa sections stained against the anti- 428 pCK. Oral mucosa specimens placed in the Epi-ExPer device were either treated with 0.25% v/v 429 EtOH in CCM (A and a), HEMA-low (B and b), HEMA-high (C and c), TEGDMA-low (D and d), or 430 TEGMA-high (E and e). Treatment with HEMA and TEGDMA for 2.5 h, resulted in epithelial atro- 431 phy (C - c and E - e), altered morphology (D and d) and vacuolar degeneration of epithelial cells (C 432 and c), and severe de-organization of the normal tissue architecture. HEMA and TEGDMA effect 433 on the integrity of oral epithelium was dose-dependent, as higher concentrations of both resinous 434 monomers resulted in more severe cellular and tissue damage. Scale bar = 100 μm. 435

3.7. Histological and IF analyses of exposed porcine epithelial tissues 436

When porcine buccal mucosa with non-keratinized/parakeratinized epithelium was 437 treated with HEMA at low and higher concentrations, a diffuse vacuolation of epithelial 438 cells in several layers was observed. However, in contrast to human epithelium, no disor- 439 ganization of the upper epithelial layer was noticed compared to the non-exposed con- 440 trols. Conversely, the influence of both lower and higher concentrations of TEGDMA in 441 porcine buccal mucosa led to extended disorganization of the upper epithelial layer and 442 vacuolation of the underlying epithelial cell layers. 443

Figure 10. H & E photomicrographs of 10 μm porcine oral mucosa sections treated with 0.25% v/v 445 EtOH in CCM (A and a), HEMA-low (B and b), HEMA-high (C and c), TEGDMA-low (D and d), or 446 TEGMA-high (E and e). Treatment with HEMA (B, C) and TEGDMA (D, E) for 24 h, resulted in 447 severe disturbance of epithelial architecture, altered cellular morphology in TEGDMA-treated mu- 448 cosa (d and e) and vacuolation of epithelial cells (b, c and d, f for HEMA and TEGDMA respectively), 449 even at deeper epithelial layers. TEGDMA posed a more severe effect on epithelial integrity, even 450 at low concentrations (D and E). Scale bar = 100μ m. 451

Figure 11. CLSM photomicrographs of 10 μm porcine buccal mucosa sections stained against anti- 453 pCK. Oral mucosa specimens were either treated with 0.25% v/v EtOH in CCM (A and a), HEMA- 454 low (B and b), ΗΕΜΑ-high (C and c), TEGDMA-low (D and d), or TEGMA-high (E and e). Treat- 455 ment with HEMA and TEGDMA for 24 h, resulted in in epithelial atrophy $(C - E$ and $c - e$), altered 456 morphology of epithelial cells and severe disturbance of epithelial architecture. TEGDMA induced 457 a more severe effect on epithelial integrity, even at low concentrations (D and d). HEMA and 458 TEGDMA effect on the integrity of oral epithelium was dose-dependent, as higher concentrations 459 of both resins resulted in more severe cellular and tissue damage. Scale $bar = 100 \mu m$. 460

4. Discussion 461

The ongoing advancement of novel dental materials that interact with human oral 462 mucosa, along with the emergence of new trans-mucosal drug delivery systems, necessi- 463 tates rigorous evaluation of these new agents [27–29]. Assessing the impact on the struc- 464 tural integrity, viability, and permeability of oral mucosa is critical, and therefore the de- 465 velopment of reliable assessment tools is essential. Engineered oral mucosal equivalents 466 have been developed for clinical use, as well as for *in vitro* studies of biocompatibility, 467 mucosal irritation, disease, and other fundamental oral biological processes [11,12,30,31]. 468 Besides, multiple studies have described the successful construction of full-thickness en- 469 gineered human oral mucosa through the cultivation of oral keratinocytes with or without 470 fibroblasts on collagen substrates [12–16], as well as dynamic oral mucosa cultures on-a- 471 chip [17]. Although significant advancements have been made, these engineered systems 472 still fall short of accurately mimicking the complex barrier functions and microenviron- 473 ment of the native oral epithelium. Yet, this level of biomimicry is often crucial for the 474 spatiotemporal evaluation of host-material interactions and responses that reflect both 475 healthy and diseased states. 476

This study introduces the Epi-ExPer device, developed to address certain limitations 477 of tissue engineering models and two-dimensional cell cultures as alternatives to i*n vivo* 478 animal testing. The Epi-ExPer device aims to provide a reliable platform for the preclinical 479 evaluation of new dental materials and oral care products, investigation of oral patholo- 480 gies, and study of fundamental biochemical and biophysical processes in oral tissues. 481

The Epi-ExPer device was designed to provide a reliable, easy-to-use, and practical 482 tool for *ex vivo* oral mucotoxicity studies. The first goal was to integrate multiple function- 483 alities, including tissue culture, exposure, and permeability evaluation, into a single 484

device. Once the epithelial tissue is assembled, no additional equipment is needed for ex- 485 posure (e.g. clone ring), and the tissue does not require transfer to another device for sub- 486 sequent permeability evaluation (e.g. Franz chambers). Another aim was to enable a more 487 sustainable, high-throughput approach for *ex vivo* testing compared to existing models, 488 by designing the device to fit in standard 24-well culture plates [32]. This reduces the re- 489 quired tissue area and reagents' volume, while increasing the experimental data-to-re- 490 sources ratio. 491

The device was designed to maintain the natural orientation of the epithelial tissue 492 during the culture stage. The lower part of the device accommodates an ALI potential, 493 where the epithelium is in contact with the air and the underlying lamina propria is immersed in culture medium [33–35]. This setup closely mimics the clinical conditions, as 495 the agents to be evaluated, such as dental materials, microbial agents, or drugs, come into 496 contact only with the epithelial side of the tissue [36]. 497

The Epi-ExPer device incorporates a compartmentalization feature inspired by a 498 modified skin culture system suggested by Companjen et al. [37]. The authors perforated 499 the filter of a culture insert and placed the dermis of the tissue through the hole, while the 500 epidermis was positioned higher than the filter level, exposing only that area to the factors 501 under study. Similarly, the Epi-ExPer device has an upper well that remains empty during 502 the ALI culture of the tissue but is filled with the agents to be evaluated during the expo- 503 sure experiments. This upper well provides controlled exposure to exogenous factors, 504 without the risks associated with other techniques, such as the movement inherent in 505 droplet exposure or the potential for sealing material residues that can occur with the 506 clone ring technique [24]. 507

Although the Franz vertical diffusion chambers are considered the gold standard for 508 *ex vivo* permeation testing [38,39], the literature has highlighted several shortcomings, in- 509 cluding the relatively large volumes of reagents they require, their bulky size, and their 510 fragility [40]. Many variations of the Franz chamber have been introduced, but their 511 scopes and intended usages differ from the Epi-ExPer device developed in this study. For 512 example, Sil et al. fabricated non-fragile, cost-effective Franz chamber analogues using 513 SLA AM [25], while Munt et al. developed a diffusion chamber targeting the examination 514 of topical spray formulations [40]. Neil et al. used vertical Franz diffusion chambers as 515 culture platforms and demonstrated the successful long-term culture of human skin be- 516 yond 9 days [41]. In contrast, the Epi-ExPer device was developed using a bottom-up de- 517 sign approach specifically aimed at optimizing the culture, exposure, and permeation 518 evaluation of human oral mucosa. **519** Separation of human oral mucosa.

The Epi-ExPer device was used to assess the biocompatibility of dental materials. For 520 this purpose, HEMA and TEGDMA were selected, as they are the most released xenobi- 521 otics from resin-based dental restorative materials that come into direct or indirect contact 522 with oral mucosa [42,43]. These monomers have been extensively studied for their biolog- 523 ical effects *in vitro* [44–46]. The time points of 2.5 and 24 hours were chosen based on phar- 524 macokinetic studies, which have shown that after *in vivo* oral application of resinous mon- 525 omers, the highest concentrations are detected during the first few hours, while they are 526 almost eliminated by 24 hours [47,48]. To the best of the authors' knowledge, there is no 527 previous study that has evaluated the effects of these two dental resinous monomers, 528 HEMA and TEGDMA, on *ex vivo* oral mucosa. 529

In the present study, porcine oral buccal samples were used alongside human biop- 530 sies to evaluate histological alterations and pCK expression of oral mucosa, as porcine 531 tissue has been found to most closely resemble human oral mucosa in terms of permea- 532 bility [49]. The porcine mucosa has a greater number of epithelial layers compared to hu- 533 mans [50]. Consequently, the human oral mucosa tissue was exposed for 2.5 h, while the 534 porcine oral mucosa was exposed for 24 h. The increased thickness of the porcine oral 535 epithelium may contribute to the resilience of the tissue to the evaluated resinous mono- 536 mers. The study findings indicate that the impact of both monomers was dose-dependent, 537 with higher concentrations resulting in more pronounced changes. Additionally, 538

TEGDMA appeared to cause more severe lesions compared to HEMA, though both mon- 539 omers induced changes in the mucosae. A combination of 3D X-ray Histology followed 540 by whole section scanning of high resolution, Η&Ε stained, whole slide images revealed 541 that the observed lesions were restricted into the epithelium, without causing any adverse 542 effects or histological changes in the architecture of the underlying lamina propria, other 543 than those related to surgical handling and experimental post-analysis. High-Throughput 544 3D X-Ray Histology can be a very useful and well-established method to be used in cases 545 seeking to locate the lesions in a complex whole mount sample, containing both exposed- 546 (tissue area delimited within the exposure ring of the Epi-ExPer device) and unexposed 547 (*in situ* control, i.e. area on the outer surface of the Epi-ExPer ring) areas (Figures, 6 and 548 7), providing valuable information for the subsequent histological sectioning and analysis 549 $[26]$. 550

For the toxicity evaluation, the MTT assay was performed, which is one of the most 551 used assays to determine cell viability for both *in vitro* and *ex vivo* testing [51,52]. Accord- 552 ing to the Organisation for Economic Co-operation and Development (OECD) Guidelines 553 for the Testing of Chemicals (TG431 and 439), the MTT assay is an essential tool for estab- 554 lishing a reconstructed human epidermis model [29,53]. In a previous study by Wang et 555 al., the researchers conducted the MTT assay, along with permeability testing and histo- 556 logical analysis, to determine the most suitable *ex vivo* animal model for mimicking human 557 mucosa, supporting the use of porcine models [54]. In the present study, the MTT assay 558 was conducted on porcine mucosa after 2.5 and 24 h of exposure to assess the toxic effects 559 of HEMA and TEGDMA at different concentrations. Negative and positive controls were 560 tested in accordance with the OECD Guidelines. The results showed that the highest con- 561 centrations of HEMA and TEGDMA had the greatest negative impact on tissue viability, 562 which was expected based on relevant *in vitro* cell culture studies reported in the literature 563 [55,56]. 564

Permeability assays are commonly conducted in drug delivery studies, as they pro- 565 vide insights into the continuity of the epithelium, which can serve as an indirect assess- 566 ment of the impact of a toxic substance. The Franz diffusion cell is considered the state-
567 of-the-art permeability test, as it is a static device consisting of a donor and a receiver 568 chamber, allowing for the evaluation of a specific substance's permeation through tissue 569 in both *in vitro* and *ex vivo* models [57,58]. Most studies in literature employ the Franz cell 570 as their primary permeability assay [59–61]. For example, Elefteriadis et al. used a buccal 571 bovine model in Franz diffusion cells to assess the performance of a mucoadhesive buccal 572 film for the simultaneous delivery of lidocaine and ketoprofen [62]. Similarly, Farias et al. 573 utilized the Franz cell setup to study the permeation of a composite polymer-based lyoph- 574 ilized wafer through multiple models i.e a RhE (Reconstructed human Epidermis) com- 575 mercially available model, a porcine buccal tissue and an artificial buccal membrane [63], 576 while some studies have also employed the Ussing chamber $[64,65]$. However, the design 577 of the Franz cells allows the testing of a specific diameter of tissue of at least 6 mm or 578 more. The Epi-ExPer device presented in the present study allows for the use of smaller 579 tissue samples, even as small as 5 mm in diameter, thereby conserving animal or human 580 tissues. 581

5. Conclusions 582

The developed Epi-ExPer device represents a promising tool for the *ex vivo* assess- 583 ment of external stimuli and/or xenobiotics that come into contact with the oral mucosa. 584 The design and manufacturing of the device facilitate the oriented culture of the oral mu- 585 cosa tissue under ALI conditions, the delimited exposure to external chemical agents 586 and/or biomaterials, and the reproducible evaluation of tissue permeability immediately 587 post-treatment. Furthermore, the device accommodates a cost-effective, multi-use, and 588 high-throughput approach for the evaluation of newly developed biomaterials and phar- 589 maceutical agents interacting with the oral mucosa. A proof-of-principle analysis of the 590 Epi-ExPer system in the present study also suggested a dose-dependent corrosive effect 591

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